

Motor neuron output in the crustacean cardiac ganglion is organized and  
maintained by homeostatic conductance relationships

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By  
RANSDELL, JOSEPH L. (MU-STUDENT)  
Dr. David J. Schulz, Dissertation Supervisor

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The undersigned, appointed by the dean of the Graduate School,  
have examined the dissertation entitled  
**MOTOR NEURON OUTPUT IN THE CRUSTACEAN CARDIAC GANGLION IS  
ORGANIZED AND MAINTAINED BY HOMEOSTATIC CONDUCTANCE  
RELATIONSHIPS**

Presented by Ransdell, Joseph L. (MU-Student)

A candidate for the degree of  
Doctor of Philosophy

And hereby certify that, in their opinion, it is worthy of acceptance.

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Dr. David J. Schulz

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Dr. Andrew D. McClellan

---

Dr. Michael L. Garcia

---

Dr. Troy Zars

---

Dr. Satish S. Nair

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## ABSTRACT

Generating appropriate and functional neuronal output is a matter of fundamental importance to nervous systems across species and phyla. Potential perturbations to a neurons intrinsic excitability alone include hebbian style plasticity, ion channel turnover and neuromodulation. With these dynamic processes in place, it is remarkable that neurons are able to maintain stable and functional output throughout the life of an organism. Yet little is known about the cellular mechanisms in neurons and networks which act to stabilize functional output. Here we utilize large cell motor neurons of the *Cancer borealis* cardiac ganglion to investigate how these cell's important burst output is generated, maintained and synchronized across cells in a rhythmic motor network.

The *C. borealis* cardiac ganglion (CG) acts as a nine cell central pattern generator (CPG) which drives the rhythmic contraction of the *C. borealis* heart. The ganglion is made up of 4 pacemaker neurons (small cells) which drive 5 motor neurons (large cells) to elicit burst organized potentials responsible for the heart contraction. Recently the large cells have been the basis for both a biological (Tobin et al., 2009), as well as two conductance based computational modeling studies (Franklin et al., 2010). Results in these studies suggest Large Cell (LC) motor neurons in the CG may regulate and preserve their important electrophysiological output using variable intrinsic conductance organization. This supports an intriguing and relatively new hypotheses, that important neuronal outputs are maintained by conserving key intrinsic conductance relationships, rather than constraining the magnitude of individual ionic currents (Goldman et al., 2001a, Golowasch et al., 2002, Prinz et al., 2004a, Schulz et al., 2006, Schulz et al.,

2007a); these conserved conductance relationships act to balance properties of excitability resulting in an appropriate electrophysiological output. Studies across model systems have provided evidence for this hypothesis by demonstrating compensatory regulation between voltage and ligand gated ion channels (Guo et al., 2005, Nerbonne et al., 2008), as well as the currents they mediate (LeMasson et al., 1993, Turrigiano et al., 1994, Turrigiano et al., 1995, Golowasch et al., 1999), which then cause properties of electrophysiological output to be maintained; this type of regulation has become known as homeostatic plasticity.

The *C. borealis* CG studies mentioned above utilize either conductance based computational modeling, or molecular biology to study how LCs organized their electrophysiological output. Here we investigate the electrical properties of the *C. borealis* LCs, as well as profile additional channel gene mRNA expression in LCs relate to the conductances mediated by those channel genes. We find that large cell motor neurons utilize multiple intrinsic currents to mediate burst potentials, and these currents are in part localized to the LC somata, distal from action potential generating currents. Next we examine the functional organization of these intrinsic currents and show that LC motor neurons, which have synchronous burst activity during normal network behavior, have differential intrinsic tuning even across LCs even in a single network.

The LC burst waveform is maintained across network LCs in part by a rapid compensatory relationship between the two potassium currents,  $I_A$  and  $I_{HTK}$ . This relationship results in a negative correlation between the two currents across LCs. We show that this relationship is maintained via a fast compensatory response, which is in part dependent on levels of intracellular calcium. Using single cell quantitative PCR we find channel genes which mediate these two currents also have a conserved relationship across cells, although the correlation is positive rather than negative. We hypothesize that this difference is due to an existing pool of channel mRNA or protein which allows a rapid compensatory interaction between the two currents.

While this differential tuning is likely the result of conserved conductance relationships, we demonstrate that conserved relationships which act in maintaining output also bridge intrinsic properties of the cell with network level properties; namely we show a conserved relationship between the transient potassium current  $I_{HTK}$  and strength of LC to LC electrical coupling. Using dynamic clamp to manipulate electrical coupling, and pharmacological blockers to manipulate  $I_{HTK}$ , we demonstrate that this relationship is important in maintaining synchronized bursts between network LCs.

Together these data demonstrate that burst output of the LC motor neuron, while driven via SC input, is heavily influenced by several ionic conductances and network

level properties. These properties are tuned in a differential manner, though with conserved relationships, to maintain appropriate LC excitability and burst output.

## INTRODUCTION

In considering the electrophysiological output of neurons we often think of action potential waveforms, these brief events consist of a rapid upswing and downswing in membrane potential, mediated primarily by fast inactivating sodium current and delayed rectifier potassium current. This idea of neuronal output neglects cells which, instead of firing single action potentials, fire in bursts of action potentials. Bursting output relies on a slow wave depolarization which places the neuronal membrane potential above action potential threshold for an extended period of time; this involves several additional ionic currents and can result in several action potentials grouped together (Rutecki, 1992, Overton and Clark, 1997). Several studies have found functionality behind this mode of output, which spans sensory and motor neurons, in both vertebrate and invertebrate species (Cattaneo et al., 1981, Bair et al., 1994, Tseng and Nadim, 2010). Neuronal bursts have been shown to increase both the reliability and efficiency of synaptic transmission as well as provide greater information content than single spikes (Lisman, 1997, Koulakov et al., 2002). However coming up with a detailed understanding of how a neuron intrinsically instigates this slow wave burst potential presents a problem for most model organisms. Measuring all or even several properties which coordinate the biophysical basis of a neuronal burst is a challenge, and measuring this in several neurons with a conserved electrophysiological signature is often impossible.

In this regard LC motor neurons of the *C. borealis* cardiac ganglion make an ideal system to investigate underlying properties responsible for burst output. The *C. borealis* CG is able to maintain rhythmic output even after it is removed from the heart musculature of the animal, meaning, if the CG is left intact, it can continue rhythmic motor output in the absence of external stimuli and musculature feed-back; we classify these types of motor networks as central pattern generators (Marder and Bucher, 2001). Central pattern generators (CPG) are neural networks responsible for rhythmic motor output often vital to the survival of the animal. Some of the behaviors these networks are responsible for include breathing, walking, chewing and swallowing (Marder et al., 2005). Simple CPG networks in invertebrate animals have become invaluable models for studying not only principles behind CPG function, but also general principles in regards to how neurons and networks are able to maintain and regulate appropriate excitability and output. Properties which make these invertebrate CPG networks particularly useful to researchers include the large size of the neurons, simple network architecture and the ability to unambiguously identify the same neuron from animal to animal (Selverston, 2010). In the following experiments we investigate how the LC motor neurons in the *C. borealis* CG generate and maintain synchronous burst potentials which allow the single chambered *C. borealis* heart to rhythmically contract.

The *C. borealis* cardiac ganglion is a central pattern generator made up of nine neurons which cause rhythmic contractions of the crab heart (Cooke, 2002b, Cruz-Bermudez and Marder, 2007b). Two neuronal types are involved: four pacemaker

neurons known as Small Cells (SC) and five motor neurons known as Large Cells (LC). The SCs endogenously burst providing excitatory input to the LC motor neurons causing a large cell burst potential; this LC burst of action potentials causes the motor output of the network, which is a single contraction of the crab heart (Hartline, 1967; Tazaki and Cooke, 1979, 1983c, a; Berlind, 1989). The anterior LC motor neurons offer several advantages for investigating properties responsible for burst output. Conductances which work in eliciting the intrinsic slow wave burst potential are present in anterior LC somata, whereas the action potential generating conductances of the anterior LCs, are localized to the distal neurite. This network architecture is present in other crustacean species CG (Tazaki and Cooke, 1986) as well as in *C. borealis* CG (for *C. borealis* network architecture see Figure 1.1). The *C. borealis* anterior LCs also have conserved LC somata spacing, allowing the use of thread ligatures to isolate and study the burst generating properties in a single identified LCs (Figure 1.1A). Finally, the somata of each LC is large enough to be individually harvested for single cell quantitative PCR.

In the following studies we characterize the native intrinsic organization underlying LC motor neuron burst potentials, along with mechanisms by which these underlying properties are regulated and maintained. To study how burst output is intrinsically mediated we eliminate external stimuli from an individual cell, and subsequently characterize / study the complement of intrinsic biophysical properties which integrate stimuli and elicit the resulting burst output. These biophysical properties can be broken into two main categories: the suite of intrinsic ionic conductances which

sum to elicit a unique change in membrane potential and the network level properties which influence the activation of voltage gated intrinsic conductances. In this group of experiments we use the three anterior LCs as a reduced preparation to investigate how the LC ionic conductances are organized, maintained and finally, interact with network level properties to generate appropriate LC burst output.

We begin by characterizing the depolarizing conductances present in anterior LC somata (chapter 1). In chapter two we characterize three outward potassium currents, and go on to study a negative compensatory relationship between two of those currents. In chapter three we show that LCs within a network have disparate intrinsic organization, which are tuned to respond to network driven depolarizing stimuli in very similar ways. Finally, in chapter 4 we show that synchronization across LCs is in part maintained by a relationship between an intrinsic potassium current and LC to LC electrical coupling strength.

## CHAPTER 1

### **Characterization of inward currents and channels underlying burst activity in motor neurons of the crab cardiac ganglion**

Large cell motor neurons in the *Cancer borealis* cardiac ganglion generate rhythmic bursts of action potentials responsible for cardiac contractions. While it is well known these burst potentials are dependent on coordinated interactions among depolarizing and hyperpolarizing conductances, the depolarizing currents present in these cells, and their biophysical characteristics, have not been thoroughly described. In this study we used a combined molecular biology and electrophysiology approach to look at channel identity, expression, localization, and biophysical properties for two distinct high-voltage activated calcium currents present in these cells: a slow calcium current ( $I_{CaS}$ ) and a transient calcium current ( $I_{CaT}$ ). Our data indicate that CbCaV1 is a putative voltage-gated calcium channel subunit in part responsible for an L-type current, while CbCaV2 (formerly *cacophony*) is a subunit in part responsible for a P/Q-type current. These channels appear to be localized primarily to the somata of the motor neurons. A third calcium channel gene (CbCaV3) was identified that encodes a putative T-type calcium channel subunit and is expressed in these cells, but electrophysiological studies

failed to detect this current in motor neuron somata. In addition, we identify and characterize for the first time in these cells a calcium-activated nonselective cationic current ( $I_{CAN}$ ), as well as a largely non-inactivating TTX sensitive current reminiscent of a persistent sodium current. The identification and further characterization of these currents allows both biological and modeling studies to move forward with more attention to the complexity of interactions among these distinct components underlying generation of bursting output in motor neurons.

Bursts of action potentials are vital to appropriate motor output in central pattern generator networks. The organization of burst potentials often relies on calcium- and sodium-mediated depolarizing currents which have an influence on neuronal function beyond eliciting a direct change in membrane potential. For example, calcium influx via voltage-gated calcium currents are known to affect second messenger systems involved in transcriptional regulation (Clapham, 2007), activate other ionic currents (Wisgirda and Dryer, 1994, Yamoah et al., 1994, Sah, 1995) as well as trigger neurotransmitter release at the synapse (Mulkey and Zucker, 1993). Sodium has been shown to activate sodium-dependent potassium currents and influence neuronal excitability (Rose, 2002, Hage and Salkoff, 2012). These higher order cation effects are also known to act as the mechanism behind different forms of plasticity in the ongoing output of a cell and/or network (Cummings et al., 1996, Turrigiano, 2008, George et al., 2012). However before we can fully understand the role of inward currents and resulting cation influx during a burst potential, we must have a thorough understanding of what depolarizing components exist in a given cell type.

The Large Cell (LC) motor neuron of the *Cancer borealis* cardiac ganglion has been a successful model for studying how underlying conductances interact to mediate burst potentials (Tobin et al., 2009, Ball et al., 2010a, Franklin et al., 2010) and new evidence shows there is rapid calcium-dependent homeostatic compensation among potassium currents which impacts both LC intrinsic excitability as well as appropriate network bursting (Ransdell et al., 2012). However there is little characterization of what depolarizing properties are active in the *C. borealis* LC burst, hindering a more complete understanding of how the LC bursts are generated and maintained. The goal of this study is to characterize the depolarizing components intrinsic to the LC motor neuron in the *C. borealis* cardiac ganglion.

Despite the extensive use of crustacean motor systems as models for understanding neuronal network function and modulation (Marder and Bucher, 2007), the inward currents have been less thoroughly studied than their outward counterparts. In neurons of the stomatogastric ganglion (STG), total voltage-activated calcium current has been successfully measured using sensitivity to cadmium chloride as an effective blocker (Golowasch and Marder, 1992). Further pharmacological dissection of STG calcium currents suggest there are two distinct high threshold calcium currents present: an L-type (CaV1) and a P/Q type (CaV2) (Hurley and Graubard, 1998, Johnson et al., 2003). Molecular cloning studies support the presence of these two calcium channel types in neurons of the STG (French et al., 2002). Because the calcium dependence of synaptic transmission in STG neurons has a more hyperpolarized threshold (-60 mV) than these

two high threshold currents, there is thought to be an additional low threshold or T-type (CaV3) current involved in neurotransmitter release (Graubard et al., 1983, Harris-Warrick et al., 1992). In the cardiac ganglion, some analysis of calcium currents has taken place in the LCs (Tazaki and Cooke, 1979, 1986), particularly in the lobster *Homarus americanus* (Tazaki and Cooke, 1990). However, a more thorough analysis of these currents is necessary to understand their role in generating burst output in LC motor neurons.

Beyond calcium currents, evidence for persistent sodium currents (TTX sensitive) has also been reported in both the STG (Turrigiano et al., 1995, Elson and Selverston, 1997) as well as the cardiac ganglion LCs of the lobster *H. americanus* (Berlind, 1993). The somata of these crustacean motor neurons do not contain spike-mediating sodium currents(Golowasch and Marder, 1992). However, a characterization of persistent sodium currents has yet to be performed in these crustacean systems. In addition, plateau potentials in the dorsal gastric neurons of the STG depend on activation of a calcium-dependent voltage-independent cationic current, or “CAN current” (Zhang and Harris-Warrick, 1995, Zhang et al., 1995), but this current has yet to be identified or characterized in LC motor neurons.

With the *C. borealis* LC motor neuron being the focus of several recent studies exploring how intrinsic conductances and channels are organized and conserved during burst generation (Tobin et al., 2009, Ball et al., 2010a, Franklin et al., 2010, Ransdell et al., 2012) a more thorough characterization of the inward currents in this species and cell

type are both important and valuable to moving research in this area forward. Here we utilize multiple techniques, including two-electrode voltage clamp, immunohistochemistry and single cell PCR analysis of channel gene expression to explore these depolarizing components in the LCs of the crab, *Cancer borealis*.

## **Materials and Methods**

*C. borealis* crabs were purchased and shipped overnight from The Fresh Lobster Company (Gloucester, MA, USA). Crabs were kept between 24 hours and two weeks in artificial sea water at 12 °C before use. Crabs were anesthetized in ice for 15 minutes prior to the dissection. The dissection took place in chilled physiological saline comprised of 440 mM NaCl, 26 mM MgCl<sub>2</sub>, 13 mM CaCl<sub>2</sub>, 11 mM KCl, and 10 mM HEPES (pH = 7.4). Details of the cardiac ganglion dissection can be found in Cruz-Bermúdez et al. (2007)(Cruz-Bermudez and Marder, 2007a). All experiments were conducted on the three anterior LCs (see Figure 1, black arrows; Figure 1C). To isolate large cell somata from action potentials and network activity individual strands of bulking nylon (made by Gütermann Creative) were used to ligate the nerve at the anterior branch point of the CG (Figure 1). To impale large cells each cell was desheathed using a desheathing pin. LC3 / LC4 were isolated from the rest of the network in a pair.

## **Electrophysiology**

All experiments were done in physiological saline cooled to 12°C. Two-electrode voltage clamp (TEVC) and two-electrode current clamp (TECC) protocols were carried out by impaling a large cell with two glass electrodes filled with 3M KCl (8-17 MΩ resistance) using an Axoclamp 2A amplifier (Axon Instruments, Union City CA). In TEVC experiments when all potassium currents needed to be blocked, the current injecting electrode was filled with 1 M tetraethylammonium (TEA) + 1M cesium chloride (CsCl) (17-18 MΩ resistance). All recordings were made from large cell somata; action potential conductances were blocked (unless noted otherwise) by tightening a thread ligature past the anterior branch point on the nerve the LC was located in (Fig. 1A). TEVC and TECC protocols were created, driven and recorded with Clampex 9.2 software (Molecular Devices). Current and voltage recordings were analyzed with Clampfit 9.2 software (Molecular Devices). Current and voltage traces were filtered with a digital lowpass boxcar filter using 7 smoothing points at a sample frequency of 5 kHz.

*Pharmacology.* Pharmacological blockers were dissolved in physiological saline and perfused onto the cardiac ganglion using a Rabbit peristaltic pump (Rainin Instrument Company) at a rate of 1.5 mL / min. or added from a concentrated stock solution via pipette. Prior to TEVC or TECC protocols perfusion was stopped for at least five minutes to let the preparation temperature stabilize.

### **Voltage Clamp Protocols**

To voltage clamp inward currents, potassium currents were blocked by perfusing 50mM TEA, 1mM 4-aminopyridine (4AP) and injecting 1M TEA + 1M CsCl using

iontophoresis (300 msec 1.2 nA pulses at 2 Hz) for a minimum of one hour. To isolate calcium currents,  $10^{-6}$ M tetrodotoxin (TTX) also was added for a minimum of 45 minutes. When necessary, calcium currents were blocked using 250 $\mu$ M cadmium chloride ( $CdCl_2$ ) perfusion for a minimum of 45 minutes. Because of difficulty in fully blocking outward currents we often carried out trace subtractions before and after  $CdCl_2$  (45 min.) and before and after TTX (45 min.) to isolate Cd-sensitive currents and TTX-sensitive currents respectively.

To separate inactivating and non-inactivating high-voltage activated calcium currents, two TEVC protocols were carried out: one from a holding potential of -40 mV and 680 ms depolarization steps from -50 mV to +15 mV in 5 mV increments ( $V_h = -40$  mV) and a second identical protocol except from a holding potential of -80 mV ( $V_h = -80$  mV). Trace subtractions were used to isolate the additional inward current clamped with the -80mV holding potential, this current is labeled throughout the paper as “ $I_{CaT}$ ” while the inward calcium current clamped from a -40 mV holding potential is labeled “ $I_{Cas}$ ” (Liu et al., 1998, Prinz et al., 2003).  $I_{CaT}$  inactivation was measured in TEVC using a 800 ms prestep (-80 mV to -40 mV, 5 mV increments) prior to a 500 ms, -20 mV depolarizing step. To remove  $I_{Cas}$  the current generated with the -40 mV pre-step was subtracted from each sweep.  $I_{Cas}$  inactivation was measured in TEVC using 2 s pre-steps (-50 mV to + 5mV, 5 mV increments) followed by a 500 ms 0 mV depolarizing step.

Inward tail current was isolated with the same pharmacological agents as voltage-gated calcium currents and its magnitude was measured at -80mV holding potential after

680 ms depolarizing pre-steps between -50 and +15mV. To isolate  $I_{Cas}$  contribution to tail current, a -40mV holding potential was used prior to the depolarizing voltage step; in this protocol the tail current was still measured at -80 mV (Fig. 5B). Reversal of  $I_{CAN}$  was measured after a 1s +20 mV depolarizing voltage step. Magnitude of  $I_{CAN}$  was always measured at peak tail current after depolarizing voltage step.

TTX-sensitive current was isolated with the same pharmacological agents used to isolate calcium currents, with the addition of 250  $\mu$ M CdCl<sub>2</sub>. Depolarizing step TEVC protocols (steps = 680 ms, -50 mV to +15 mV;  $V_h$  = -40 mV) and voltage ramp TEVC protocols (4 s ramp, -80 mV to +20 mV) were carried out before and after 30 min. exposure to 10<sup>-6</sup> M TTX and trace subtractions were used to isolate the TTX sensitive current.

### **Sequencing of Calcium Channels**

We obtain *de novo* partial ORF sequence corresponding to three calcium channel alpha subunit cDNAs to aid in characterizing the channels potentially underlying calcium currents in LC motor neurons. The methods for this degenerate PCR approach are as described in detail previously (Schulz et al., 2006, Schulz et al., 2007a). Briefly, channel transcripts were amplified from a cDNA template derived from total RNA extracted from mixed nervous system tissue from *C. borealis*. We first designed and employed degenerate primer pairs based on conserved amino acid sequence compared across multiple invertebrate and vertebrate species, including *Lymnaea stagnalis*, *Drosophila*

*melanogaster*, *Apis mellifera*, *Daphnia pulex*, *Mus musculus*, and *Homo sapiens*. We used these primers in RT-PCR reactions (GoTaq Green, Promega) to obtain PCR products of predicted length, which were subsequently ligated into pGEM-T easy plasmid vector (Promega) and sequenced using dye terminator cycle sequencing (DTCS Quick Start Kit, Beckman Coulter). Sequences obtained were compared to orthologous sequences using BlastX (NCBI). Initial sequence obtained was extended by a process of additional RT-PCR reactions, each using one gene-specific primer within the newly elucidated sequence and one degenerate primer outside the known sequence that would allow us to extend the sequence. Once we obtained enough sequence information to feel that we definitively could identify a calcium channel ortholog, a final PCR (Platinum Taq DNA polymerase, Invitrogen) was performed with gene-specific primers that spanned the entire assembled sequence to ensure a contiguous cDNA existed in our template pool. Accession numbers for these new sequences are as follows: (Cb = *Cancer borealis*) CbCaV1: JN809809, CbCaV2: JN809808, CbCaV3: JN809810. Primer sequences that will result in PCR products that contain the entirety of the assembled sequence thus far are as follows: CbCaV1-Forward 5'- CAATGCATTACGATGGAGGGG – 3' ; CbCaV1-Reverse 5' – AACACCTCCTGAAGTAGTCTTG – 3'; CbCaV2-Forward 5' – TGGAACATTATGGACTTCGTTG – 3' ; CbCav2-Reverse 5' - CCAGCCCCACCAAGCCTCCTG – 3' ; CbCav3-Forward 5' – CAAGGATGGCTGGGTCAACAT – 3' ; CbCav3-Reverse 5' – GGCTCTAATGCCCTTGGCCAT – 3'.

## Single-cell PCR

Details regarding the harvesting of individual LC motor neurons for single-cell molecular analysis are provided in a previous publication (Tobin et al., 2009). Briefly, ganglia were desheathed around the area where large cells (LCs) were visually identified, and to facilitate removal of the neurons, the ganglia were exposed to protease (Sigma) for several minutes. The protease was replaced with a cold (~0° C) solution of 70% ethylene glycol and 30% saline, and the ganglia were put in a -20° C freezer for up to 1 hour. The cells were then manually removed with fine forceps and each cell was placed in a cryogenic tube with 350 ml lysis buffer (buffer RLT, Qiagen) and 1% β-mercaptoethanol. The tubes were immediately placed on ice, then stored at -80°C until RNA extraction.

Quantitative RT PCR was performed as in Schulz et al. 2006, and modified as in Tobin et al. 2009. Primers specific for real-time PCR detection of CbCaV1, CbCaV2, and CbCaV3 using SYBR Green were developed and designed using Primer3 software as follows: CbCaV1–Forward 5'– GATGGAGGGAGACGACAAGA –3'; CbCaV1–Reverse 5' – GGTTGTTGAGCCTCGTCATT – 3'; CbCaV2–F 5'– GTATCCGGCGGACAGTAAAG –3'; CbCaV2–R 5'– AAACTTGGTGAGAAATGGCG –3'; CbCaV3–F 5'– CCAGTTGGATGTGTTCATCG –3'; CbCaV3–R 5'– ATGATGGTTGGGTTGATTGG –3'. PCR amplicon sizes were 90bp (CbCaV1), 120bp (CbCaV2), and 93bp (CbCaV3). Primer sets were validated for PCR efficiency, linear dynamic range, and limit of detection using both a plasmid template that contained the gene of interest, as well as cDNA generated from total RNA

extracted from crab neural tissue. All qPCR reactions were carried out with a final primer concentration of 0.25 µM for each primer, using RT<sup>2</sup> SYBR Green qPCR Mastermix (SABiosciences). RNA from single neurons was extracted using RNeasy micro kit (Qiagen), and reverse transcription using SuperScript III (Invitrogen). See Schulz et. al 2006, Schulz et. al. 2007 for more details. Assay quality and variability was monitored via 18S rRNA quantitation (Schulz et al., 2006, Schulz et al., 2007a, Tobin et al., 2009, Ransdell et al., 2010). Data in this study are presented as raw copy number per cell (see Tobin et al. 2009).

### **Cell fills and Immunohistochemistry**

To visualize stereotypical localization of LC somata and projections in the cardiac ganglion, we iontophoresed a fluorescent tracer (AlexaFluor 568, Invitrogen) using backfilled microelectrodes by overriding the electrode capacitance compensation for 5 minutes. Dye was allowed to diffuse throughout the ganglia for 24 hours in physiological saline at 4° C, and then preparations were directly imaged using a Leica M205F Stereomicroscope with a Leica DFC 345 FX camera.

For immunohistochemistry, cardiac ganglia with desheathed LCs were pinned to Sylgard and fixed in 0.1 M phosphate buffered saline (PBS; 440 mM NaCl, 11 mM KCl, 10 mM Na<sub>2</sub>HPO<sub>4</sub>, 2 mM KH<sub>2</sub>PO<sub>4</sub>, pH 7.4) containing 2% paraformaldehyde for 40-90 minutes and then washed 2 x 10 minutes in PBS containing 0.1% Triton-X (PBT). Rabbit pan polyclonal primary antibody to CaVα1 subunit (Anti-CaVpan α1; Alomone Labs)

was applied overnight at a concentration of 1:100 in PBT at 4 °C. Ganglia were rinsed 4 x 10 min. in PBT. CaV $\alpha$ 1-like immunoreactivity was investigated with 1:250 dilution goat anti-rabbit IgG conjugated to Alexa Fluor® 568 dye in PBT (Molecular Probes/Invitrogen) for 12-20 hours. Ganglia were rinsed again in PBS at least 5 x 15 min., and mounted in ProLong Gold which contained DAPI (Invitrogen). Images were acquired with an Olympus IX81 epifluorescent microscope with MicroSuite software.

## Statistics

Analyses were done using SigmaPlot 11.0. R-values reported are results of Pearson correlation (Fig. 3I). After passing Shapiro-Wilk tests for normality, changes in current magnitude before and after pharmacological treatments were analyzed with paired *t*-tests.

## Results

### Calcium channel expression in LCs

To determine which calcium current subtypes may be present in LC motor neurons, we decided first to adopt a molecular approach and look for expression of voltage-gated calcium channels at the mRNA level. The most thorough combined molecular and electrophysiological characterization of voltage-gated calcium channels in invertebrates has been performed for the snail, *Lymnaea stagnalis* (Spafford et al., 2003,

Spafford et al., 2006, Senatore and Spafford, 2010). Thus we will use direct comparisons of our channels and currents to these well characterized invertebrate examples as basis for interpretation of our molecular calcium channel genes. We obtained *de novo* sequence, or extended partial sequences, for three channel genes that appear to be orthologous to single representatives for each of three calcium channel gene families CaV1 (L-type), CaV2 (P/Q-type), and CaV3 (T-type) found in most invertebrates (Jeziorski et al., 2000, Spafford and Zamponi, 2003). We will refer to each crab gene as CbCaV1, CbCaV2, and CbCaV3, Cb to denote *C. borealis* and 1, 2, or 3 for the gene family to which the sequence is most orthologous. We assigned gene identities to our channel transcripts by comparing our three putative calcium channel genes to the orthologous *L. stagnalis* calcium channel sequences (Figure 2A). Obtaining partial sequence of the calcium channel genes allowed us to develop primers to analyze single large cell mRNA expression of each channel gene (Fig. 2B). LC motor neurons expressed detectable amounts of all 3 putative calcium channel subunits, with CbCaV1 having the lowest mRNA copy number, while higher levels of both CbCaV2 and CbCaV3 were detected (Fig. 2B).

Across the respective stretches of these channel sequences between *Cancer borealis* and *Lymnaea stagnalis*, CbCaV1 sequence shares 581 out of 801 identical amino acids with *Lymnaea stagnalis* (LCaV1; 73%), CbCaV2 (initially referred to as *cacophony*; see Tobin et al. 2009) shares 970 out of 1483 identical amino acids (65%) to LCaV2, and CbCaV3 shares 325 out of 428 identical amino acids (76%) to LCaV3. The location of these regions of overlap between *C. borealis* and *L. stagnalis* are shown in Figure 2C

with respect to putative transmembrane domains and IQ-like binding motifs of these channels (Van Petegem et al., 2005). These binding domains and their amino acid similarity to mammalian orthologs are shown in Figure 2D. In addition, to confirm their identity as calcium channels we identified and aligned the EEEE and EEDD loci of the pore forming loops with consensus mammalian sequences. These EEEE/EEDD loci are known to confer divalent cation selectivity to these channels (Tang et al., 1993, Yang et al., 1993, Cens et al., 2007), and are a hallmark for the identification of voltage-gated calcium channels.

### Calcium currents

To isolate voltage-gated calcium currents we minimized competing sodium and potassium currents with pharmacological blockers (see methods). Total inward current under these conditions was measured (Figure 3A). This revealed what appeared to be a faster transient inward current ( $I_{CaT}$ ; Figure 3A), a slower more persistent inward current ( $I_{Cas}$ ; Figure 3A), a late outward current, and an inward tail current (Figure 3A). Addition of  $CdCl_2$  (see Figure 4F) completely eliminates the inward currents and reduces or eliminates the tail current, leaving behind only a small residual outward current that is presumably due to an incomplete block of  $I_A$  and/or  $I_{Kd}$ . Taken together, these data plus the gene expression results suggest the presence of multiple distinct calcium and calcium-dependent inward currents in the LC motor neurons.

We then attempted to characterize these distinct currents by a combination of pharmacology and voltage-clamp protocol manipulation. Low-threshold, T-type calcium currents in *L. stagnalis* (LCaV3) activate at hyperpolarized voltages around -60 mV, are transient, and sensitive to block with nickel (Senatore and Spafford, 2010). We were unable to elicit inward current in LC motor neuron somata for any voltages lower than -30 mV (see Figure 3D), and application of NiCl<sub>2</sub> (75-250 µM, N = 4) resulted in no change in inward current magnitude or kinetics (data not shown). Therefore, although we detected relatively abundant transcripts for CbCaV3 in LC motor neurons (Figure 2B), we were unable to detect any active T-type current from somatic voltage-clamp experiments in these cells.

P/Q-type calcium currents (e.g. LCav2) are more rapidly transient than L-type calcium currents (e.g. LCav1) and inactivate at more hyperpolarized holding potentials (Tsien et al., 1988, Hille, 2001). Therefore, we set out to separate these potentially distinct native high-threshold calcium currents by subtracting inward current clamped with a -40 mV holding potential from inward current with a -80 mV holding potential in LC motor neurons. The more persistent calcium current (I<sub>CaS</sub>; Figure 3B) activates at -30 mV and reaches its peak near 0 mV (Figure 3D). The transient current (I<sub>CaT</sub>; Figure 3C) activates at similar voltage as I<sub>CaS</sub> (i.e. -30 mV), but reaches its peak at more hyperpolarized voltages near -20 mV (Figure 3D). Native current levels for I<sub>CaS</sub> and I<sub>CaT</sub> in individual LC motor neurons was variable from cell to cell, and ranged from approximately 3 to 6 nA for both currents (Figure 3E). However, the most noticeable distinction between I<sub>CaS</sub> and I<sub>CaT</sub> in these cells is the voltage dependence of inactivation.

$I_{CaT}$  shows an approximately 30 mV more hyperpolarized half-inactivation voltage than  $I_{Cas}$  (Figure 3F). In addition,  $I_{CaS}$  and  $I_{CaT}$  are distinguished by differences in time constant of inactivation (Figure 3G), and time to peak (Figure 3H), as a function of voltage. There is a consistent relationship between time to peak current for  $I_{Cas}$  and  $I_{CaT}$  that would suggest these currents are able to maintain distinct impacts on cell voltage across a range of activation voltages (Figure 3I). These characteristics are consistent with differences reported between high-voltage activated calcium currents LCaV1 and LCaV2 in *L. stagnalis* (Spafford et al., 2006) and similar to differences among L- and P/Q-type calcium currents in mammals (Tsien et al., 1988, Hille, 2001). Based on these results, we propose that  $I_{Cas}$  current in crab LC motor neurons is homologous to CaV1 current as described in *L. stagnalis* (Spafford et al., 2006), and reminiscent of mammalian L-type calcium currents (Tsien et al., 1988, Hille, 2001), while  $I_{CaT}$  is homologous to LCaV2 as described in *L. stagnalis* (Spafford et al., 2003, Spafford et al., 2006) and reminiscent of mammalian P/Q-type currents (Tsien et al., 1988, Jeziorski et al., 2000, Hille, 2001). To further confirm the characteristics of these calcium currents, as well as investigate any calcium-dependent aspects of their kinetics, we performed our voltage clamp experiments with  $BaCl_2$  substituted for  $CaCl_2$  in the saline, as well as with addition of  $CdCl_2$  to the saline. Both  $I_{Cas}$  and  $I_{CaT}$  are carried by  $Ba^{2+}$ , and show similar activation characteristics to the native calcium currents (Figures 4A and 4C). Furthermore, both  $I_{Cas}$  and  $I_{CaT}$  are eliminated by  $CdCl_2$  administration (Figure 4F). This further supports the hypothesis that these inward currents are indeed calcium mediated. We also noted that the slow inactivation of  $I_{Cas}$  is eliminated or significantly reduced ( $P < 0.01$ ;  $N=5$ ) in the corresponding  $I_{Ba}$  (Figure 4B, black arrows; Figure 4E), suggesting that the inactivation

of this current is not purely voltage-dependent, but rather a calcium-dependent inactivation (CDI). This is also a characteristic consistent with mammalian and other invertebrate L-type calcium currents (Hille, 2001). We were able to identify in our CbCaV1 sequence an IQ-binding motif that has been shown to strongly influence CDI in mammalian L-type channels (Zuhlke et al., 2000). Site directed mutagenesis shows that the IQ amino acid residues of this motif, as well as an FRK motif within the domain are significant mediators of CDI, with the mutagenesis of K to A having the least impact in the motif (Zühlke et al. 2000). Our putative IQ-domain shows this same pattern of amino acid residues (Figure 2D), differing only in the K-residue, which is consistent with the observation of CDI in our  $I_{CaS}$  characterization. Additionally, we sometimes detected a decrease in the magnitude of  $I_{CaT}$  following barium substitution (Figure 4D), which could be indicative of a calcium-dependent facilitation of the native transient calcium current in these cells (Tazaki and Cooke, 1990). While these collective data are consistent with CDI of  $I_{CaS}$  as suggested by barium substitution, it is possible that barium influences other currents that may be incompletely blocked by our experimental protocol, altering the apparent inactivation kinetics of  $I_{CaS}$ .

Barium did not cause a change in inactivation kinetics of  $I_{CaT}$  (Figure 4D; 4E), suggesting that this current does not show CDI. There is less known about the molecular basis of CDI and the IQ-domain in P/Q-type currents. However, CDI in these channels has been linked to an interaction with an IQ-like binding domain (including IM amino acid residues; see Figure 2D) with a calmodulin binding domain within CaV2 channels in mammals (Lee et al., 2003). While this interaction is not yet well characterized, it is

noteworthy that our CbCaV2 IQ-like domain lacks the IM motif implicated in CDI, consistent with our lack of evidence for CDI for  $I_{CaT}$ .

### CAN (calcium-activated nonselective cationic) current

We observed a native inward tail current (Figure 3A) that is eliminated following CdCl<sub>2</sub> administration (Fig. 4F) and significantly decreased after BaCl<sub>2</sub> substitution (pre-Ba<sup>2+</sup> mean =  $-5.7 \pm 0.5$  nA; post-Ba<sup>2+</sup> mean =  $-2.7 \pm 1.0$  nA; N = 3; P = 0.03) (Fig. 4B, 4C; gray arrows), suggesting the presence of a calcium-activated depolarizing conductance in these cells. The observed characteristics of this current are very similar to a calcium-activated nonselective cationic current ( $I_{CAN}$ ) found in STG neurons of lobster, and described in detail by Zhang et. al. (1995). We performed subsequent voltage-clamp and pharmacological manipulations to determine whether the current we observe in LC motor neurons shares the same kinetics and properties of  $I_{CAN}$  as described in lobster(Zhang et al., 1995).

To analyze  $I_{CAN}$  in LC motor neurons, we bath applied TTX, TEA, 4-AP and iontophoresed Cs<sup>+</sup> intracellularly as described in the Methods. We then elicited inward currents with increasing depolarizing voltage steps, followed by clamping tail currents at -80 mV. As seen in Figure 3A, as well as Figure 5A (inset), these protocols resulted in initial inward current activation, usually a late outward current, and then an inward tail current measured at -80 mV (see Figure 5A inset, arrow). The tail current activated at

voltages above -30 mV (concomitant with  $I_{Ca}$ , see Figure 3D), reaching a peak around +15 mV (Figure 5A).

We next investigated if the pre-pulse voltage and thus activation of distinct voltage-dependent calcium currents ( $I_{Cas}$  and  $I_{CaT}$ ) is correlated to tail current activation by clamping the LC to depolarized potentials which activate both currents (holding potential = -80 mV). We found that while using a holding potential of -80 mV (eliciting both  $I_{Cas}$  and  $I_{CaT}$ ) results in a larger overall tail current (Figure 5B), holding at -40 mV (activating only  $I_{Cas}$ ) still is sufficient to activate the tail current (Figure 5B) but reduced in magnitude approximately 35%. These results suggest that the tail current is activated by calcium influx via both  $I_{Cas}$  and  $I_{CaT}$ .

To measure the reversal potential of the tail current, inward current was activated with a depolarizing step from a holding potential of -40 mV up to +20 mV, and then the tail current clamped across a range of voltages from -85 mV to -20 mV (Figure 5C). Through these experiments we obtained an I-V curve based on measurements of the peak tail current, from which we extrapolated the reversal potential of the tail current to be approximately -30 mV (Figure 5D).

Finally, we investigated whether the tail current is sensitive to increases in intracellular calcium release. Figure 5E demonstrates that caffeine exposure (bath applied for 10 minutes at 10 mM), known to stimulate intracellular calcium release (Friel and Tsien, 1992b, a, Zhang and Harris-Warrick, 1995, Yoshimura, 2005) as well as an

increased level of calcium induced calcium release (Mironov and Usachev, 1991, Levi et al., 2003), causes an increase in the inward tail current ( $N = 4$ ,  $P = 0.047$ ). These results suggest that the tail current is indeed calcium-activated and not solely dependent on extracellular calcium influx via voltage-gated calcium currents. Taken together these results are very similar to the characteristics of the CAN current in lobster, including sensitivity to caffeine exposure(Zhang and Harris-Warrick, 1995), indicating the same current is indeed present in LC motor neurons of the crab.

**TTX application reveals a largely non-inactivating TTX-sensitive current in LC motor neurons**

During our experiments, we observed that in the presence of TEA and 4-AP,  $\text{CdCl}_2$  alone does not consistently prevent all voltage-activated inward current (Figure 6A), but rather  $\text{CdCl}_2$  and TTX combined are required to eliminate inward current (Figure 6A). These observations suggest that there is a TTX-sensitive current, distinct from spike-mediated sodium currents, involved in bursting in these cells. We attempted to voltage-clamp this current by subtracting the TTX sensitive inward current in both step and ramp voltage clamp protocols, with inconsistent results. Because of the small magnitude of the TTX-sensitive current (on the order of 2 nA or smaller, clamped from the soma), voltage-clamp protocols using step depolarizations often were not adequate to clearly characterize this current above background noise, though they did suggest the current is largely non-inactivating (Figure 6B). Voltage ramp protocols used before and after TTX ( $10^{-6}$  M, 30 min.) to isolate the TTX sensitive current during a -80 to +20 mV

ramp demonstrated TTX-sensitive current activation began at  $-37.5 \text{ mV} \pm 4.7 \text{ mV}$  and peak activation occurred at  $6 \text{ mV} \pm 3.2 \text{ mV}$  (Figure 6B, N=3).

Because we had mixed success voltage-clamping the TTX-sensitive current, and because of its often smaller magnitude, we set out to determine whether this current plays an active role in the burst dynamics of LC motor neurons. To investigate this, we induced exaggerated burst potentials in isolated LCs by adding 50 mM TEA to the saline and generating large burst potentials with depolarizing current pulses (Figure 6C). These potentials are intrinsically driven because the depolarizing potential lasts longer than the brief current injection. After burst potentials were successfully generated,  $10^{-6} \text{ M}$  TTX was added, thus eliminating the TTX-sensitive inward current. In 6 out of 6 experiments, TTX administration completely eliminated these burst potentials (Figure 6C), supporting the presence of this current and suggesting an active role for this current in burst output. However, the exact impact of this TTX-sensitive current on burst dynamics in these cells is beyond the scope of this study. Nevertheless, it does appear that despite its small magnitude, this current is present and plays a role in the output of these cells.

### **Hyperpolarization-activated mixed cationic current ( $I_H$ )**

We also employed hyperpolarized voltage steps in voltage-clamp, as well as negative current inject in current clamp, to investigate the presence of hyperpolarization-activated mixed cationic current ( $I_H$ ) in the somata of these cells. Although relatively abundant mRNAs for the HCN channel have been detected in these cells (Tobin et al.

2009), we did not see any evidence for the H current in the somata of these cells (data not shown) for voltages as low as -120 mV from a holding potential of -40 mV.

### **Immunohistochemical localization of voltage-gated calcium channels in LC motor neurons**

The crustacean CG LC burst potential is mediated by intrinsic conductances at least in part isolated to the LC somata. In many crustacean species this intrinsic burst, termed a driver potential, can be regularly elicited in an isolated LC somata with a short depolarizing current injection (Tazaki and Cooke, 1983a, Cooke, 2002b). However, in *C. borealis* CG the isolated LC soma will rarely fire an intrinsic burst without the application of potassium current blockers such as TEA. While outward currents are clearly present (Ransdell et al. 2012), our voltage-clamp showed relatively low calcium current levels in the LC somata. This could be due to the fact that the calcium channels are localized more distant to the soma, or reflect a low overall calcium current in the soma itself. Therefore, we sought to find if and to what degree calcium channels are localized to the LC somata. We used a pan-species primary antibody selective for high-voltage-activated calcium channels (i.e. L-type and P/Q-type) combined with fluorescence microscopy to investigate the distribution of CbCaV1/CbCaV2 channels in the cardiac ganglion. The 19-amino acid residue epitope against which the primary antibody was raised is a 100% amino acid identity match to CbCaV1 and matches 17 of 19 amino acids in CbCaV2 (Figure 7; see also Figure 1C). No similarity of the epitope to CbCaV3 or full length LCaV3 was detected via BLASTP comparison.

LC somata and their projections are stereotypically distributed and clearly identifiable in this preparation (see Figure 1C), making rudimentary subcellular localization fairly straightforward. We found clear punctate staining localized to the LC somata and to a lesser degree staining in the neurites extending from the LC somata (Figure 7). In all, 9 whole mount cardiac ganglion preparations were stained, and in each preparation we were able to detect punctate staining localized to the LC somata. Additionally, we often detected staining in the processes of the anterior branch point of the ganglion (Figure 7C), where synaptic connectivity seems to be most prevalent amongst the cells of the *C. borealis* cardiac ganglion. We performed additional DAPI staining within these preparations to determine whether the punctate immunoreactivity on the somata may be the result of glia or other support cells positively staining. Immunofluorescence + DAPI overlays showed no evidence of overlapping fluorescence to indicate this was the case (e.g. see Figure 7D2). We also performed secondary antibody-only incubations that showed no significant fluorescence indicative of non-specific signal attributable to the secondary antibody. Finally, pre-absorption of the primary antibody with the antigen peptide eliminated immunolabeling as well.

## Discussion

The crustacean LC is a valuable model for studying motor neuron burst organization. The robust nature of the LC somata in electrophysiology experiments and segregation from action potential conductances as well as other network components

make these cells ideal in experiments (Hartline, 1967b, Cooke, 2002b). However, a detailed understanding of the ionic conductances and their underlying ion channels, particularly depolarizing conductances, is lacking in these cells. Here we report the results of sequence from three voltage-gated calcium channel alpha-subunit genes in the crab, *Cancer borealis*, and then characterize their expression as well as the depolarizing currents present in LC motor neurons of the cardiac ganglion. While we detect mRNA for three different channel types in individual LCs, we measured and can distinguish only two distinct voltage-activated calcium currents in LC somata. We additionally identified a calcium-activated nonspecific cationic current (CAN) as well as a TTX sensitive persistent inward current in these cells. Finally, we performed immunostaining that demonstrates the high voltage-activated calcium channels described are at least partially localized to the LC somata.

Sequence analysis reveals that the three calcium channel alpha subunits in this study, namely CbCaV1, CbCaV2, and CbCaV3, correspond very closely to identified calcium channel subunits of the snail, *L. stagnalis* (LCaV1, LCav2, and LCaV3) respectively. Thorough sequence and expression analyses of these snail channels have been performed, and the resulting current properties and kinetics of each channel reported (Spafford et al., 2003, Spafford et al., 2006, Senatore and Spafford, 2010). Based on the extensive similarities between these expressed snail currents and the native crab currents characterized in our study, we are confident that we can use this analysis to infer the identity of these channels and currents. The characteristics of crab LC  $I_{CaS}$ , a slowly inactivating high-voltage activated calcium current, are very similar to the current carried

by the LCaV1 channel(Spafford et al., 2006), which has been classified as an invertebrate L-type calcium channel and current. Therefore, based on the similarities in sequence between CbCaV1 and LCaV1, and the similarities between crab  $I_{CaS}$  and current carried by LCaV1, we suggest that CbCaV1 encodes an L-type calcium current with the properties described here as the slow calcium current,  $I_{CaS}$ . Similarly, the characteristics of crab  $I_{CaT}$ , a transient inactivating high-voltage activated calcium current, are very similar to the current carried by the LCaV2 channel(Spafford et al., 2003), which has been classified as an invertebrate calcium channel with biophysical characteristics found in mammalian P/Q and N-type channels. Based on the similarities in sequence between CbCaV2 and LCaV2, and the similarities between crab  $I_{CaT}$  and current carried by LCaV2, we suggest that CbCaV2 encodes a P/Q-type calcium current with the properties described here as the transient calcium current  $I_{CaT}$ .

The two voltage gated calcium currents ( $I_{CaS}$  and  $I_{CaT}$ ) both were present in experiments where the LC soma was isolated, indicating that these channels are present in the LC somata. This result is supported by immunohistochemistry experiments where high voltage activated calcium channel antibody was used to stain entire CG, resulting in immunostaining largely localized to the LC soma, although some staining also could be seen on neuronal processes in different regions of the ganglia. These results are also consistent with previous immunolocalization of calcium channel subunits in the lobster stomatogastric ganglion; Ca1A (P/Q-type) and Ca1D (L-type) immunoreactivity both were localized to STG somata, as well as primary neurites (French et al. 2002).

Calcium currents previously have been studied in crustacean motor neurons, particularly in the STG. Total calcium current has been characterized in STG neurons of two species of lobster (Turrigiano et al. 1995; Zhang and H-W 1995; Johnson et al. 2003), as well as crab (Golowasch and Marder 1992; Hurley and Graubard 1998). However, across these studies there are species and cell-specific differences in the calcium current types reported. For example, Hurley and Graubard (1998) specifically searched for, but failed to find, two distinct calcium currents with differing kinetics in the somata of STG neurons of the crab, *Cancer productus*. However, Turrigiano et al. (1995) measured calcium currents in isolated STG neurons of the lobster *Panulirus interruptus* in culture and noted both transient and persistent components to these currents, ultimately deciding to model calcium current in these cells as two separate components. Much of these discrepancies also may be explained by the fact that these inward currents have been, and continue to be, difficult to characterize in voltage clamp (Golowasch and Marder 1992; Turrigiano et al. 1995). Here, with the additional insight of molecular biology and a scaffolding of comparison provided by work in *L. stagnalis*, we believe we have made substantial progress toward a better understanding of these complex native currents in crustacean motor neurons.

Beyond the voltage-activated calcium currents, LCs also possess a calcium-activated inward current represented by the CAN current. The calcium activated non-specific cationic current is found in a variety of excitable cell types (Partridge and Swandulla, 1988) but is often implicated in neuronal bursting (Swandulla and Lux, 1985, Wilson et al., 1998, Rubin et al., 2009). This current in invertebrates has been best

characterized in crab STG (dorsal gastric) neurons. In these cells, the current is important in coordinating bistability of output; voltage-gated calcium currents allow calcium influx which activates  $I_{CAN}$ , inducing plateau potentials indicative of the output of these cells (Zhang and Harris-Warrick, 1995, Zhang et al., 1995). LC motor neurons of the cardiac ganglion do not undergo plateau potentials during normal network output, so this is unlikely the role of this current in the cardiac output. While we do not yet know the role of  $I_{CAN}$  in the cardiac motor neurons, a model for similar rhythm generation in mammalian pre-Bötzinger complex invokes CAN current as vital in triggering network-wide bursts after recurrent synaptic excitation - a role which may have parallels to CAN current in LCs (Del Negro and Hayes, 2008).

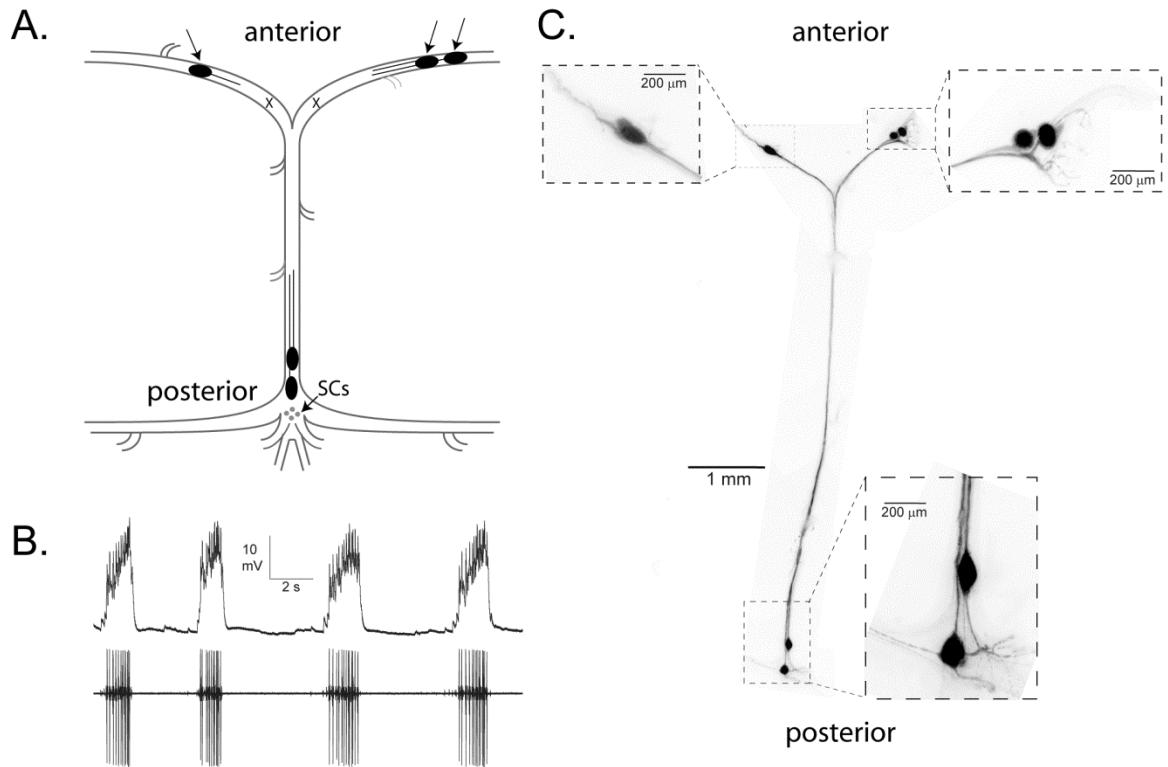
Finally, we also report for the first time in crab LCs a largely non-inactivating TTX sensitive current, that is necessary for driver potential generation in these cells, which could indicate the presence of a persistent sodium current ( $I_{NaP}$ ).  $I_{NaP}$  currents are often implicated in burst potential generation. In mammalian pre-Bötzinger neurons,  $I_{NaP}$  presence is known to be important in burst generation and its relationship with leak conductances is thought to dictate whether the neuron spontaneously bursts or requires excitatory input (Del Negro et al., 2002a, Del Negro et al., 2002b). There is evidence that DG neurons of the STG contain  $I_{NaP}$  important to plateau potential generation (Elson and Selverston, 1997) and a TTX sensitive persistent current has been voltage clamped in cultured STG cells (Turrigiano et al., 1995). While there is no channel gene known to directly mediate this current, indeed there is only one voltage gated sodium channel known in invertebrates (Loughney et al., 1989, Olson et al., 2008), there is the possibility

that the  $I_{NaP}$  current is mediated by the same channel population as the fast inactivating sodium current as seen in rat tuberomammillary neurons (Taddese and Bean, 2002). However, because there are no spike-mediating sodium currents in these crustacean motor neuron somata (Golowasch et al. 1992), it seems unlikely that these persistent sodium currents represent a window in fast-spiking sodium currents. Rather, it seems more likely that a distinct channel isoform could mediate these currents, perhaps as a result of a splice variant (Lin et al., 2009) or RNA editing event (Liu et al., 2004) of the previously identified CbNaV channel (Dai et al., 2010).

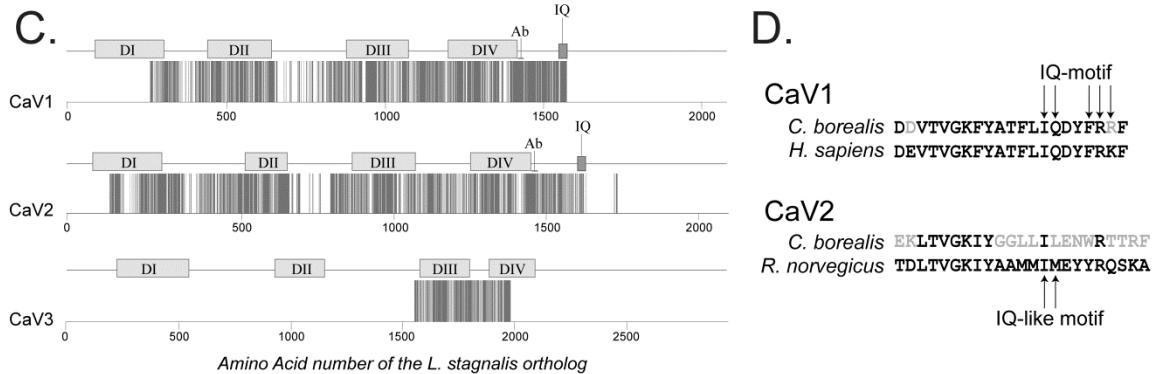
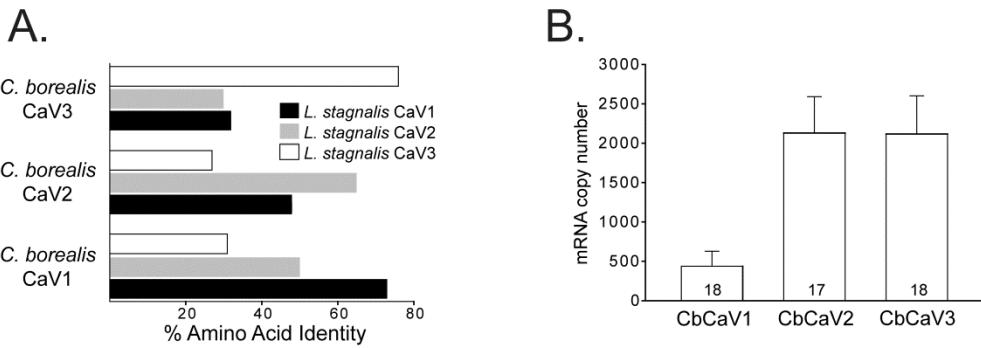
The specific roles of the inward currents in these cells, especially those which are calcium-mediated, are still to be experimentally determined. The crustacean cardiac motor neurons share extensive similarities with other excitatory central pattern generator circuits. For example, over 90% of rat pre-Bötzinger complex neurons elicit burst potentials only when driven by excitation; and like LC motor neurons these neurons also express  $I_{CAN}$ ,  $I_{NaP}$ , and intrinsic calcium currents (Del Negro et al., 2002b, Pena et al., 2004, Morgado-Valle et al., 2008). Whether the CG network LC burst potential is a result of summed EPSPs or requires some or all of these intrinsic inward components to generate its intrinsic burst potential is currently under investigation (Ball et al., 2010a, Franklin et al., 2010).

The depolarizing components found in the LC bursting neurons are prevalent across animal phyla especially in those neurons which are also bursters. The experimental advantages of the crustacean CG and the simplicity of the network make it an ideal

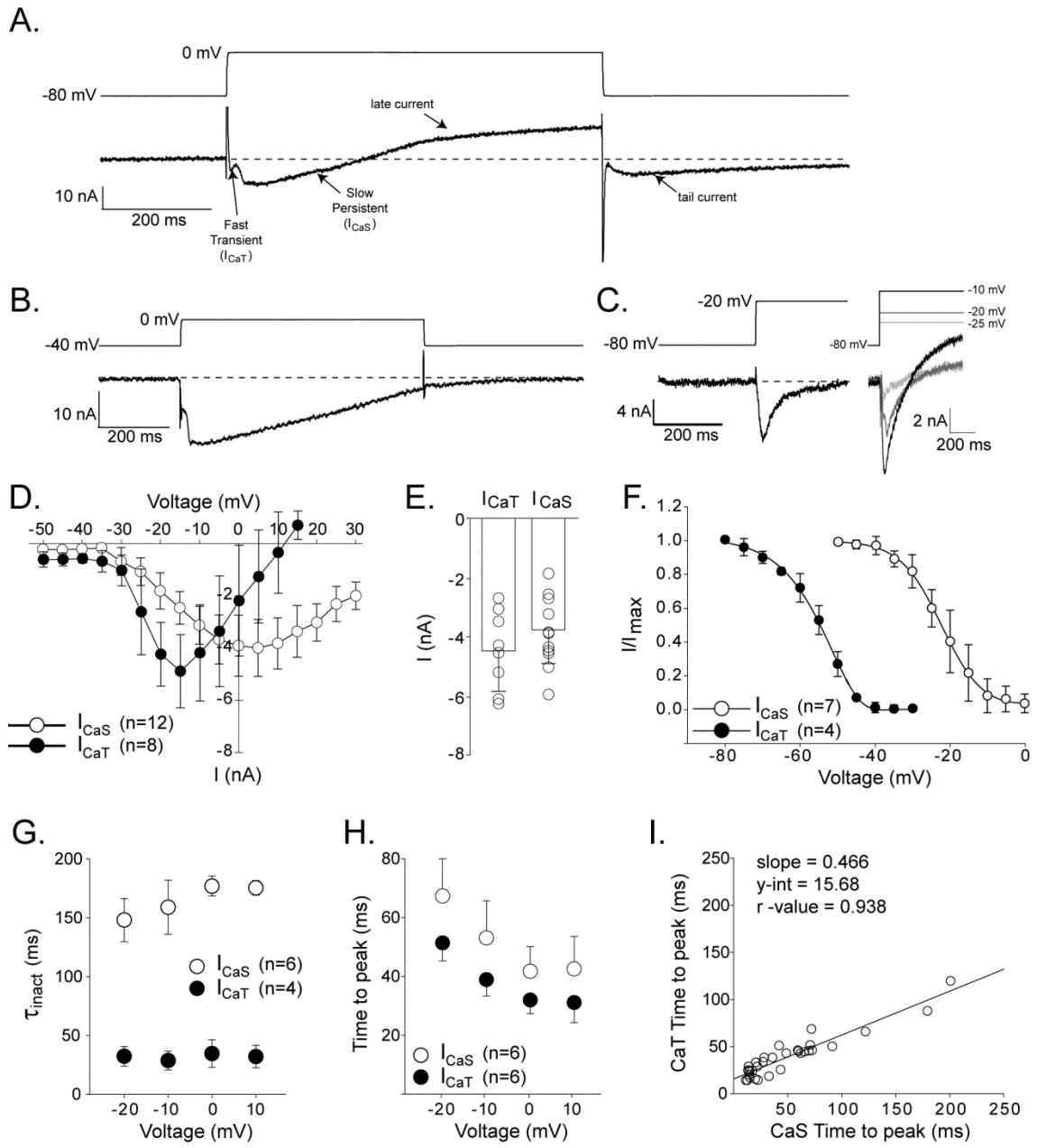
system to study how these components interact with each other and other network characteristics to shape and maintain output. In characterizing the inward components of *C. borealis* LC motor neuron, we obtain critical information to now move forward in investigating how the LC intrinsic components function within the rest of the cardiac network, and how this model can be applied broadly to understand neural network function in general.



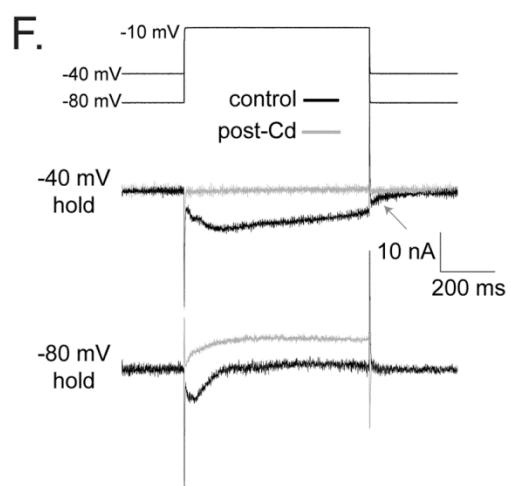
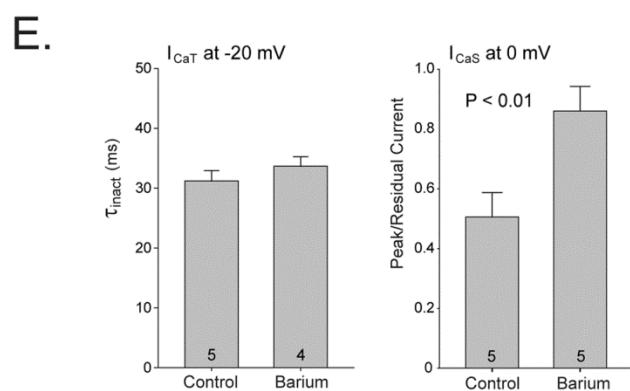
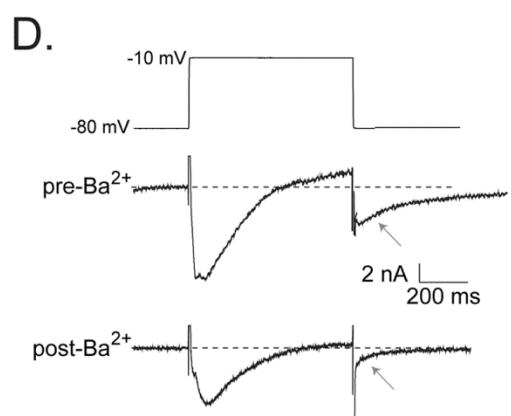
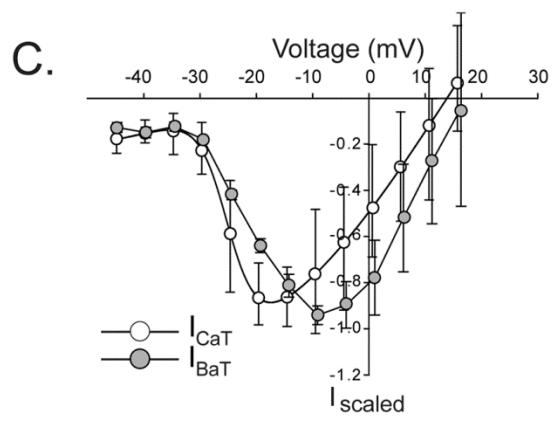
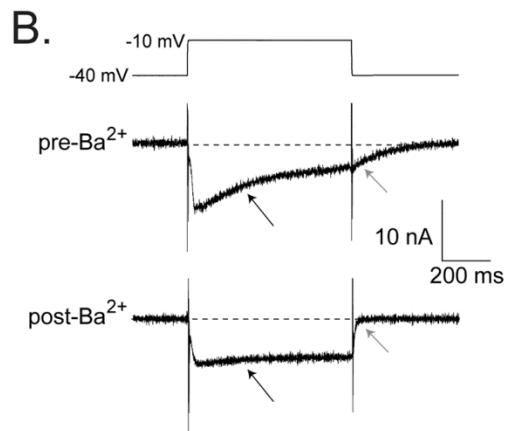
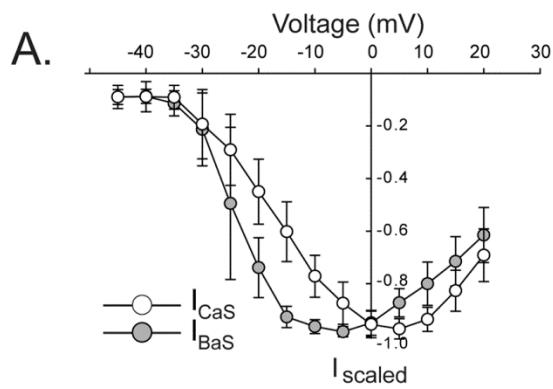
**FIGURE 1.1** The crustacean cardiac ganglion as a model system. **A.** Schematic showing the location of the 5 LC motor neurons (black ovals), with the anterior cells used in this study marked with black arrows. The somata of these anterior large cells were isolated from the remainder of the ganglion via thread ligatures placed at the branch points labeled by “X”. Small cell (SC) pacemakers are indicated as well. **B.** Electrophysiological recording showing the endogenous network activity, with a simultaneous intracellular recording of a LC3 motor neuron (top trace) with an extracellular recording of the entire network output (bottom trace). **C.** Dye fills (AlexaFluor 568) of the 5 LC motor neurons of an intact cardiac ganglion, showing the relative locations as well as clarity with which LC somata can be identified visually.



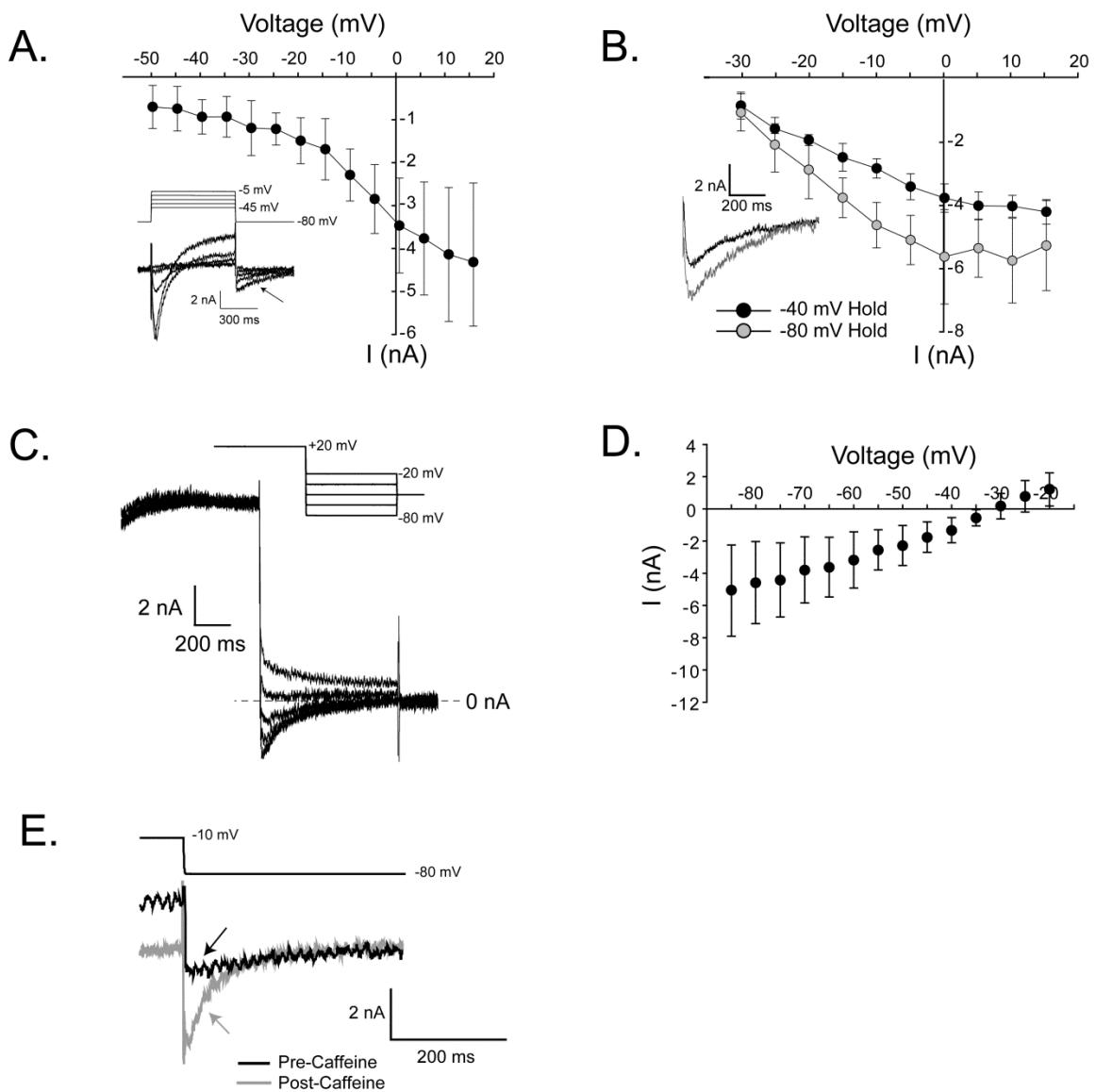
**FIGURE 1.2 Sequencing of voltage-gated calcium channel alpha subunits from *Cancer borealis*.** **A.** Percent amino acid identity for sequence obtained of putative CbCaV channel genes and their orthologs in the snail, *Lymnaea stagnalis*. **B.** Mean ( $\pm$  SD) single LC copy number for CbCaV1, CbCaV2, and CbCaV3 mRNAs. Samples sizes as shown in each bar. **C.** Graphical amino acid alignment between full-length *L. stagnalis* protein sequence for each voltage-gated calcium channel subtype (amino acid position represented by the x-axes) and the corresponding portion identified in *C. borealis*. Identical amino acids, as quantified in Fig 2A, are denoted with a vertical bar at each amino acid position along the x-axis. Putative transmembrane domains (DI – DIV), the IQ-binding domain (IQ), and the epitope to which the primary antibody was made (Ab) are denoted above each channel sequence. **D.** Amino acid alignments of the IQ- and IQ-like binding domains of CbCaV1 and CbCav2 with human (Accession: 2BE6\_D) and rat (Accession: NP\_037050.2) orthologs respectively. Gray residues indicate differences in the crab sequence relative to mammal sequence. Arrows denote key residues identified in modulating properties of these channels with respect to calcium-dependent inactivation in mammalian systems (described in text). **E.** Sequence alignments of the pore-forming loops of consensus mammalian sequence from alpha subunits for Cav2.1, Cav1.2, and Cav3.2 with the corresponding *C. borealis* ortholog. Gray boxes highlight the position of EEEE (HVA channels) or EEDD loci (LVA channels) in each domain of the channel subunit that confer divalent cation selectivity. Sequence from CbCaV3 (inset box) was sufficient only for comparison of Domain III.



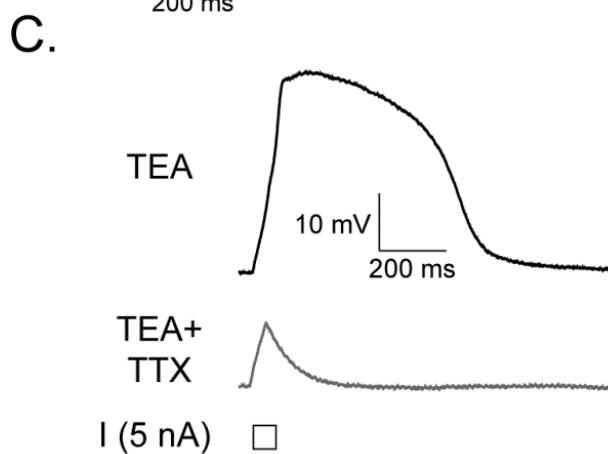
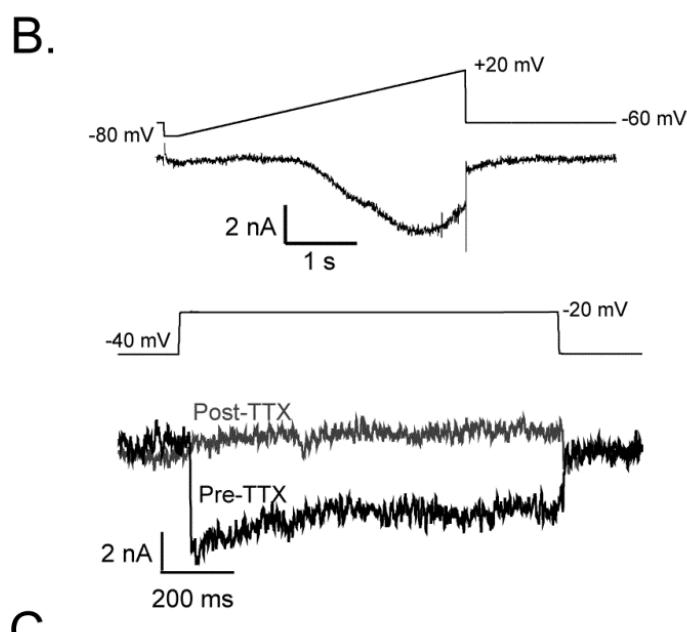
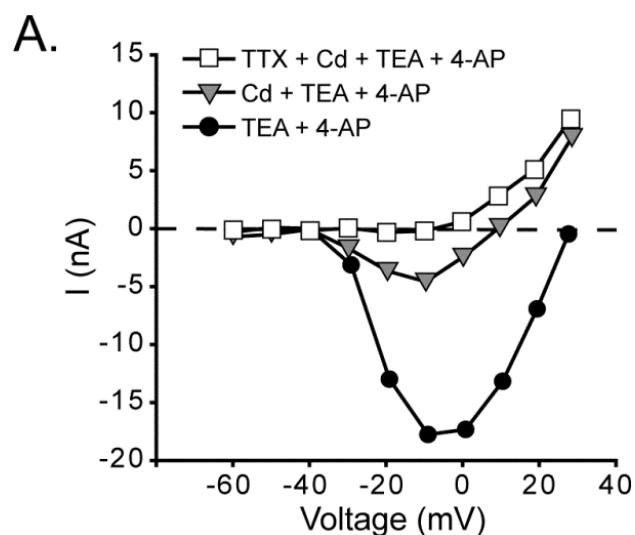
**FIGURE 1.3 Properties of voltage-gated calcium currents in LC motor neurons.** **A.** Raw trace of total current elicited at 0 mV from a holding potential of -80 mV in saline containing TEA, 4-AP, and TTX. Four distinct aspects of the total current are labeled, including a “transient” inward ( $I_{CaT}$ ), “slow”-inactivating inward ( $I_{Cas}$ ), late outward (late current), and an inward tail current (tail current). The voltage trace used to elicit the current trace is shown above the current recording. **B.** Typical recording of  $I_{Cas}$  at 0 mV from a holding potential of -40 mV in saline containing TEA, 4-AP, TTX and  $Cs^+$  loaded to reduce  $K^+$  currents to the minimum possible. The voltage trace used to elicit the current is shown above the current recording. **C.** Representative recording of  $I_{CaT}$  at -20 mV from a holding potential of -80 mV in saline containing TEA, 4-AP, TTX and  $Cs^+$  loaded to reduce  $K^+$  currents to the minimum possible. The voltage trace used to elicit the current is shown above the current recording. -20 mV allowed us the best recordings of  $I_{CaT}$  with a minimal contamination of  $I_{Cas}$ , as the current shown is the result of a subtraction of current elicited from holding potential of -40 mV (i.e.  $I_{Cas}$ ) from the current elicited from a holding potential of -80 mV ( $I_{Cas} + I_{CaT}$ ). We also provide representative traces of voltage-dependent activation of this current at -25 mV, -20 mV, and -10 mV. **D.** The mean ( $\pm SD$ ) I-V relationship for  $I_{Cas}$  and  $I_{CaT}$  indicating the voltage dependence of activation. **E.** Mean ( $\pm SD$ ) current levels for  $I_{Cas}$  and  $I_{CaT}$  across LC motor neurons. Individual points represent one cell. These data are from the same cells used to generate the I-V curves in Fig. 3D (N's as described).  $I_{Cas}$  measurements were taken at 0 mV, while  $I_{CaT}$  at -20 mV. **F.** Mean ( $\pm SD$ ) I-V relationships for voltage dependence of inactivation of  $I_{Cas}$  and  $I_{CaT}$  as shown by normalized currents measured at 0 mV and -20 mV respectively, from a varying holding potential plotted on the X-axis. **G.** Mean ( $\pm SD$ ) time constant of inactivation of  $I_{Cas}$  and  $I_{CaT}$  as a function of voltage. **H.** Mean ( $\pm SD$ ) time to peak current of  $I_{Cas}$  and  $I_{CaT}$  as a function of voltage. **I.** Correlation of time to peak current of  $I_{Cas}$  and  $I_{CaT}$  across voltages from -20 to +10 mV (data are from cells used in Figure 2H). R-value is the result of a Pearson correlation test.



**FIGURE 1.4 Barium currents in LC motor neurons.** **A.** The mean ( $\pm$  SD)  $I_{\text{scaled}}$  -V relationship for  $I_{\text{Cas}}$  ( $N = 8$ ) and the corresponding current in barium substituted saline ( $N = 4$ ). Because post- $\text{Ba}^{2+}$  currents often varied much greater in magnitude relative to native  $\text{Ca}^{2+}$  currents, we plotted normalized currents to allow direct comparison of activation characteristics. Scaled currents are normalized relative to the peak current in each cell by dividing  $I_{\text{Ca}}$  or  $I_{\text{Ba}}$  at a given voltage by the absolute value of  $I_{\text{peak}}$  for each cell. **B.** Typical recordings of  $I_{\text{Cas}}$  at -10 mV from a holding potential of -40 mV before (pre- $\text{Ba}^{2+}$ ; top trace) and after (post- $\text{Ba}^{2+}$ ; bottom trace) barium substitution. *Black* arrows show the apparent loss or decrease of inactivation in this current after barium substitution, *gray* arrows show the loss of tail current after barium substitution. **C.** The mean ( $\pm$  SD)  $I_{\text{scaled}}$  -V relationship for  $I_{\text{CaT}}$  and the corresponding current in barium substituted saline ( $N = 5$  for both). Currents were scaled as in panel A. **D.** Typical recordings of  $I_{\text{CaT}}$  at -10 mV from a holding potential of -80 mV before (pre- $\text{Ba}^{2+}$ ; top trace) and after (post- $\text{Ba}^{2+}$ ; bottom trace) barium substitution. *Gray* arrows again show the loss of tail current after barium substitution. **E.** Quantification (mean  $\pm$  SD) of changes in inactivation time constant for  $I_{\text{CaT}}$  (*left*) and the ratio of peak to residual  $I_{\text{Cas}}$  (*right*) following barium substitution. Sample sizes as indicated in each bar. Significant differences are reported for the results of a paired t-test. **F.** Effects of cadmium chloride on  $I_{\text{Cas}}$  and  $I_{\text{CaT}}$ . All four traces taken from the same cell before and after cadmium exposure. -40 mV hold traces are unsubtracted. -80 mV traces represent the difference current before and after cadmium, as obtained by subtracting the current from the -40 mV hold from the -80 mV hold to get the difference current. One representative cell is shown, but this experiment was performed  $N = 4$  times. *Gray* arrow shows the loss of tail current after cadmium substitution.

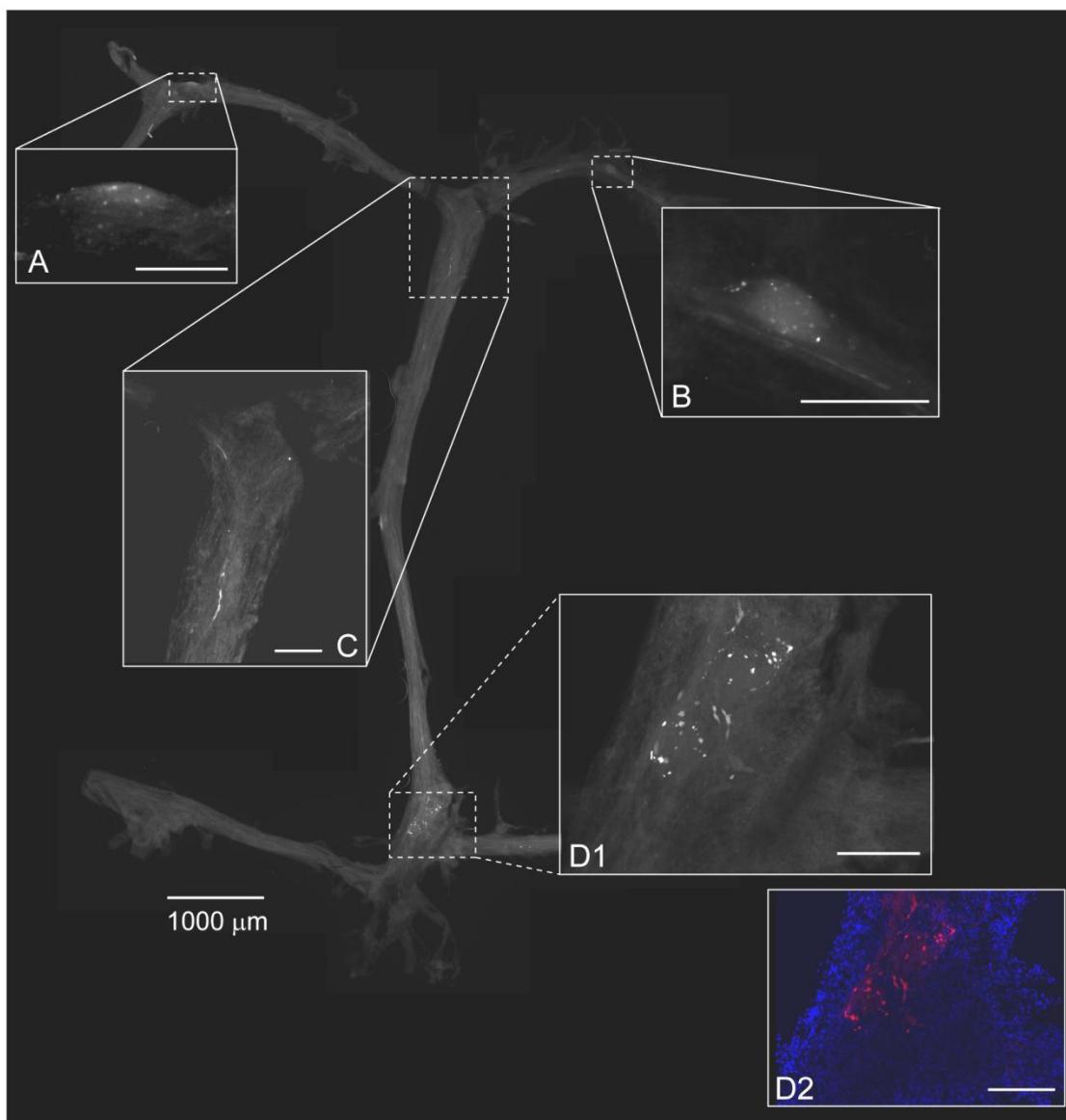


**FIGURE 1.5 Properties of calcium activated nonselective cationic current (CAN) in LC motor neurons.** Recordings were made in saline containing TEA, 4-AP, TTX, and cells loaded with  $\text{Cs}^+$ . **A.** Mean ( $\pm\text{SD}$ ) I-V relationships for activation of  $I_{\text{CAN}}$  measured at -80 mV from a varying depolarizing pulse potential (x-axis) to elicit calcium currents (holding potential of -80 mV,  $N = 5$ ). *Inset:* Typical recordings of the total current, including tail current (black arrow) elicited from these voltage protocols. **B.** Mean ( $\pm\text{SD}$ ) I-V relationships for activation of  $I_{\text{CAN}}$  from holding potentials of -40 mV (black circles) activating predominantly  $I_{\text{Cas}}$  or -80 mV (gray circles) which activates both  $I_{\text{Cas}}$  and  $I_{\text{CaT}}$  ( $N = 3$ ) *Inset:* representative tail currents in the same cell elicited from a holding potential of -40 mV (black trace) or -80 mV (gray trace). **C.** Typical recordings used to measure the reversal potential of tail current. Current traces were obtained by depolarizing the LC neuron from a holding potential of -50 mV to +20 mV and then measuring tail currents at varying tail holding potentials from -80 mV to -20 mV (as shown in the voltage traces). **D.** Mean ( $\pm\text{SD}$ ) I-V relationships used to interpolate the reversal potential (dotted line) of these tail currents ( $N = 8$ ). **E.** Caffeine-evoked increase in tail current amplitude in LCs. Recording of tail currents from a holding potential of -80 mV before (black trace/arrow) and after (gray trace/arrow) bath application of 10 mM caffeine (this experiment was performed  $N = 4$  times).



**FIGURE 1.6 TTX-sensitive persistent current in LC motor neurons.** **A.** I-V relationship in a LC motor neuron indicating the presence of a TTX-sensitive current. Inward currents were measured from a holding potential of -40 mV at depolarizing voltage steps under subsequent blocker conditions. Currents first were elicited in TEA + 4-AP (black circles), then Cd<sup>2+</sup> was added to block calcium currents (gray triangles), revealing a residual inward current that was subsequently blocked with TTX (white squares). **B.** Representative recording of TTX-sensitive current elicited in saline containing TEA, 4-AP, and Cd<sup>2+</sup> with a -80 mV to +20 mV voltage ramp, and then subtracted from this current was the same voltage ramp with the addition of TTX (top trace) N = 3. Step depolarizations also reveal a persistent TTX sensitive inward current. *Gray trace*- inward current in the presence of CdCl<sub>2</sub>; *black trace*- current after the addition of 10<sup>-6</sup>M TTX (bottom trace) N = 4. **C.** TTX-sensitive current is necessary for burst potential generation in LC motor neurons. Exaggerated driver potentials are elicited in 50 mM TEA and a short depolarizing current injection (5 nA, 50 ms; top trace). These driver potentials are eliminated in the presence of TTX, even though calcium currents remain intact (bottom trace) N = 6.

Anti-Ca(v) Pan- $\alpha$ 1 DNF DYLTRDWSILGPHHLD  
*CbCaV1* DNF DYLTRDWSILGPHHLD  
*CbCaV2* DNF DYLTRDSSILGAHHLD



**FIGURE 1.7 High-voltage activated calcium channels (HVACC) are localized to the somata of LC motor neurons.** We used an Anti-CaV Pan- $\alpha$ 1 primary antibody to detect putative HVACC immunoreactivity in the cardiac ganglion. The alignment of the antibody epitope with the corresponding amino acid sequence in CbCaV1 and CbCaV2 is shown at the top of the figure. The entire cardiac ganglion is shown based on assembled tiled images taken at 4x magnification. Insets are magnified images of the corresponding portion of the ganglion marked with dashed boxes. We detected immunoreactivity for HVA calcium channels in the somata of all five LC motor neurons. A and B. HVACC immunoreactivity in anterior LCs appears to be localized to the somata, consistent with the ability to measure these currents in isolated LC somata. C. Immunoreactivity was also detected in processes of neurons in the cardiac ganglion, particularly in the anterior branch point. D1. The paired posterior LC neurons also showed immunoreactivity apparently localized to the somata, which (D2) is not the result of glial or support cell staining as revealed by co-localization of immunoreactivity (RED) and DAPI counter stain (BLUE). Scale bars in insets all represent 200  $\mu$ m.

## CHAPTER TWO

### **Rapid homeostatic plasticity of intrinsic excitability in a central pattern generator network stabilizes functional neural network output**

Neurons and networks undergo a process of homeostatic plasticity that stabilizes output by integrating activity levels with network and cellular properties to counter longer-term perturbations. Here we describe a rapid compensatory interaction among a pair of potassium currents,  $I_A$  and  $I_{KCa}$ , that stabilizes both intrinsic excitability and network function in the cardiac ganglion of the crab, *Cancer borealis*. We determined that mRNA levels in single identified neurons for the channels which encode  $I_A$  and  $I_{KCa}$  are positively correlated, yet the ionic currents themselves are negatively correlated, across a population of motor neurons. We then determined that these currents are functionally coupled; decreasing levels of either current within a neuron causes a rapid increase in the other. This functional interdependence results in homeostatic stabilization of both the individual neuronal and the network output. Furthermore, these compensatory increases are mechanistically independent, suggesting robustness in the maintenance of neural network output that is critical for survival. Taken together, we

generate a complete model for homeostatic plasticity from mRNA to network output where rapid post-translational compensatory mechanisms acting on a reservoir of channels proteins regulated at the level of gene expression provide homeostatic stabilization of both cellular and network activity.

The balance of plasticity and stability in generating appropriate output is a matter of fundamental importance in the nervous system across all functional levels. These processes occur even at the most fundamental level, the excitability of individual neurons, and yet little is known about mechanisms governing these processes (Marder, 2011b, Turrigiano, 2011b). Early work identified such processes of “homeostatic plasticity” of intrinsic excitability (LeMasson et al., 1993, Turrigiano et al., 1994, Turrigiano et al., 1995, Golowasch et al., 1999), but subsequent focus more intensely shifted to determining how stabilization of synapses is accomplished through synaptic scaling (Turrigiano, 2012). Recently, a resurgence of interest in plasticity of intrinsic excitability has accompanied work on synaptic scaling (Debanne and Poo, 2010, Misonou, 2010, Turrigiano, 2011b).

Fewer studies on homeostatic plasticity have considered functional compensation in the context of endogenous network activity. The most dramatic example may be complete recovery of motor network output following loss of central inputs as a result of changes in conductances in the crustacean stomatogastric ganglion (STG) (Thoby-Brisson and Simmers, 1998, 2002). Knockouts of K<sup>+</sup> channels in mice have been shown to have modest effects on phenotype and cellular output as a result of compensation by

other K<sup>+</sup> channels (Guo et al., 2005, Nerbonne et al., 2008). Additionally, overexpression of A-type K<sup>+</sup> channels in STG neurons results in little change in neuronal output as a result of compensatory increases in H-current (MacLean et al., 2003, MacLean et al., 2005). However, these examples feature mechanisms that act over longer time scales of days to weeks. While initial reports of plasticity in intrinsic excitability were found over shorter time scales (Desai et al., 1999, Golowasch et al., 1999), surprisingly little is known of the role these mechanisms may play in short-term ongoing activity of biologically intact networks, specifically where an expectation for rapid conservation of output could be argued, such as in central pattern generators (CPGs).

Compensation in CPG circuits may be inferred from the fact that normal populations of unmanipulated motor neurons of two invertebrate CPGs, the cardiac and stomatogastric ganglia, show correlations in expression levels of mRNAs for ion channels (Schulz et al., 2007a, Tobin et al., 2009) and membrane conductances (Khorkova and Golowasch, 2007, Temporal et al., 2012). One relationship detected in previous work (Tobin et al., 2009) is a positive correlation between *BKKCa* and *shaker* mRNA levels in neurons of the cardiac ganglion. These channels encode calcium-activated and A-type K<sup>+</sup> currents, respectively. However, it is unclear how a neuron would use two similar hyperpolarizing conductances additively to generate or maintain its output. In this study we focused on elucidating the functional relationship between these two conductances in motor neurons of the crab cardiac ganglion. We discovered a striking discrepancy in the relationship of these channels across functional levels: mRNAs for these channels were *positively* correlated, while their conductances were

*negatively* correlated. Therefore, we propose a comprehensive hypothesis for plasticity of excitability from mRNA to network output whereby rapid compensation provides stabilization of cellular and network activity.

## MATERIALS AND METHODS

### Animals

*Cancer borealis* crabs of either sex were purchased and shipped overnight from The Fresh Lobster Company (Gloucester, MA). Crabs were kept between 24 hours and two weeks in artificial sea water at 12 °C before use. Crabs were anesthetized in ice for 15 minutes prior to the dissection. The dissection took place in chilled physiological saline comprised of 440 mM NaCl, 26 mM MgCl<sub>2</sub>, 13 mM CaCl<sub>2</sub>, 11.2 mM Trizma base, 11 mM KCl, and 5 mM Maleic acid (pH = 7.4). When we wanted to isolate individual large cells, individual strands of bulking nylon were used to ligate the nerve on both sides of a large cell soma. To impale large cells, each cell was individually desheathed using a tungsten needle (Fine Science Tools, Foster City CA).

### Quantitative single-cell RT-PCR

Quantitative RT-PCR was performed as previously described (Schulz et al., 2006a; Tobin et al., 2009). Primers specific for real-time PCR detection of *shal*, *BKKCa*, *shab*, and *shaker* using Sybr Green were developed and designed using Primer3 software

and are the same as previously reported (Schulz et al., 2006a; Tobin et al., 2009). Briefly, total RNA was isolated using RNeasy micro column based RNA extraction kit (Qiagen, Valencia, CA), reverse transcribed using SuperScript III reverse transcriptase (Invitrogen), and used as a template in real-time RT-PCR with Sybr Green (SABiosciences, Frederick, MA) in a RotorGene 3000 real-time PCR machine (Corbett Research, Australia). Previous studies have determined that in LC motor neurons, correlations can be equally well detected among channel mRNA levels with and without normalization of real-time results to 18S rRNA (Tobin et al., 2009). Values reported here are total copy numbers from a single neuron, and are not normalized with respect to 18S levels.

## **Pharmacology**

Pharmacological blockers were dissolved in physiological saline and perfused onto the cardiac ganglion using a Rabbit peristaltic pump (Rainin Instruments Company, Oakland, CA) at a rate of 1.5 mL / min or added to the preparation from a stock solution via pipette. The following pharmacological agents were used: tetraethylammonium dissolved in saline at 25mM, 4-aminopyridine dissolved in saline at 1mM, cadmium chloride dissolved in saline at 250 $\mu$ M (Acros Organics, Geel, Belgium), tetrodotoxin dissolved in saline at 1 $\mu$ M (Alomone Labs, Jerusalem, Israel), BAPTA-AM dissolved DMSO and applied at 30 $\mu$ M in saline, ryanodine dissolved DMSO and applied at 100 $\mu$ M in saline, staurosporine dissolved in DMSO and applied at 5 $\mu$ M in saline, okadaic acid dissolved in DMSO and applied at 500nM in saline (Ascent Scientific; Cambridge, MA),

cyclosporine A dissolved in DMSO and applied at 2 $\mu$ M in saline (Tocris Biosciences, Minneapolis, MN). All DMSO applications resulted in a final concentration of DMSO that was <1% (range: 0.000025% to 0.5%).

Pharmacological agents used to investigate intracellular mechanisms involved in the compensatory response (BAPTA-AM, ryanodine, okadaic acid, cyclosporine A, staurosporine) were applied to the cardiac ganglion 1 hour prior (2 hours prior with ryanodine) to the application of the blocker which caused the compensation (TEA or 4AP). A cell or preparation was exposed only to one channel blocker type (TEA or 4AP) for a given experiment.

### **Current Measurements**

All experiments were carried out in physiological saline cooled to 12°C. To measure current magnitudes and activation properties, two-electrode voltage clamp (TEVC) experiments were carried out by impaling a large cell with two glass electrodes filled with 3M KCl (8-17 M $\Omega$  resistance) and an Axoclamp 2A amplifier (Axon Instruments, Union City CA). All recordings were made from anterior large cell somata; action potential conductances were blocked (unless noted otherwise) by tightening thread ligatures on both sides of the large cell soma, preserving space clamp. TEVC protocols were created, driven and recorded with clampex 9.2 software (Axon Instruments, Union City CA). Current recordings were analyzed with Clampfit 9.2 software (Axon Instruments, Union City CA). Current and voltage traces were sometimes filtered with a

lowpass boxcar filter using 7 smoothing points. Most voltage clamps were modified from those used previously in STG preparations (Golowasch and Marder, 1992, Khorkova and Golowasch, 2007, Temporal et al., 2012). High threshold potassium current ( $I_{HTK}$ ) magnitude was measured using a leak subtracted TEVC protocol with a holding potential of -40mV and 16 voltage steps from -55mV to +20mV (5mV intervals). A-type potassium current ( $I_A$ ) magnitude was measured by subtracting the  $I_{HTK}$  current traces from a TEVC protocol that is identical except for a holding potential of -80mV. Calcium-activated potassium current ( $I_{KCa}$ ) was isolated by subtracting post-cadmium (250 $\mu$ M CdCl<sub>2</sub>, 1 hour)  $I_{HTK}$  current traces from pre-cadmium  $I_{HTK}$  current traces (isolating the cadmium sensitive outward current). Delayed rectifier potassium current ( $I_{Kd}$ ) was isolated using the  $I_{HTK}$  TEVC protocol after cadmium exposure (250 $\mu$ M CdCl<sub>2</sub>, 1 hour). All current magnitude measurements were taken at 0mV on an I-V plot made from the current traces.

### **Large Cell Excitability and Network Output**

Cardiac network output was monitored with a single intracellular recording (using same equipment as TEVC protocols) taken from one of the three anterior large cells and an extracellular differential recording made with a model 1700 A-M Systems AC amplifier (Sequim, WA) and two stainless steel wires; one placed inside and one outside a vaseline well located around the central nerve of the CG (see Figure 1). Pharmacological blockers (TEA or 4AP) were perfused on the entirety of the CG with the exception of the four small cell and two posterior large cell somata. These cells were

isolated from the perfusion by a vaseline well placed around these cells and the posterior branch point containing regular physiological saline (see Figure 1). Using this experimental configuration we monitored the effect of the LC compensatory response (isolated to the best of our ability from small cells) in the context of the functioning network. Network activity was recorded in 10 minute intervals before and during blocker perfusion. These recordings were analyzed using Spike2 v6.00 software (Cambridge Electronic Design Limited, Cambridge, UK).

LC intrinsic excitability was examined under similar conditions except  $10^{-6}$ M TTX saline was placed in the vaseline well around the four small cell and two posterior LC somata. This eliminated spontaneous network activity and small cell excitatory input into the anterior LCs. Excitability in the anterior LCs was then monitored using two-electrode current clamp (TECC) protocols run prior to and every five minutes after TEA or 4AP perfusion. TECC protocol was a six step depolarizing current injection (from 1-6nA) lasting six seconds per step and six seconds between steps.

## Statistics

All statistical tests were performed with SigmaPlot v11.0 (Systat, Aspire Software International, Ashburn, VA). All data were confirmed to be of normal distribution as required by statistical analyses employed. Relationships between channel mRNAs and ionic currents were analyzed using Pearson's correlation test, and coefficients of

determination were calculated from the resulting correlation coefficients. In the case of Figures 2C and 2D, a potential outlier was identified that could be anchoring a false positive for the Pearson's test (see arrows). Analyses on these data sets were carried out both with and without the data point in question and both results reported. Bonferroni corrections were employed for multiple comparisons in the correlation analyses, and the p-value adjusted to 0.017 for statistical significance (three comparisons each for mRNA and ionic currents). Changes in current magnitude before and after pharmacological block were analyzed in one of two ways. Raw currents were analyzed before and after blockade via paired *t*-tests, and these are reported in Figure 3. In Figure 5, significant changes in a current relative to baseline were expressed as a percent change from zero, and analyzed via one-sample *t*-test with the hypothesized population mean set to 0. Overall changes in burst duration, spikes per burst, and spike frequency within the burst reported in Figure 4 were analyzed as with repeated measures ANOVA.

## RESULTS

### **The crustacean cardiac ganglion as a model for central pattern generator network activity**

The rhythmic pumping of the heart in decapod crustaceans such as the crab, *Cancer borealis* (our model organism), is neurogenic in nature, and under the control of a simple central pattern generator network called the cardiac ganglion (Alexandrowicz,

1932) (see Fig. 1). The ganglion consists of only nine neurons: four ‘small cell’ interneurons (SCs) that generate the pacemaker activity and five ‘large cell’ motor neurons (LCs) that innervate the heart musculature (Hartline, 1967; Tazaki and Cooke, 1983c). The SCs of the cardiac ganglion are endogenous oscillators, i.e., they undergo spontaneous and rhythmic generation of a depolarizing wave of membrane potential that leads to a bursting phenotype of multiple spikes per burst (Tazaki and Cooke, 1983a, Cooke, 2002b). The LCs of the CG produce bursts of action potentials as a result of synaptic pacemaker input from the SCs, ultimately leading to muscle contraction (Hartline, 1967; Tazaki and Cooke, 1979, 1983c, a; Berlind, 1989). The behavioral output of the ganglion represents a direct correlation of the influence of LCs on heart muscle (Sakurai and Wilkens, 2003, Garcia-Crescioni et al., 2010), and thus a direct measure of heart activity. Yet the entire network can be dissected out intact, and maintained in physiological saline for extended periods of recording while continuing to produce its endogenous rhythmic output. The motor neurons are all individually identifiable, and due to their distributed nature within the ganglion (Fig. 1), we can perform pharmacological manipulations on one or multiple motor neurons, either in isolation or in the intact, functional network. (Tazaki and Cooke, 1983a; Cooke, 2002). The underlying burst potentials of the LCs represent functional output at the motor neuron level, and our preliminary modeling studies show how the simplicity of this model system can be used to study functional implications of the relationships between mRNAs and ionic conductances on cellular output (Ball et al., 2010; Franklin et al., 2010).

## **Relationship between $I_A$ and $I_{KCa}$ in a population of large cell motor neurons**

Potassium currents were measured using protocols developed for the STG cells of the same species (Golowasch and Marder, 1992). The total outward current of LC motor neurons consists primarily of three  $K^+$  currents (Fig. 2B; Golowasch and Marder 1992): A-type transient  $K^+$  current ( $I_A$ ), calcium-activated  $K^+$  current ( $I_{KCa}$ ), and delayed rectifier  $K^+$  current ( $I_{Kd}$ ).  $I_{KCa}$  and  $I_{Kd}$  can be found in one combined current trace elicited from holding potentials at -40 mV or higher, and is termed here as the high-threshold  $K^+$  current ( $I_{HTK}$ ), while the A-type current can be measured by subtracting  $I_{HTK}$  from the total outward current elicited from a holding potential of -80 mV.

We first examined the relationships among mRNA levels in single identified LC motor neurons for three channel genes that correspond to these three  $K^+$  currents (Atkinson et al., 1991, Tsunoda and Salkoff, 1995, Kim et al., 1998): *BKKCa* ( $I_{KCa}$ ), *shaker* ( $I_A$ ), and *shab* ( $I_{Kd}$ ). We detected a significant correlation between *BKKCa* and *shaker* mRNA levels across a population of 20 LC motor neurons (Fig. 2A; *left*), but no correlations among any other channel mRNAs (Fig. 2A; *middle* and *right*). A fourth channel mRNA encoding an A-type  $K^+$  current, *shal*, also was significantly positively correlated to *BKKCa* mRNA levels ( $P < 0.005$ ;  $R^2 = 0.58$ ), as well as to *shaker* ( $P < 0.002$ ;  $R^2 = 0.42$ ) but not to *shab*, suggesting an overall relationship between  $I_{KCa}$  and  $I_A$ , but not with  $I_{Kd}$ , in these cells.

We next examined the relationships among the ionic currents encoded by these channel genes across a population of LC motor neurons.  $I_A$ ,  $I_{KCa}$ , and  $I_{Kd}$  were all measured in each cell across a population of LC motor neurons. A similar pattern of correlated current levels was seen as with the mRNA with one striking distinction: only  $I_A$  and  $I_{KCa}$  showed a significant correlation (Fig. 2A), but the correlation was strongly *negative* as opposed to positive as seen in the mRNA measurements. No significant correlations were found between  $I_A$  and  $I_{Kd}$ , or  $I_{KCa}$  and  $I_{Kd}$  (Fig. 2A). Because of the striking difference between the mRNA correlation (positive), and the current correlation (negative), we were most interested in pursuing the relationship between  $I_A$  and  $I_{KCa}$ , but had concerns about the effects of pharmacological blockers used to measure  $I_{KCa}$  (see Fig 3F); we use  $Cd^{2+}$  to block calcium currents that evoke  $I_{KCa}$  in order to measure this current via subtraction from  $I_{HTK}$ , as we have not identified any blockers specific to  $I_{KCa}$  in our preparation despite many attempts. Therefore, we decided to use the peak  $I_{HTK}$  as an indicator of  $I_{KCa}$  abundance in these experiments.

$I_{HTK}$  (High Threshold  $K^+$ ) is known from previous work (Golowasch and Marder, 1992, Haedo and Golowasch, 2006, Khorkova and Golowasch, 2007) to, in large part, consist of  $I_{KCa}$ , particularly the transient portion, as  $I_{Kd}$  shows no transient peak that could account for the peak in  $I_{HTK}$  (see Figure 2B). We also determined that measurements of the peak  $I_{HTK}$  were likely sufficient to reveal the relationship between  $I_{KCa}$  and  $I_A$ , as the only transient peak seen in the currents that underlie  $I_{HTK}$  belongs to  $I_{KCa}$  (see Fig. 2B, *right*). Peak  $I_{HTK}$  also shows the same negative relationship with  $I_A$  as does  $I_{KCa}$  (Fig. 2C *left*), and peak  $I_{KCa}$  itself very strongly correlates with peak  $I_{HTK}$  (Fig. 2C *middle*), but not

$I_{Kd}$  (Fig 2C right). Accordingly, for the remainder of the study, we used  $I_{HTK}$  peak current from baseline as a measure of  $I_{KCa}$  abundance, to allow for measurement of all  $K^+$  currents under the least manipulative pharmacological blocker regime, i.e., without the need to block voltage-gated calcium currents.

### **$I_{KCa}$ and $I_A$ are rapidly up-regulated within the same LC motor neuron**

Because the focus of the study was on the negative relationship between  $I_A$  and  $I_{KCa}$ , we decided to repeat the initial measurements in a new population of LC motor neurons to confirm the original finding before examining the functional impact of this relationship. In a distinct population of 20 LC motor neurons, we once again found a strong negative relationship between  $I_A$  and  $I_{KCa}$  (as revealed by  $I_{HTK}$  measurements; Fig. 3A), confirming our original finding. This strongly suggested a causal relationship between  $I_A$  and  $I_{KCa}$ . Specifically, we hypothesized that if these two currents are functionally interrelated, then a decreased level of  $I_A$  should result in an increased level of  $I_{KCa}$  and vice versa. We tested this hypothesis by blocking one current in this pair and determining whether there was an effect on the magnitude of the other. We measured baseline levels of  $I_A$  in a given cell, then used tetraethylammonium (TEA) to block the HTK-current for 60 minutes, and then measured  $I_A$  again post-TEA. 60 minutes of exposure to TEA significantly increased peak ( $P < 0.001$ ; paired  $t$ -test) A-current (Fig 3B; 3C). The converse experiment was performed using 4-aminopyridine (4AP) for 60 minutes to block  $I_A$ . The peak ( $P < 0.003$ ) of  $I_{HTK}$  was significantly increased following 60 minutes of 4-AP blockade (Fig 3B; 3C). Additionally, these results appear to be due

to an overall increase in conductance, since no change was seen in the voltages of activation of  $I_A$  and  $I_{HTK}$  concomitant with the changes in total current as a result of the block experiments (Fig 3D). No consistent or significant effects of TEA and 4-AP on neuronal input resistance were observed in these cells ( $\Delta R_{IN}$  TEA:  $-1.87 \pm 2.5 \text{ M}\Omega$ ,  $\Delta R_{IN}$  4-AP:  $-0.52 \pm 1.7 \text{ M}\Omega$ ).

Our initial data strongly implicate  $I_{KCa}$  and  $I_A$  as the key pair of currents involved in this response. Since  $I_{HTK}$  is a mixed current comprised predominantly of  $I_{KCa}$  and  $I_{Kd}$ , and both of these currents are blocked by TEA, we determined whether the changes seen in  $I_{HTK}$  as a result of 4AP blockade were attributable to just one or to both of these currents. Most convincingly, while 4AP block significantly increases  $I_{HTK}$  (Fig 3C), one hour of exposure to 4AP had no significant effect on  $I_{Kd}$  magnitude itself (Fig 3E *left*). Unfortunately, we have not identified a blocker specific to  $I_{KCa}$  in our preparation to directly test the effects of blocking this current on changes in  $I_A$ . However, we can indirectly block  $I_{KCa}$  by using  $CdCl_2$  to block voltage-gated  $Ca^{2+}$  channels that trigger  $I_{KCa}$ . Blocking with  $Cd^{2+}$  completely eliminates  $I_{KCa}$  in these cells, and causes a significant increase in  $I_A$  after one hour of exposure that is very similar to that seen with TEA (Fig. 3E *right*). Taken together, these data strongly suggest that the relationship between  $I_A$  and  $I_{HTK}$  identified in the experiments (Fig. 3) are the result of a causal relationship between the levels of  $I_A$  and  $I_{KCa}$  in a given motor neuron.

**$I_A$  and  $I_{KCa}$  act in a compensatory fashion to stabilize cellular excitability and network output**

The negative correlation we measured between  $I_A$  and  $I_{KCa}$  in the normal population, together with the rapid change in currents seen within a cell after TEA and 4AP block, led us to hypothesize that levels of  $I_A$  and  $I_{KCa}$  may be acting in a compensatory fashion to stabilize both cellular and network output. To determine if such a functional compensation exists, we followed over time the activity of both isolated LCs, as well as LCs in an intact network, with either 4AP or TEA blockade, and then determined whether the output of the cells and of the network changed over the course of the blockade and the potential compensation.

As seen in Figures 4A and 4B, TEA blockade caused a substantial increase in the excitability of the LC motor neuron in the initial 10-20 minutes. However, over the time course of the measured increase in  $I_A$  seen in previous experiments (see Figure 2C) there was a compensatory change in the output of the cell and of the network towards the baseline level of activity. In isolated LCs (Figure 4A), both TEA and 4AP application shifted the cells from a less excitable state to a state characterized by large sustained burst potentials. However, over the time course of compensation, the excitability of isolated cells returned to control levels, losing the large burst potentials and showing firing patterns similar to those before the application of the blocker (Figure 4A).

In the intact network, TEA often caused a complex multi-phase bursting output in treated LCs (see Figure 4B; 10 min recording). Given this somewhat complex pattern of bursting, we determined that measurements of burst duration across a population of these

cells represented the clearest means to quantify changes in output over time. Over the course of 60-90 minutes, TEA blockade resulted in a significant change in burst duration ( $P < 0.01$ ; ANOVA; Figure 4C *left*), initially increasing to nearly twice as long as control before re-establishing a stable burst duration indistinguishable from that at the control level (Figure 4B).

In the companion experiment with 4AP blockade in the intact network, we see a similar effect of compensation as in the LC motor neuron output (seen in Figures 4B and 4C). 4AP block does not cause the same change in burst duration as with TEA. Rather, 4AP blockade initially causes a significant increase in spike frequency and the number of spikes fired per burst ( $P < 0.01$ ; ANOVA). Over the time course of the blockade, this spike frequency and number of spikes per burst returns to control levels (Figure 4D). These data indicate that the changes seen in the level of  $I_A$  and  $I_{KCa}$  as a result of TEA and 4AP block, respectively, are a functional compensatory response that stabilizes the output of the cells and of the network as a whole. However, the roles of  $I_A$  and  $I_{KCa}$  are not simply functionally redundant; blocking either current causes an initial change in the output of the cell that is not the same. These results implicate distinct roles for these two currents in addition to their ability to partially compensate for one another. However, we do not rule out the possibility that there could be other currents or mechanisms involved in the compensatory effect.

### **Compensatory changes in $I_A$ and $I_{KCa}$ follow distinct regulatory pathways**

We then set out to determine the underlying mechanisms implementing the compensation in these currents. We first investigated whether the change in  $I_{KCa}$  elicited by 4AP blockade was dependent on intracellular calcium. To check this, we co-applied the calcium chelator BAPTA with the blocker. When BAPTA was co-applied with 4AP, there was no change in  $I_{HTK}$ , in contrast to the characteristically significant increase in  $I_{HTK}$  with 4AP blockade (Figure 5A). We also confirmed that this effect was not simply due to an effect of BAPTA on the calcium-dependence of  $I_{KCa}$ ; BAPTA alone did not result in a significant reduction of  $I_{HTK}$  (data not shown; see also Turrigiano et al. 1994). More specifically, the calcium-dependence of the increase in  $I_{HTK}$  was attributable to the release from intracellular calcium stores since co-application of 4AP and the intracellular calcium release blocker ryanodine also prevented the compensatory increase in  $I_{HTK}$  normally seen with 4AP blockade (Figure 5A). These results suggest that the compensatory increase in  $I_{KCa}$  is dependent on intracellular calcium signaling mechanisms that depend on the release of intracellular calcium stores.

Because relatively rapid changes in current magnitude can often be attributed to changes in phosphorylation states of ion channels and associated regulatory proteins, we examined the effects of phosphatase and kinase inhibitors on the ability of the blockers to elicit the compensatory changes in these currents. Okadaic acid is a broad spectrum inhibitor of serine/threonine protein phosphatases (Cohen et al., 1990). While application of okadaic acid alone did not affect baseline levels of  $I_{HTK}$  (data not shown), co-application of okadaic acid with 4AP also abolished the compensatory increase in  $I_{HTK}$  (Figure 5A), suggesting the action of a serine/threonine protein phosphatase in this

compensatory effect. Because calcineurin is a well-known  $\text{Ca}^{2+}$ -dependent protein serine/threonine phosphatase (Klee et al., 1998), we used cyclosporine A to inhibit calcineurin activity in our system. Cyclosporine alone did not affect baseline levels of  $I_{\text{HTK}}$  (data not shown), but combined application of 4AP with cyclosporine eliminated the compensatory increase in  $I_{\text{HTK}}$  (Figure 5A), indicating that the increase in  $I_{\text{HTK}}$  is dependent, at least in part, on the activity of calcineurin.

In complete contrast, the compensatory influence of TEA on  $I_A$  appears to be implemented via mechanistically distinct pathways compared to those we found for the 4AP block on  $I_{\text{HTK}}$ . The increase of  $I_A$  in response to TEA blockade is neither calcium-dependent (Figure 5B) nor dependent on the activity of serine/threonine phosphatases (Figure 5B). Parallel experiments showed that BAPTA, ryanodine, okadaic acid and cyclosporine, when co-applied with TEA, failed to prevent a significant increase in  $I_A$  (Figure 5B). The only exception was that the application of ryanodine in conjunction with TEA appeared to reduce the magnitude of increase in  $I_A$ , although this effect was not statistically significant with respect to TEA alone ( $P = 0.103$ ; *t*-test), or TEA plus BAPTA ( $P = 0.08$ ).

We also examined the effects of inhibiting kinase activity on the compensatory effects of 4AP and TEA blockade. Staurosporine is a potent, cell permeable protein kinase C inhibitor which also partially inhibits other kinases such as PKA, PKG, and CAMKII (Ruegg and Burgess, 1989). Co-application of staurosporine with 4AP appears to cause a significant *decrease* in  $I_{\text{HTK}}$  (Figure 5A). However, this is a more complex

result than that for the other pharmacological blockers. Unlike any of the other pharmacological blockers used in this study, staurosporine was the only one to cause a change in baseline levels of  $I_{HTK}$  when applied alone (Figure 5C). Therefore, combined application of 4AP and staurosporine results in a relative decrease in  $I_{HTK}$  compared to that with staurosporine alone, but the net effect of 4AP + staurosporine is a restoration of  $I_{HTK}$  to baseline levels (Figure 5D).

Once again, the effects of staurosporine on  $I_A$  in the context of TEA blockade contrast with those for 4AP and  $I_{HTK}$ . There is no effect of staurosporine on baseline levels of  $I_A$  (Figure 5C), and while staurosporine co-applied with TEA results in an apparent decrease in the magnitude of the effect on  $I_A$ , there is still a significant increase in  $I_A$  with staurosporine present (Figure 5B), which is not statistically significant from the effect of TEA alone ( $P = 0.08$ ;  $t$ -test).

## DISCUSSION

### **Rapid compensation between $I_A$ and $I_{KCa}$ preserves both cellular and network outputs**

We have identified a naturally occurring co-regulatory relationship between potassium currents ( $I_A$  and  $I_{KCa}$ ) in an intact CPG network that results in homeostatic

compensation of neuronal excitability as well as network function. Furthermore, we have determined that these compensatory changes in  $K^+$  current magnitudes are independently regulated by distinct mechanisms. Compensatory increases in  $I_{KCa}$  are calcium dependent and due, at least in part, to the activity of calcineurin-based phosphatase activity. Conversely, compensatory increases in  $I_A$  are independent of all of the regulatory pathways implicated in the  $I_{KCa}$  response. These effects are also fairly rapid, acting over the course of 60-90 minutes to stabilize the activity of a critical CPG network responsible for cardiac muscle contraction and heart beat generation in the animal. While such homeostatic responses and their role in stabilizing synaptic function have been well studied (Bergquist et al., 2010, Turrigiano, 2011b), we know much less about the mechanisms underlying homeostatic plasticity of intrinsic excitability and the role this form of plasticity plays in the stabilization of neuronal and motor network output (Turrigiano, 2011b).

Even neurons and networks with extremely robust output display highly variable underlying physiological parameters responsible for neuronal output, particularly membrane conductances (Schulz et al., 2006a; Khorkova and Golowasch, 2007; Schulz et al., 2007; Goaillard et al., 2009; Temporal et al., 2012). Our work reveals that embedded within this variability are co-regulatory relationships that act to stabilize the excitability of the cell, in part by balancing the sum total of major transient outward currents,  $I_A$  and  $I_{KCa}$ . A similar relationship between  $I_A$  and  $I_{KCa}$  was reported in the STG. Artificial depolarization of inferior cardiac neurons results in increased  $I_A$  and decreased  $I_{HTK}$ ,

which is abolished by Cd<sup>2+</sup> blockade of calcium channels (Golowasch et al., 1999). These experiments did not reveal a naturally existing correlation between these currents (Golowasch et al., 1999), suggesting that excitability in the STG may be a more complex interaction among multiple conductances, or perhaps between conductances and their constitutive neuromodulation (Harris-Warrick, 2011). Although it is not known what effect this has on network output in the STG, our complementary results suggest that such homeostatic mechanisms may be common among motor neurons in different CPGs.

### **Distinct intracellular pathways mediate compensation**

The mechanisms involved in the regulation of the compensatory response mediated by I<sub>KCa</sub> after 4AP block in the CG network are consistent with work supporting changes in K<sup>+</sup> current density in a homeostatic fashion (Desai et al., 1999; Schulz et al., 2006b; Debanne and Poo, 2010); Misonou, 2010). In particular, the mechanisms we see for the compensatory increase in I<sub>KCa</sub> are similar to those found in regulation of excitability in cultured hippocampal neurons (Misonou et al., 2004; Misonou and Trimmer, 2004; Misonou et al., 2005). Increased excitability in these cultured neurons results in calcineurin-dependent dephosphorylation of Kv2.1 channels, leading to a functional potentiation of these channels via a shift in activation voltage, and to restoration of excitability (Misonou et al., 2004). While our data strongly suggest that I<sub>KCa</sub> is primarily responsible for the observed change in I<sub>HTK</sub>, we cannot conclusively rule

out a role for  $I_{Kd}$  (similar to Kv2.1). However, cyclosporine has been shown to alter  $I_{KCa}$  channels directly (Hay, 1998), and calcineurin is known to have widespread effects on neuronal plasticity and excitability beyond its effects on Kv2.1 activity (Groth et al., 2003). The effects seen in our experiments likely can be attributed to an overall increase in the maximal conductance of  $I_{KCa}$ , as we see no changes in either activation curves or any consistent or significant changes in input resistances of these cells (O'Leary et al., 2010).

The mechanisms underlying compensatory increases in  $I_A$  are less clear, but distinct from the pathways involved in the upregulation of  $I_{KCa}$ . Unlike for  $I_{KCa}$ , the increase in  $I_A$  is neither calcium-dependent, nor influenced by the activity of calcineurin or any other phosphatases that would be affected by treatment with okadaic acid (Cohen et al., 1990). Indeed, blocking neither phosphatase nor kinase activity by two broad spectrum blockers was able to prevent an increase in  $I_A$  as a result of TEA blockade, possibly precluding the contribution of phosphorylation state to this half of the compensation story. However, we were able to dampen the effect by blocking release of intracellular calcium with ryanodine, as well as by inhibiting kinase activity, suggesting a more complex path of regulation in this response. Given the potential non-specific effects of pharmacological treatment, we cannot rule out at least some role for a kinase in this pathway. For example, Kv1.2 potassium channels are known to be affected by cyclic AMP/protein kinase A pathways which enhance their conductance, in part by altering trafficking of these channels (Connors et al., 2008). Our staurosporine treatment

may result in only partial inhibition of PKA (Ruegg and Burgess, 1989), which could explain the intermediate effects seen on the A-type current compensation. Regardless, the fact that  $I_A$  and  $I_{KCa}$  are regulated by distinct pathways demonstrates an inherent robustness to this homeostatic response, which may be characteristic of networks responsible for critical functions, such as CPGs.

### **Reservoirs of channel proteins might implement rapid compensation**

Our data also begin to shed light on a striking disparity between levels of regulation in this system. Namely, we see an entirely different relationship at the level of mRNA for the channel genes *BKKCA* and *shaker* (positive correlation), than we do for the currents  $I_{KCa}$  and  $I_A$  that these channels most directly encode (negative correlation). Indeed, to date every correlation we have found between channel mRNAs at the single cell level has been a positive correlation (Schulz et al., 2007; Tobin et al., 2009; Temporal et al., 2012). These data include measurements of at least nine different channel genes in seven different motor neuron types in the crustacean stomatogastric and cardiac ganglia (some data unpublished, S. Temporal and D.J. Schulz), for a total of no fewer than 60 correlations in channel expression detected among channel transcript levels, and every one has thus far been positive. In addition, our data impact the present, although admittedly limited, understanding of the relationship between channel mRNA and ionic current in a given neuron. Namely, that mRNA for a given  $K^+$  channel

correlates positively with its corresponding ionic conductance (Schulz et al. 2006). Although both of these measurements were not made in the same cells in this study, logic dictates that there cannot simply be a positive relationship between mRNA and conductance for both K<sup>+</sup> currents in this study. Clearly, and not particularly surprisingly, our data demonstrate that more complexity lies within the relationship of mRNA and ionic conductance than a one-for-one tracking between these disparate levels of function in all cell types. However, our data continue to support the concept that correlation among mRNA levels (Schulz et al. 2007; Tobin et al. 2009) underlie a functional relationship at the conductance level.

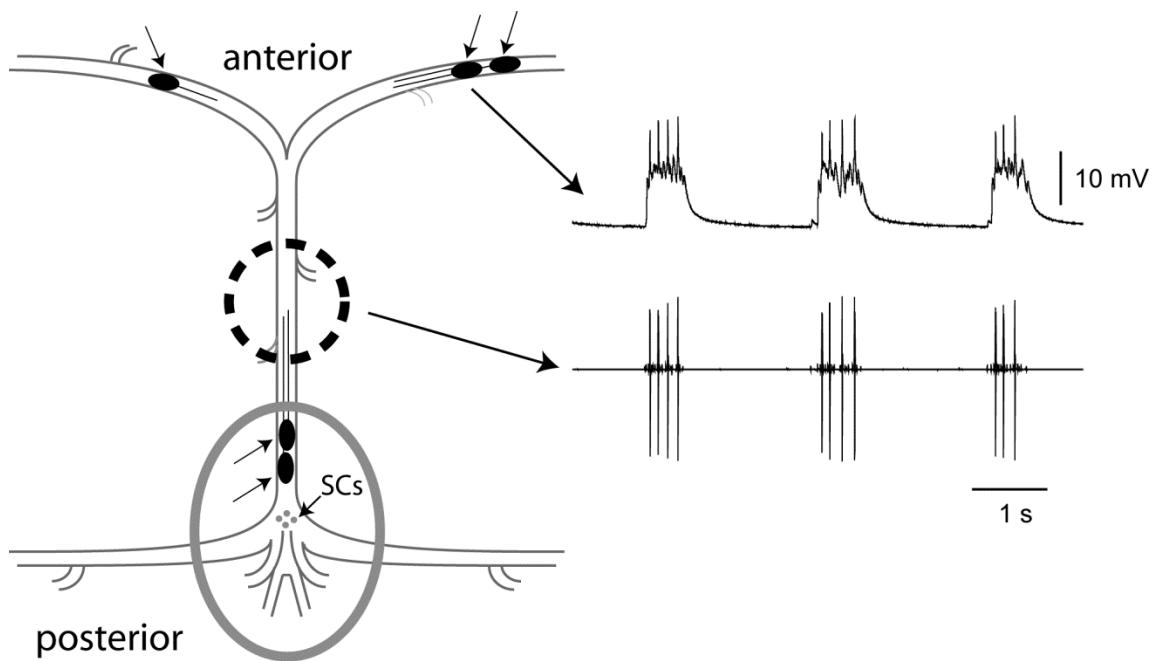
So then why do we see only positively correlated mRNA levels for channel genes in these motor networks? The linkage to cellular and network output in our study enables us to propose a new hypothesis in this regard. We hypothesize that rapid compensation of intrinsic excitability, such as that reported in this study, is implemented via an already existing pool of protein. That is, protein pools for the two opposing channels must already be available in relatively equivalent numbers, even if they are not functionally equally represented. This requires that mechanisms must occur at the level of gene regulation to ensure a sufficient “reservoir” of protein capable of compensating for the loss of a given channel. Thus, regardless of whether channels act in concert to set neuronal output (Ball et al., 2010; Franklin et al., 2010), or act in a compensatory fashion, the overall gene regulation between the two must be relatively balanced. Such a reservoir perspective is reminiscent of mechanisms seen for synaptic vesicle protein dynamics

(Fernandez-Alfonso et al., 2006), or extra-synaptic AMPA receptors that serve as a reservoir during synaptic plasticity (Hayashi et al., 2000; Zhu et al., 2000). Interestingly, insertion of AMPA receptor during synaptic plasticity is also under the control of phosphorylation-dependent processes (Lin et al., 2009). Therefore, this hypothesis provides a compelling framework for future investigation of the relationship between mRNA levels and ionic conductance, as well as the interplay between gene expression and post-transcriptional mechanisms involved in homeostatic plasticity of intrinsic excitability over different time scales.

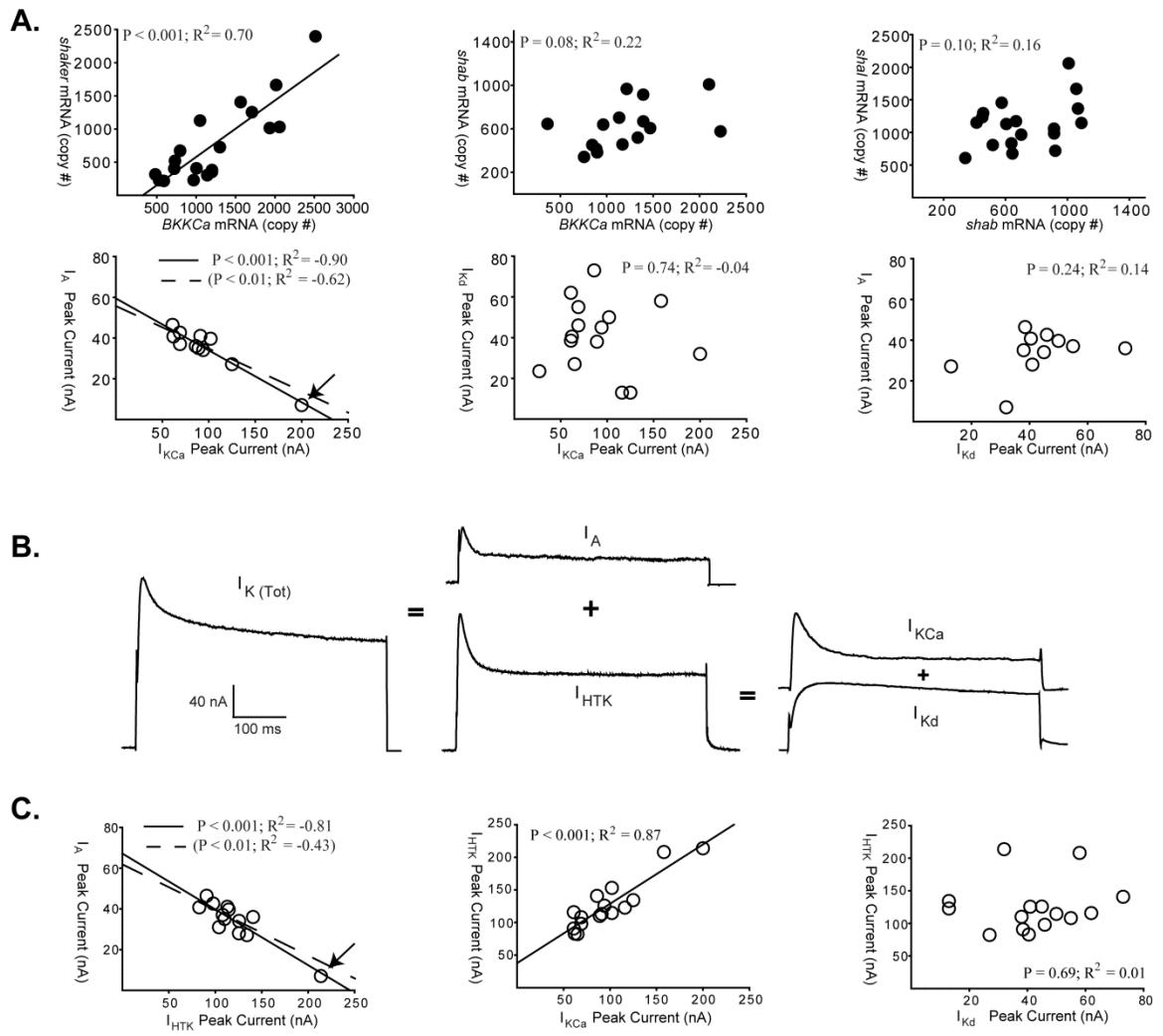
### **Putting it all together**

Our findings represent one of the first comprehensive demonstrations of rapid homeostatic plasticity of intrinsic excitability that results in a stabilization of output in a mature, intact network of a CPG. These rapid compensatory increases are mechanistically independent, suggesting robustness in the maintenance of neural network output that is critical for survival. Furthermore, this study reveals a distinct mechanism for compensation that leads us to at least one working model of homeostatic plasticity in this system (see Figure 6). We hypothesize that one pathway to functional compensation in this system relies on intracellular calcium concentration as a measure of cell excitability (Kennedy, 1989; Ross, 1989; LeMasson et al., 1993). A block of A-type K<sup>+</sup> channels leads to an increase in the excitability of the cell, causing release of intracellular calcium

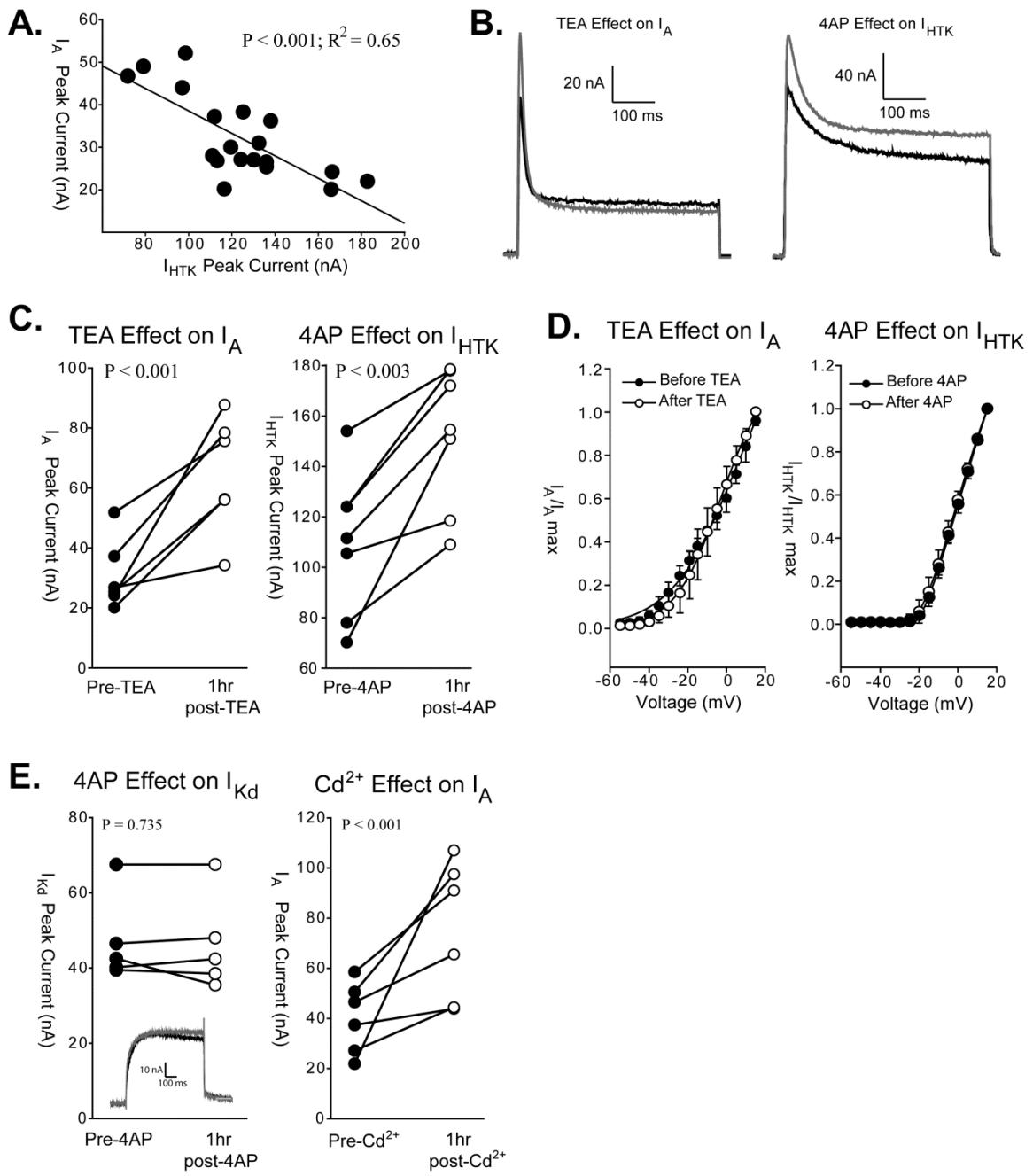
stores. This calcium influx alters calcineurin activity, resulting in dephosphorylation of targets, perhaps the KCa-channels themselves, that increases  $I_{KCa}$ . This ultimately restores the outward current balance that was lost during decreased  $I_A$  and thus restores excitability. The corresponding mechanism responsible for compensatory increases in  $I_A$  (Figure 6) is presently unknown, but is likely to involve distinct mechanisms for monitoring excitability (Dirnagl et al., 2003), as well as other candidate mechanisms that alter A-type conductances (Connors et al., 2008). Finally, we hypothesize that positive co-regulation of mRNA numbers for channel genes may ultimately provide a reservoir of channel protein (Figure 6) for implementing compensation over rapid time scales during which de novo synthesis may be insufficient to implement full compensation.



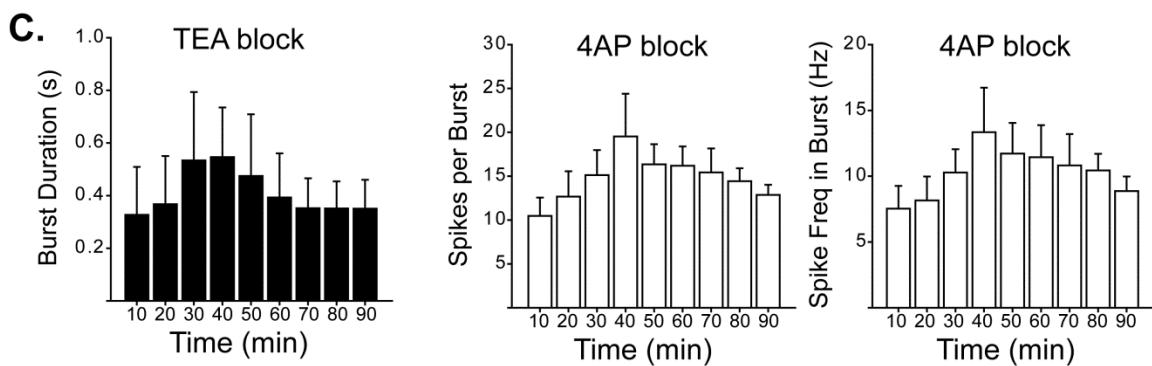
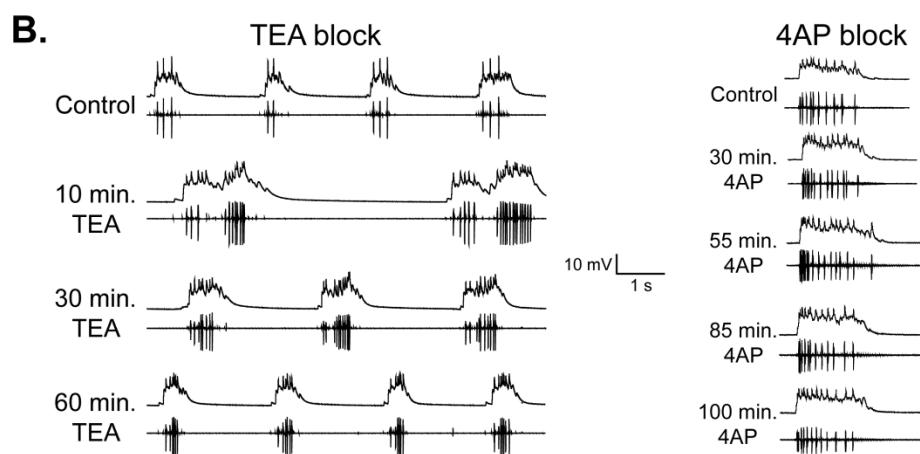
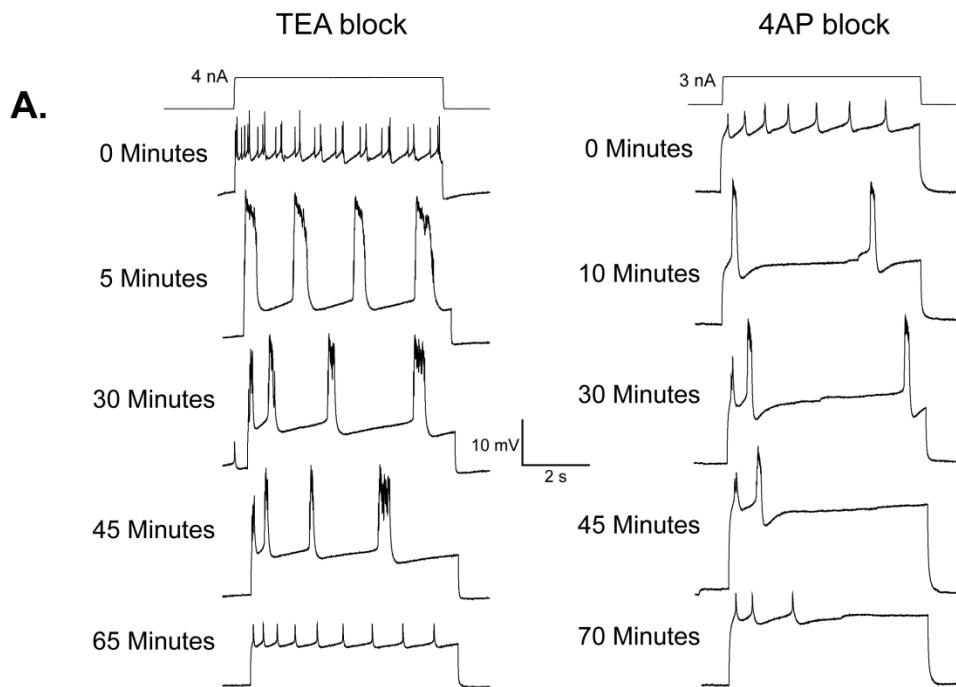
**Figure 2.1 The crustacean cardiac ganglion.** When dissected from the animal, the cardiac ganglion can be pinned flat and simultaneous recordings of network activity and intracellular recordings can be obtained. Five large cell somata (dark ovals marked with arrowheads) are distributed throughout the ganglion. Individual or pairs of large cells can be isolated for voltage clamp with thread ligature, or for pharmacological treatment with a vaseline well. The recording shows a simultaneous extra- and intracellular recording of network activity. The bursting of the network is seen at the site indicated by the dotted circle and corresponds to the extracellular (*bottom*) trace. Burst output of a single LC motor neuron is seen in the *top* trace, taken from an intracellular recording of a LC soma. This rhythmic motor activity corresponds directly to the contraction of the single-chambered crab heart muscle, showing an *in vitro* maintenance of biological network activity. The gray oval represents a vaseline well used in pharmacological blocker experiments. During measurements of individual LC excitability (Figure 4A), this well was used to apply TTX to the small cell pacemaker neurons (SCs, small gray circles) to silence the network activity but preserve output capability in anterior LCs. During measurements of compensation during ongoing network activity, this cell was used to protect SCs from blocker application in the bath (Figure 4B).



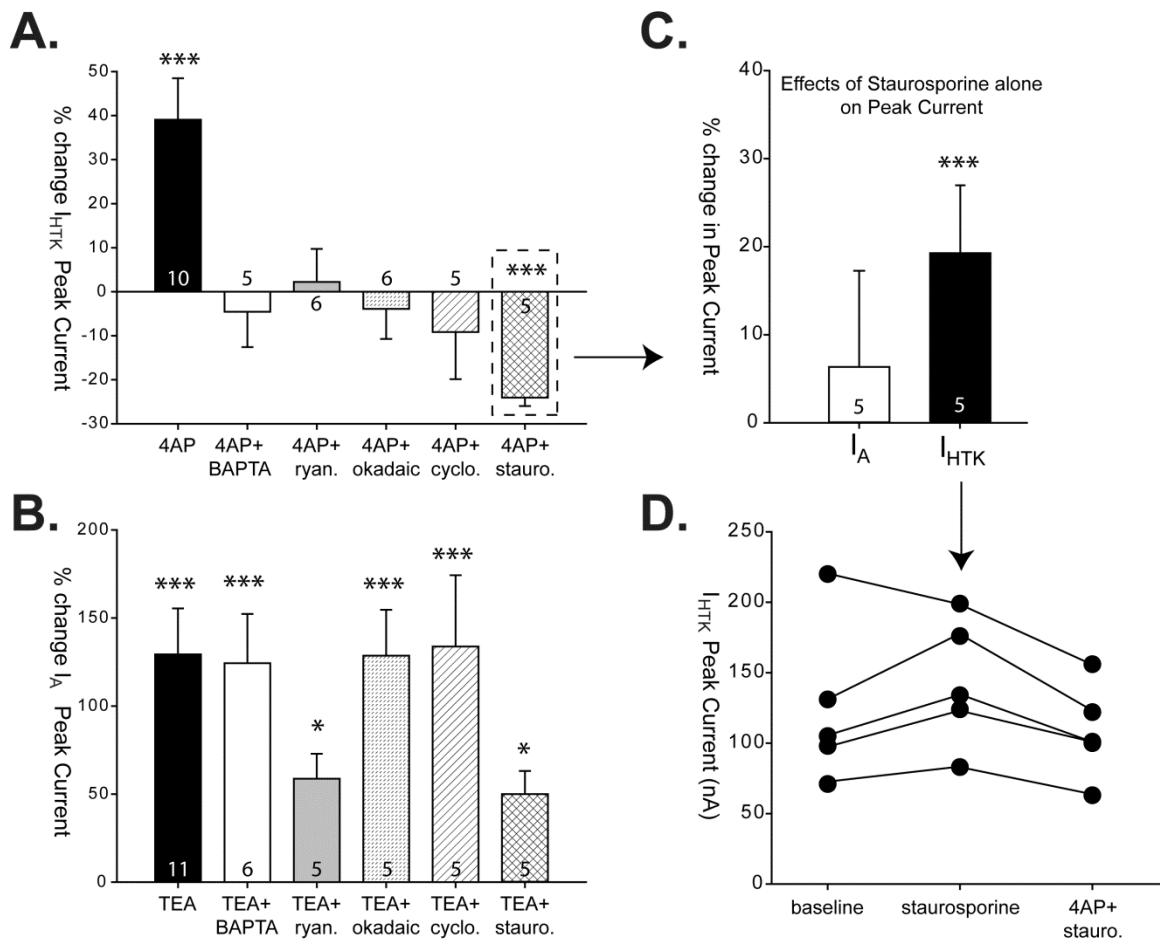
**Figure 2.2 Relationships among channel gene mRNA levels and among ionic currents in a normal population of large cell motor neurons.** **A.** Correlations between mRNA levels from single identified LC motor neurons for *BKKCa*, *shaker*, and *shab* channel genes (top row) and the corresponding K<sup>+</sup> current correlations from single identified LC motor neurons for I<sub>KCa</sub>, I<sub>A</sub>, and I<sub>Kd</sub> (bottom row). Each point represents values from a single neuron. Regression lines shown only for significant correlations as revealed by Pearson's test, for which the P-value and R<sup>2</sup> values are reported in each plot. When two regression lines are present, the solid line and top set of statistics refers to the entire data set, while the dotted line and the bottom set of statistics represents the correlation with the single point indicated by the arrow removed. Despite having this outlier removed, the correlation is still significant and largely unchanged. **B.** The total K<sup>+</sup> current (I<sub>K[Tot]</sub>) in LC motor neurons consists primarily of three distinct K<sup>+</sup> currents: A-type K<sup>+</sup> (I<sub>A</sub>), and the high-threshold K<sup>+</sup> current (I<sub>HTK</sub>) that can be subdivided into calcium-activated K<sup>+</sup> (I<sub>KCa</sub>) and delayed rectifier K<sup>+</sup> (I<sub>Kd</sub>). **C.** Correlations between currents reveal that I<sub>HTK</sub> peak is highly representative of I<sub>KCa</sub> levels, but not of I<sub>Kd</sub>. With these results, we use I<sub>HTK</sub> peak levels as an indicator of I<sub>KCa</sub> for any given cell for the remainder of the study. Statistics as in panel A.



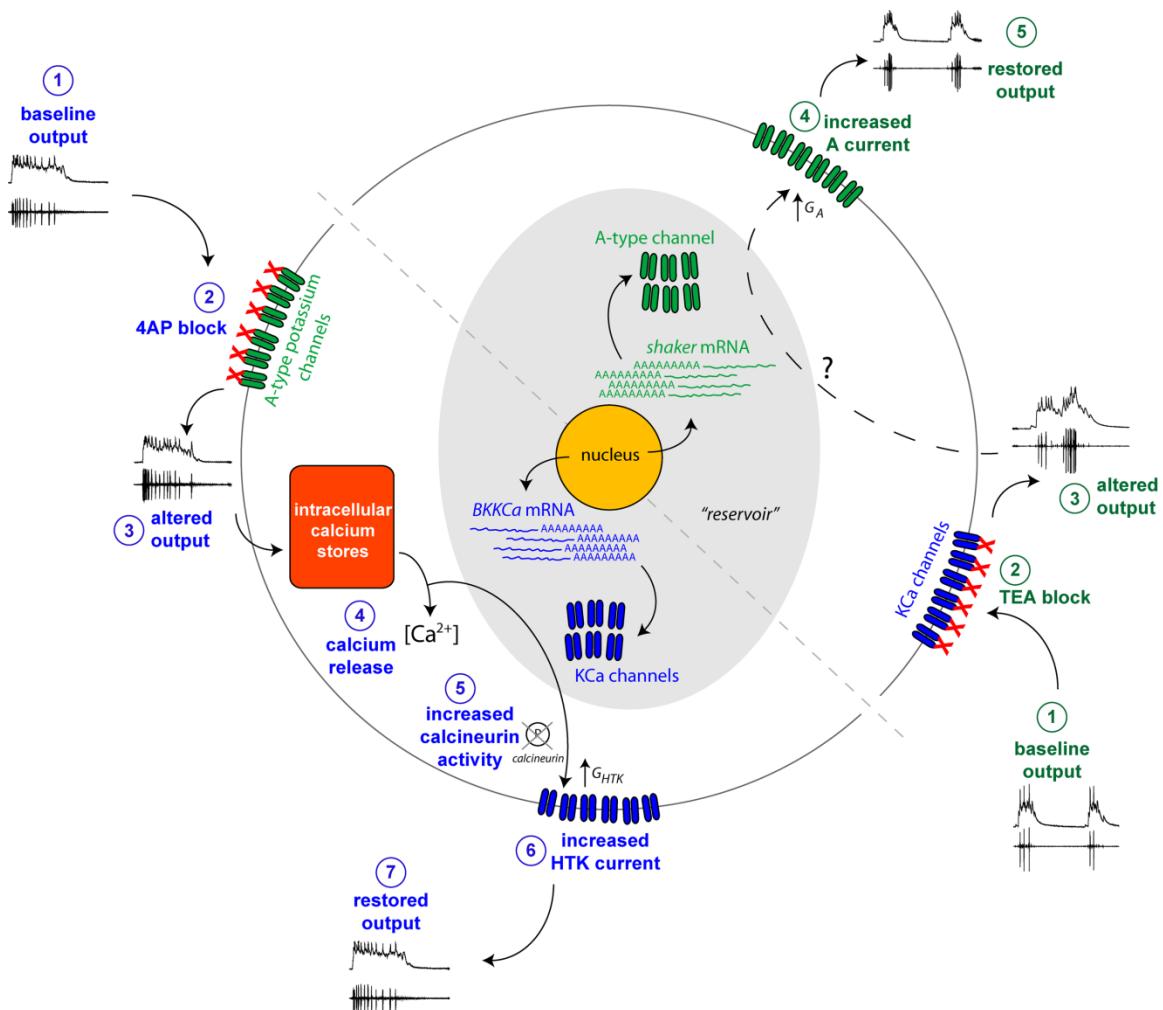
**Figure 2.3 Reciprocal interaction of  $I_A$  and  $I_{HTK}$  levels in LC motor neurons.** **A.** Correlation between peak  $I_A$  and  $I_{HTK}$  across a second population of LC motor neurons distinct from those in Figure 2. Statistics represent results of a Pearson's test ( $n=20$ ). **B.** Representative recordings of the increase in  $I_A$  after TEA exposure (*left*) and the increase in  $I_{HTK}$  after 4AP exposure (*right*). Black trace is the control, gray trace is the same cell after 60 min exposure to blocker. **C.** Quantified effects of TEA (*left*) and 4AP (*right*) on the peak  $I_A$  and  $I_{HTK}$  respectively in  $N = 6$  cells. The same cell before (black) and after (white) is connected with a solid line. Statistics represent paired *t*-test on mean current before and after blocker. **D.** Activation characteristics, expressed as  $I/I_{max}$  for an  $N = 5$  cells, of  $I_A$  (*left*) and  $I_{HTK}$  (*right*) before and after block with TEA and 4AP respectively. Each point represents mean  $\pm$  SD. **E.** Effects of 4AP on  $I_{Kd}$  (*left*;  $N = 5$ ) and  $Cd^{2+}$  on  $I_A$  (*right*;  $N = 6$ ). Insert in the left panel shows representative traces of  $I_{Kd}$  before (black) and after (gray) exposure to 4AP. Legends and statistics as in panel C.



**Figure 2.4  $I_A$  and  $I_{KCa}$  engage in a compensatory relationship that stabilizes neuronal excitability and network output.** **A.** Representative recordings of the effects on the excitability of individual LC motor neurons isolated from network activity after exposure to TEA (*left*) and 4AP (*right*). Because the pacemaker neurons of the network were silenced with TTX in this experiment, DC current injections were used to elicit activity in LC motor neurons (current traces shown at top). **B.** Representative recordings of the effects of TEA (*left*) and 4AP (*right*) exposure on network output over time. Pacemaker cells were shielded from exposure to the blocker (see Figure 1), while the 3 upper motor neurons were exposed to blocker. Paired intracellular (*top* traces) and extracellular recordings were made over the time course of the experiment. **C.** Quantified effects of TEA and 4AP effects on burst characteristics of LC motor neurons in the intact network. Bars represent mean  $\pm$  SD of  $N = 5$  preparations at 10 minute intervals. The first 10 minute interval is baseline without blocker, and subsequent bins represent cumulative time after blocker exposure.



**Figure 2.5 Use of pharmacological inhibitors to probe mechanisms of changes in  $I_A$  and  $I_{KCa}$ .** **A.** Effects of BAPTA, ryanodine, okadaic acid, cyclosporine, and staurosporine (referred to as the *treatment*) on the induction of increased  $I_{HTK}$  with 4AP exposure. All bars are mean  $\pm$  SD, sample sizes as shown in bars. All results are % change in peak  $I_{HTK}$  with 4AP + treatment relative to *treatment alone* (see methods). None of the treatments caused a change in baseline levels of  $I_{HTK}$  with the exception of staurosporine (dotted box; see panel C). \*\*\* represents a significant ( $P < 0.001$ ) difference from 0 via one-sample *t*-test. **B.** Effects of BAPTA, ryanodine, okadaic acid, cyclosporine, and staurosporine on the induction of increased  $I_A$  with TEA exposure. All results are % change in peak  $I_A$  with TEA + treatment relative to *treatment alone* (see methods). None of the treatments caused a change in baseline levels of  $I_A$ . \*\*\* ( $P < 0.001$ ) and \* ( $P < 0.01$ ) represent a significant difference from 0 via one-sample *t*-test. **C.** Effects of staurosporine alone on baseline levels of  $I_A$  and  $I_{HTK}$ . \*\*\* represents a significant ( $P < 0.001$ ) difference from 0 via one-sample *t*-test. **D.** Overall effects of staurosporine alone and then 4AP + staurosporine on  $I_{HTK}$ . Each individual cell is connected with a solid line across the treatments.



**Figure 2.6 A working model for the induction of homeostatic plasticity of intrinsic excitability via rapid compensation between  $I_A$  and  $I_{KCa}$ .** This model summarizes all of the data in the current study and provides a framework for interpretation and future experimentation. The two halves of the cell represent the distinct mechanisms induced by a block of  $I_A$  with 4AP (*left, blue pathway*) and a block of  $I_{KCa}$  with TEA (*right, green pathway*). *BLUE PATHWAY (4AP blockade)*: The baseline activity (1) is disrupted by the block of A-type channels with 4AP (2), causing an alteration in the excitability of the cell and its output in the network, in this case rapid initial firing frequency (3). This change presumably results in the release of calcium from intracellular stores (4) that increases activity of the calcium-dependent phosphatase calcineurin (5). Calcineurin activity induces an increase in  $I_{KCa}$  (6), restoring the excitability of the cell and re-establishing motor neuron activity in the intact network (7). *GREEN PATHWAY (TEA blockade)*: Baseline network activity (1) is disrupted via TEA blockade (2), causing substantial changes in the output properties of the motor neuron and the network (3). While the intracellular mechanisms remain unclear at this point, a subsequent increase in  $I_A$  that is independent of the pathway invoked by 4AP blockade compensates for loss of  $I_{KCa}$ , restoring output of the neurons and the network (5). This compensation is rapid (on the order of 1 hour), suggesting that there is an already existing “reservoir” or channel protein available that is maintained via positive co-regulation at the transcription/mRNA level of the channel genes responsible for  $I_{KCa}$  and  $I_A$  (*GRAY OVAL*).

## CHAPTER THREE

### **Neurons within the same network independently achieve conserved output by differentially balancing variable conductance magnitudes**

Biological and theoretical evidence suggest that individual neurons may achieve similar outputs by differentially balancing variable underlying ionic conductances. Despite the substantial amount of data consistent with this idea, a direct biological demonstration that cells with conserved output, particularly within the same network, achieve these outputs via different solutions has been difficult to achieve. Here we demonstrate definitively that neurons from native neural networks with highly similar output achieve this conserved output by differentially tuning underlying conductance magnitudes. Multiple motor neurons of the crab (*Cancer borealis*) cardiac ganglion have highly conserved output within a preparation, despite showing a 2-4 fold range of conductance magnitudes. By blocking subsets of these currents, we demonstrate that the remaining conductances become unbalanced, causing disparate output as a result. Therefore, as strategies to understand neuronal excitability become increasingly sophisticated, it is important that such variability in excitability of neurons, even among those within the same individual, is taken into account.

Neurons with similar and conserved output across individuals can exhibit 2-6 fold variability in their intrinsic conductances (Golowasch et al., 2002, Swensen and Bean, 2005b, Schulz et al., 2006, Goaillard et al., 2009a, Ransdell et al., 2012) as well as in ion channel mRNA levels (Schulz et al., 2006, Schulz et al., 2007b). This observation has motivated several computational studies that used populations of model cells with variable intrinsic properties and constrained output features to demonstrate that model neurons could achieve similar voltage output with disparate intrinsic parameters (Goldman et al., 2001b, Prinz et al., 2004b, Taylor et al., 2009, Ball et al., 2010b). This approach has complemented and extended accumulating biological evidence that is consistent with the idea that output features across identified cells may be conserved by both balance and compensation among key intrinsic conductances, rather than by tightly regulating the magnitude of individual conductances (MacLean et al., 2003, Swensen and Bean, 2005b, Grashow et al., 2010, Ransdell et al., 2012). However, most of these studies involve compensation that leads to conservation of output following perturbation of the cellular excitability (MacLean et al., 2003, Bergquist et al., 2010), often via gene knockout (Van Wart and Matthews, 2006, Nerbonne et al., 2008) or pharmacological manipulation (Swensen and Bean, 2005b, Ransdell et al., 2012). While these studies demonstrate that variability could arise as a result of such homeostatic plasticity, these studies do not address intrinsic variability found in these neurons with all conductances intact, or whether this variability represents differential tuning to conserved output *in vivo*.

We utilize the crustacean cardiac ganglion, which contains multiple large cell (LC) motor neurons that produce synchronous bursting output, to test whether individual neurons achieve conserved output by differentially balancing conductance magnitudes. We examine multiple motor neurons within the same ganglia, which are genetically identical and have similar output in the native network, and find that they have varying underlying conductances. Then by disrupting a select subset of conductances in these cells with pharmacological blockade, we demonstrate a corresponding disruption in conserved output. We believe this is the first direct demonstration that multiple neurons, particularly within the same neural network, naturally generate similar output by differentially balancing variable underlying conductances, independent of induced compensatory changes.

## MATERIALS AND METHODS

### Animals

Crabs (*Cancer borealis*) of either sex were purchased and shipped overnight from The Fresh Lobster Company (Gloucester, MA, USA). Crabs were kept at 12°C in artificial seawater. Dissections took place in chilled physiological saline: 440 mM NaCl, 26 mM MgCl<sub>2</sub>, 13 mM CaCl<sub>2</sub>, 11 mM KCl, and 10 mM HEPES (pH = 7.4). Chemicals were obtained from Fisher Scientific (Pittsburgh, PA) unless otherwise noted.

### Electrophysiology

All intracellular recordings were made from LC3, 4, and 5 somata. LC structure consists of a cell soma and proximal neurite that projects to a common spike initiation area located posterior to the anterior branch point (Hartline, 1967a, Tazaki and Cooke, 1983b, Cooke, 2002a, Ransdell et al., 2013) [see Fig 1A]. Somata were separated from action potential (AP) conductances (unless noted otherwise) by tightening a thread ligature past the anterior branch point on the nerve the LC was located in (see Fig. 1A, 2A, 2B). Isolated somata carry ionic conductances that generate driver potential output (Tazaki, 1972, Tazaki and Cooke, 1983b, Tazaki and Cooke, 1986, Cooke, 2002a), even with ligatures as close as 200  $\mu$ m from the soma (Tazaki and Cooke, 1983b).

Experiments were performed in physiological saline at 12°C. Extracellular recordings were made with stainless steel pin electrodes in petroleum jelly wells placed on the nerve. Signals were amplified and filtered using a differential AC amplifier (A-M Systems, Sequim, WA). Intracellular recordings were made with glass electrodes containing 3 M KCl (8-17 M $\Omega$ ) using an Axoclamp 2A amplifier (Axon Instruments, Union City CA). Two-electrode voltage clamp (TEVC) and two-electrode current clamp (TECC) protocols were created, driven and recorded with Clampex 9.2 software (Axon Instruments). Recordings were analyzed with Clampfit 9.2 (Axon Instruments).  $R_{in}$  was measured in TECC with 10 negative current injection steps ( $t = 2$  s, -1 to -10 nA).

TEVC measurements for  $I_A$ ,  $I_{HTK}$ ,  $I_{Ca}$ , and  $I_{NaP}$  were made using protocols described in detail in our previous work (Ransdell et al., 2012, Ransdell et al., 2013). Outward currents were measured at 0 mV, inward currents at peak conductance.

### **Stimulus Protocols**

To generate current injection waveforms, we recorded voltage waveforms from LC somata during intact network activity. For Stimulus Protocol 1, this consisted of 20s recordings from LC3 that included four burst potentials with both pacemaker EPSPs and LC back-propagating APs (BPAPs). During this recording  $V_{rest} = -55$  mV. For Stimulus Protocol 2, to remove LC BPAPs, we hyperpolarized the LC soma to -65 mV to eliminate spiking. This enabled us to record the voltage change caused by a single burst of pacemaker EPSPs. We then isolated LC3 with ligature and used the voltage waveforms recorded as the command voltage in TEVC. The average current injection over five sweeps necessary to generate each of the voltage waveforms was used for Stimulus Protocols 1 and 2.

Each stimulus protocol was applied at  $V_{rest}$  and four starting voltages (-60, -50, -40, -30 mV) controlled with DC current injection. Blockers (25 mM TEA or 1 mM 4AP) were applied to the preparation for 30 minutes, after which stimulus protocols were repeated at each starting voltage.

## Statistics

Analyses utilized SigmaPlot 11.0 and Clampfit 9.2 software. R-values are results of Pearson correlation (Fig. 2) or cross-correlation function estimate (Fig. 3, 4) with a 10 ms lag; in cross-correlation analysis, the peak R-value across the lag period was used. Correlation analyses were conducted only between LCs of the same ganglion using the entire voltage trace from each stimulus protocol. After failing Shapiro-Wilk tests for normality, changes in  $R_{in}$ ,  $V_{rest}$ , and differences between R-values before and after pharmacological blockade were analyzed with Mann-Whitney  $U$ -tests.

## RESULTS

In the intact cardiac ganglion (Fig. 1A), bursts in LCs are initiated via excitatory input from pacemaker interneurons (Fig. 1B) that result in synchronous burst and AP generation in all five LC motor neurons (Fig. 1B). In addition, LC somata contain the intrinsic conductances that influence burst potentials (Fig. 1C). However, the magnitudes of these currents vary not only across animals (Fig. 1C), but even among cells of the same ganglion (Fig. 1D). If variability in current magnitude suggests that individual cells differentially balance their conductances to achieve a common output, then blocking a subset of conductances should reveal differential tuning of the remainder, as demonstrated by a shift away from conserved output. Our initial data were consistent with this hypothesis: when LCs were exposed to high-threshold K<sup>+</sup> current ( $I_{HTK}$ ) blocker (TEA – see Fig. 1D inset), their normally synchronous waveforms in spontaneously

active networks became desynchronized and variable (Fig. 1E). TEA application localized to LC somata is able to affect spiking output, causing changes in the spiking pattern as well as apparent desynchronization of spiking as revealed by a decrease in spike amplitude that we interpret as loss of summed, synchronous AP activity (Fig. 1F). This decrease in amplitude cannot be attributed to TEA block of APs, as the somata localization of the TEA in this experiment left axonal conductances intact. These data demonstrate that LC somatic conductances play a significant role in shaping waveform as well as spiking output in these cells.

Because cells in intact networks are subject to many factors that influence output, we employed an experimental strategy to test solely the influence of variable conductances on output in neurons isolated from their constituent network connections. To reliably demonstrate a shift away from conserved output at the single cell level following conductance block, we devised standardized, biologically relevant current injection protocols. We isolated the somata of the three anterior LCs from pacemaker synaptic input, electrical coupling, and BPAPs, effectively isolating their burst generating conductances (Fig. 2A, 2B). We then used current injection to characterize cell output before and after blocking conductances. In designing the protocol, which employs somatic current injections, we considered that somata naturally receive two kinds of current input: synaptic and BPAPs. We recorded these somatic input currents from cells in intact networks, and subsequently used these recordings as the basis for realistic current injections applied to isolated cell somata (Figs. 2A, 2B; see Methods). Stimulus Protocol 1 consists of both biologically realistic synaptic currents plus BPAPs (Fig. 2A).

Stimulus Protocol 2 consists solely of current injection of synaptic drive to the soma via pacemaker inputs (Fig. 2B). We first determined that our current injection protocols, when applied to isolated somata with all intrinsic conductances intact, produced virtually identical voltage responses across LCs as measured by cross-correlation analysis. Under control conditions, current injection elicited conserved membrane waveforms across LCs in the same network (Figs. 2 A1, B1 – controls). Thus the basis for our experiments is whether these conserved output responses are maintained subsequent to pharmacological blockade of conductances.

We considered four key points in testing the hypothesis of conserved output from variable underlying conductances. First, we ensured that individual conductance levels do indeed vary across isolated cells. We measured current levels carried by four ionic conductances in LC somata:  $I_{HTK}$  (high-threshold  $K^+$  current, a combination of  $I_{Kd}$  and  $I_{KCa}$ ),  $I_A$  (transient  $K^+$ ),  $I_{Ca}$ , and  $I_{NaP}$  (persistent  $Na^+$ ). Each current measured varied at least 2-4 fold across individual cells (Fig. 1C). Second, if output simply were constrained by electrical synapses between LCs, then isolated neurons should no longer produce conserved output from standardized current injection. This was not the case; isolated LCs with all conductances intact produced remarkably consistent output (Fig. 2, controls). Third, if conserved output is simply a result of isolated cells passively following current injection, then blocking conductances should not alter this output. This also was not the case; when  $I_{HTK}$  is blocked with TEA (Fig. 1D), cell output as a result of the standardized current injection was substantially altered (Fig. 2 A2, B2 – blue boxes). Finally, and perhaps most pertinent to the hypothesis, if cells are not differentially tuned

to produce similar output, then blocking a conductance might still be expected to alter output, but should produce uniform changes across cells. This was not the case; when TEA was applied to isolated LCs, and standardized current injection applied, the once similar outputs diverge between cells (Fig. 2) as revealed by significantly lower (and highly variable) R-values from cross-correlation analyses following TEA exposure (Fig. 3 A,B). To ensure that these differences were not due to changes in  $V_{rest}$  after TEA exposure, current injections were performed from native  $V_{rest}$ , as well as standardized baseline voltages ranging from -60 mV to -30 mV. TEA did not cause a significant change in  $V_{rest}$  (mean  $\pm$  SD - control:  $-49 \pm 7.03$  mV, TEA:  $-46.3 \pm 10$  mV,  $p = 0.23$ ,  $N=12$ ). However, TEA did cause significant reduction in mean R-value between cells at  $V_{rest}$ , -50 mV, -40 mV, and -30 mV starting voltages, but not at -60 mV, in both Stimulus Protocols (Fig. 3A,B). At -60 mV, the depolarization in membrane potential due to current injection did not reach the activation voltages of most of the conductances (Ransdell et al., 2012, Ransdell et al., 2013). Therefore, the -60 mV data actually demonstrate what happens when these cells are simply passive followers of current injection, and support the result that at voltages where conductances are activated, there is a true loss of tuning when a subset of currents are blocked.

To ensure these results are not due to changes in input resistance ( $R_{in}$ ) of cells in TEA, we analyzed relationships between  $R_{in}$  and activity. TEA did not significantly or predictably alter  $R_{in}$  (mean  $\pm$  SD – control:  $5.03 \pm 2.4$  M $\Omega$ , TEA:  $5.25 \pm 3.28$  M $\Omega$ ,  $p = 0.795$ ,  $N=12$ ). However, we predicted that if loss of conserved activity across LCs with blockade were a result of variable impact of the TEA on  $R_{in}$ , then the largest changes in

activity between cells should occur with the largest difference in  $R_{in}$  between those two cells. We found no such relationship between change in  $R_{in}$  of individual cells, or the difference in  $R_{in}$  between pairs of cells, with the change in R-value in the corresponding cross-correlation (Fig. 3C-F).

Finally, if this is a general phenomenon and not just specific to  $I_{HTK}$ , then blocking another conductance in this system also should result in loss of conserved output. We blocked a second  $K^+$  current,  $I_A$ , using 4-aminopyridine (4-AP). 4-AP caused the same loss of conserved output in LCs (Fig. 4A) with both Stimulus Protocols, as well as an overall increase in variability of R-values (Fig. 4B).

## DISCUSSION

Evidence for compensation of intrinsic excitability that stabilizes neuronal output has accumulated from nervous systems across phyla, ranging from the cardiac neurons used in this study (Ransdell et al., 2012) to mammalian systems (Desai et al., 1999, Nerbonne et al., 2008). This homeostatic plasticity of intrinsic excitability is likely a critical mechanism underlying neural network dynamics (Davis, 2006, Turrigiano, 2011a), and may be involved in disorders of neuronal excitability such as epilepsy (Echegoyen et al., 2007, Howard et al., 2007). These compensatory responses, and the changes and variability in ionic conductances they induce, are usually the result of pathology, injury, or experimental manipulations that substantially and drastically alter the parameter landscape of these neurons. Yet few of these model systems capture native

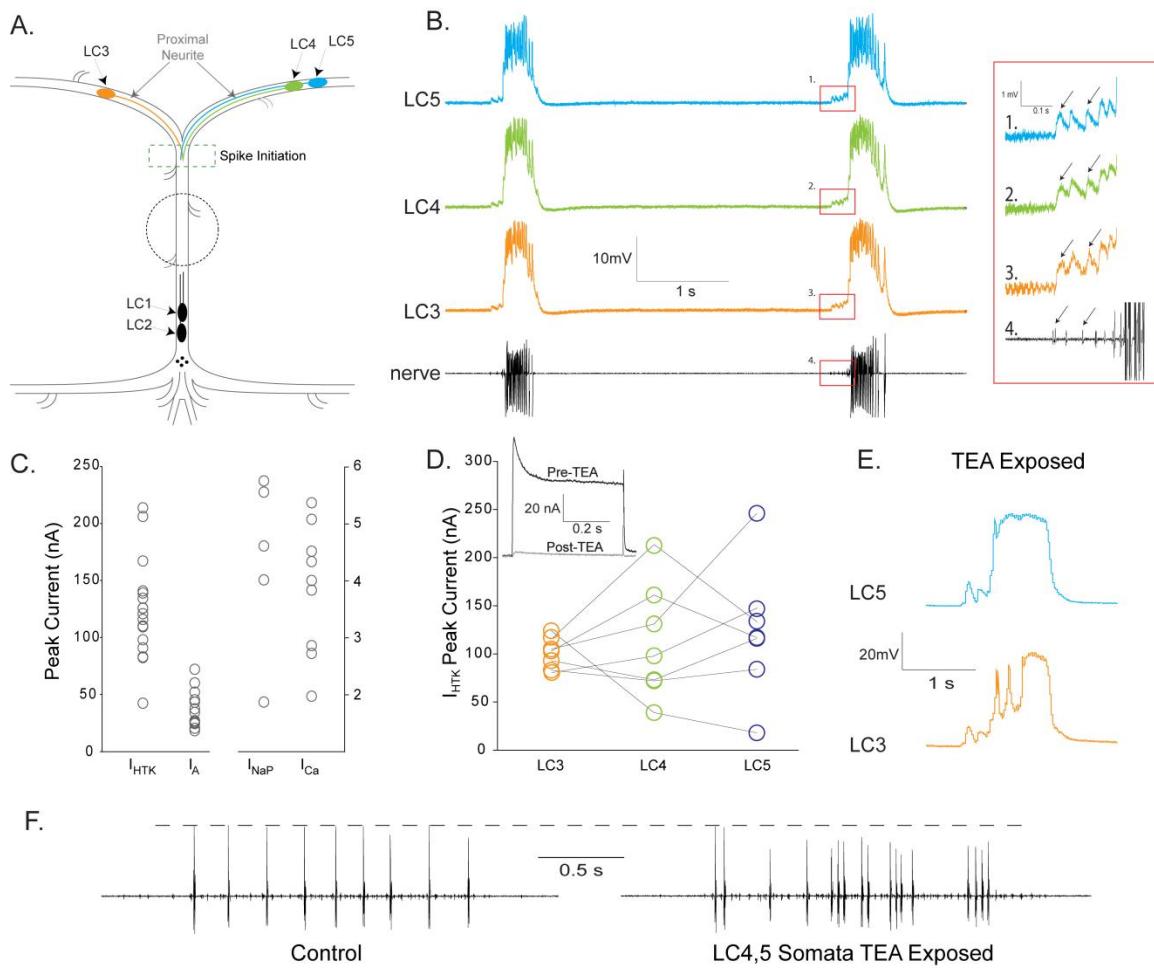
variability of neurons within unmanipulated networks. So the question remains, do neurons in native networks, that are genetically identical (i.e., cells within the same network), achieve similar output at least in part by differentially tuning the underlying intrinsic conductances via distinct mechanisms? It is this question, independent of compensation, that our study addresses.

We addressed several key components of this question in this study. First, we demonstrated that motor neurons of the cardiac ganglion have similar membrane potential waveforms within the same network, both during intact network activity (Fig. 1B) and as isolated neurons responding to biologically relevant current injection protocols (Fig. 2). This ability to record from unambiguously identified neurons both in intact networks and under experimentally controlled conditions, both of which are crucial to directly test the hypothesis in this paper, represents a key strength of this model system, and how it can contribute uniquely to this question. Second, we measured native current magnitudes of multiple ionic conductances, to ensure that these cells also showed variability in magnitudes of conductances as reported in other systems (Fig. 1C). Not only did these cells show 2-4 fold variability in their underlying conductances, but even cells within the same network showed substantial variability in current magnitudes (Fig. 1D). Third, we ruled out the possibility that the voltage waveforms of isolated cells were passively following external current injection (Fig. 2C, 2D). Finally, these preconditions allowed us to directly pose the experimental question: does natural variability in underlying current magnitudes result from differentially tuned conductances converging on similar output via distinct solutions? We tested this with a relatively straightforward

experimental design. Namely, if output is the result of finely balanced ratios of ionic conductances, then disrupting one conductance should cause each cell to experience a cell-specific de-tuning, resulting in loss of conserved output. Our results were entirely consistent with the hypothesis: blocking either  $I_{HTK}$  or  $I_A$  independently results in loss of similar output across three LC neurons within the same network (Figs. 2, 3A, 3B).

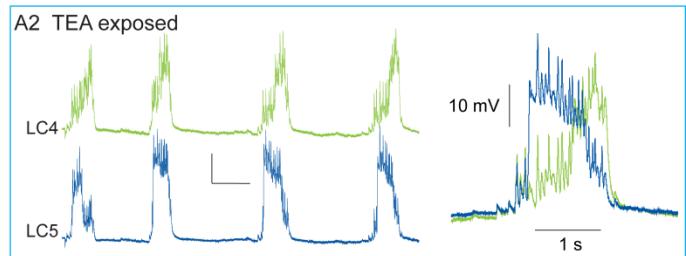
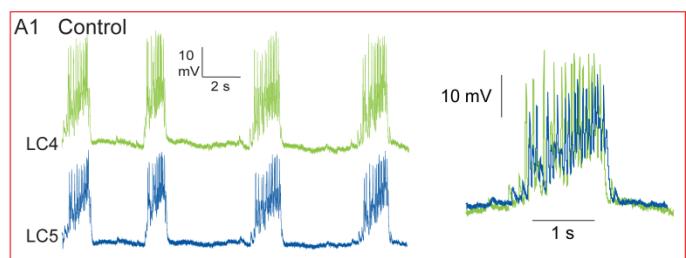
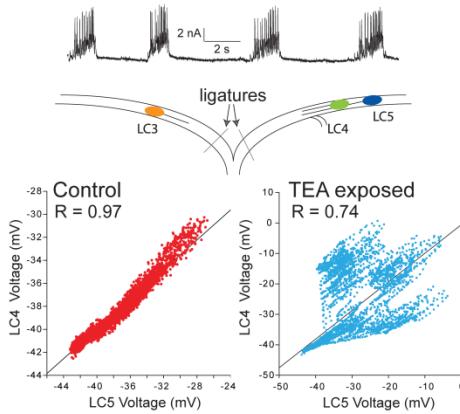
Similar manipulations in pacemaker neurons of the stomatogastric ganglion (STG) have yielded different results (Szucs and Selverston, 2006). In the STG, 4AP used to disrupt A-type current in paired pyloric dilator neurons, also reported to have variable conductance magnitudes (MacLean et al., 2005), showed little impact on synchronized activity between these cells (Szucs and Selverston, 2006). These data, while seemingly contradictory, are intriguing as Szucs et al. (2006) left chemical and electrical synaptic connectivity, as well as neuromodulatory inputs to these networks (Marder and Thirumalai, 2002), intact during 4AP application. We carefully selected cardiac LCs as a model where we have control over these higher order network properties, allowing us to focus solely on intrinsic excitability. Interpreted in the context of the Szucs and Selverston work (2006), convergent output as a result of differentially tuned conductances likely is only one layer of regulation in these systems ensuring synchronized output (see Prinz et al. 2004). Work is ongoing to determine whether and how higher order processes, such as electrical coupling and neuromodulation, ensure that cellular and network output are maintained in patterns necessary for robust function (Grashow et al., 2009, 2010, Marder, 2012).

The most parsimonious explanation for our results is that cells with variable underlying conductances are indeed individually tuned to produce conserved output. We believe these findings provide a clear and unambiguous demonstration of this phenomenon, helping unify a substantial amount of compelling and consistent evidence in multiple model systems, both biological and theoretical (Marder, 2011a, Marder and Taylor, 2011, Turrigiano, 2011a). It is striking that differential tuning is not simply found across different individuals, but is seen even among cells with in the same individual. One compelling question that arises from these findings is the nature of the developmental and post-developmental origin of this variability. Specifically, are individual neurons produced with common underlying conductance relationships that then diverge over time (via compensation), or is variability inherent to the initial development and tuning of a neuron, and maintained across the lifetime of the animal? Answers to these questions will rely on model systems that allow for identified neurons to be characterized effectively over both developmental and post-developmental time scales.

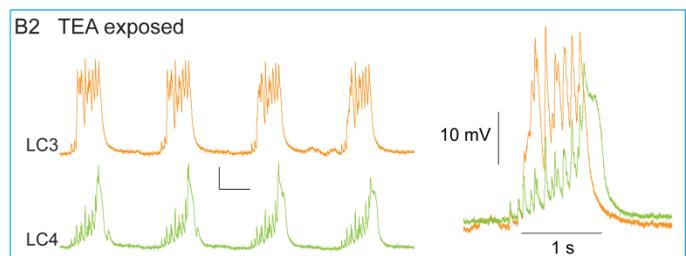
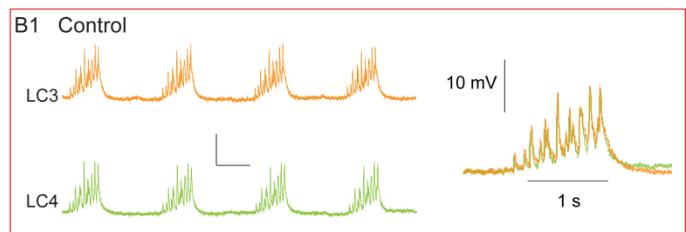
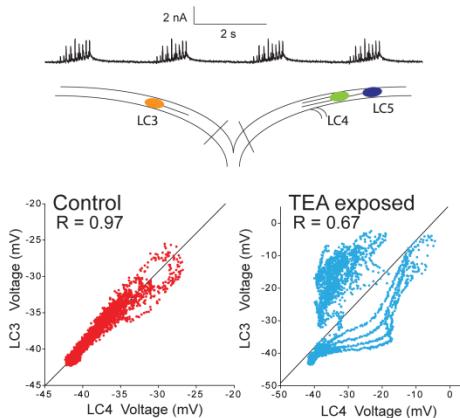


**Figure 3.1 A) Schematic of *C. borealis* cardiac ganglion showing location of LC somata (ovals) and pacemaker interneurons (small circles).** Extracellular recordings are taken from the central nerve (dashed circle). All experiments were conducted on three anterior LCs 3-5 (colored ovals). These cells project a proximal neurite from their somata towards a common spike initiation zone region (green dashed box), and then axons continue posterior. **B)** Activity of LC neurons during spontaneous network activity. Extracellular recording (bottom trace) shows LC (tall spike) and pacemaker (short spike) APs. *Inset, red box-* enlarged recordings displaying that each pacemaker AP (small spike) results in an EPSP in all three anterior LCs. Two pacemaker APs and resulting EPSPs are labeled (arrows). **C)** Variability in LC inward and outward current magnitudes. **D)**  $I_{HTK}$  variability across LCs within the same network. Lines connect LCs from same individual. *Inset:*  $I_{HTK}$  is blocked by 25 mM TEA exposure (30 min). Current traces before (blue) and after (red) TEA were clamped at 0 mV step from -40 mV holding potential. **E)** TEA exposure in the intact network desynchronizes membrane potential waveforms of LCs during ongoing rhythmic activity. **F)** Spiking output (extracellular recordings) is affected by TEA applied to LC4 and LC5 somata. Dashed line for comparison of spike amplitudes. Traces were taken from the same recording well within 10 minutes of one another.

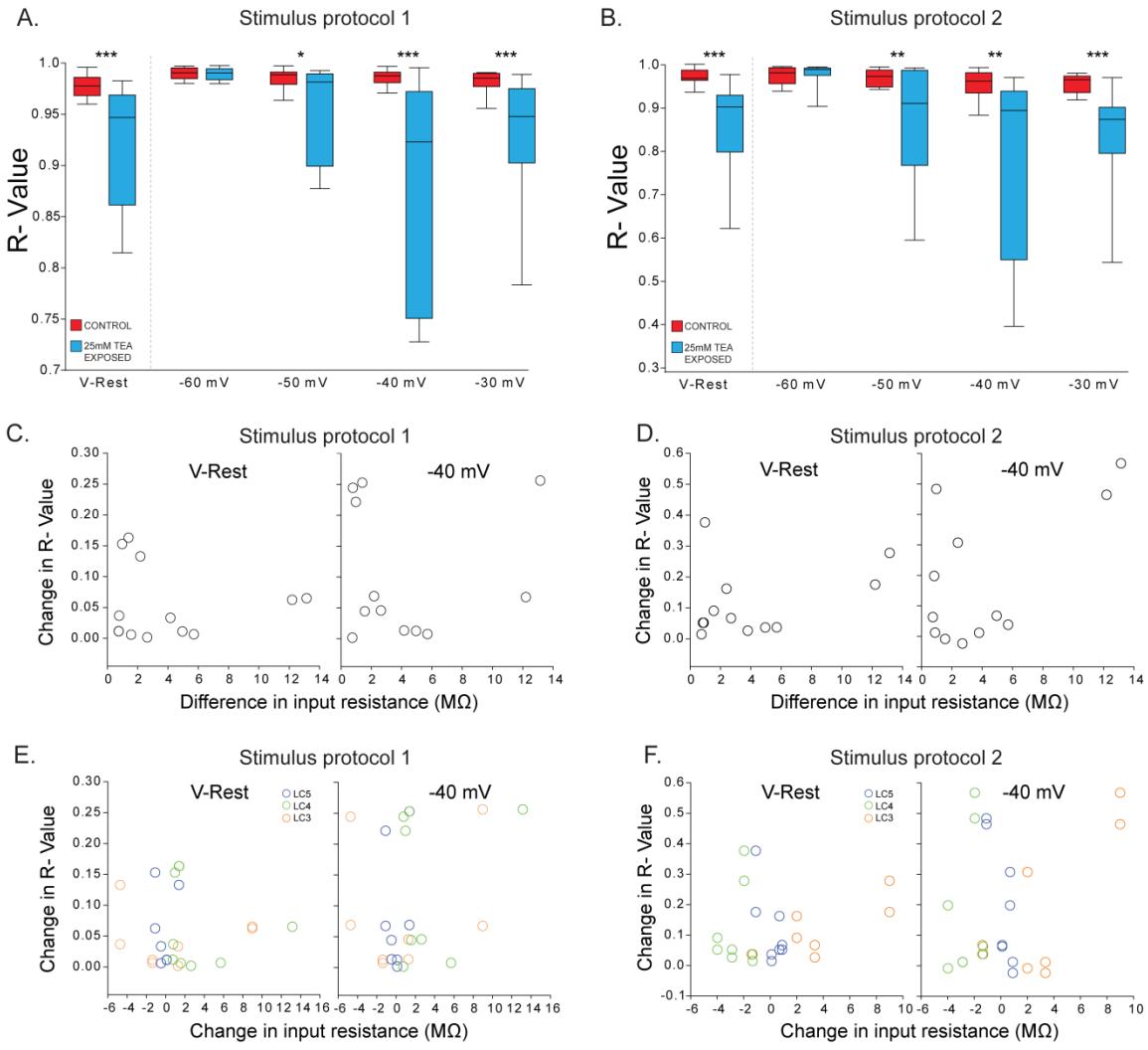
**A. Stimulus protocol 1**  
(synaptic + BPAPs)



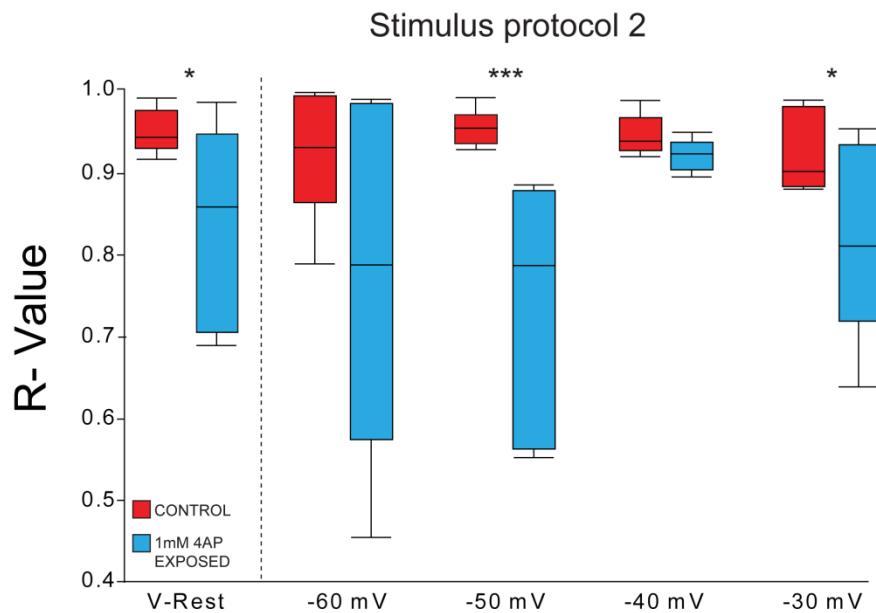
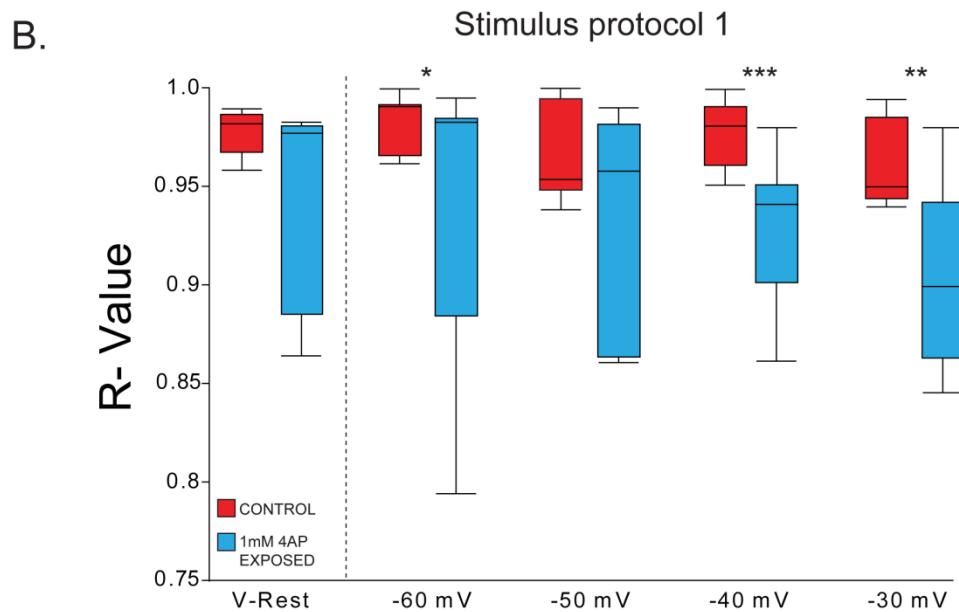
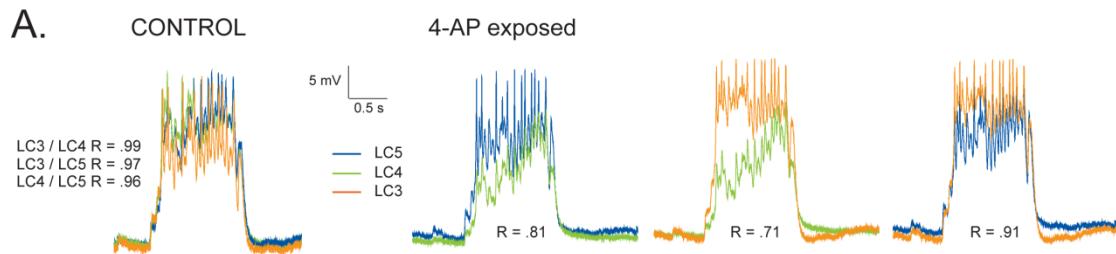
**B. Stimulus protocol 2**  
(synaptic only)



**Figure 3.2 Realistic current injection protocols used to test intrinsic excitability of isolated LCs.** **A.** Stimulus protocol 1 reproduces both synaptic currents and back propagating APs (BPAPs). LCs 3, 4, and 5 are isolated from the network via thread ligatures (slash marks), and the stimulus protocol is applied before (A1 - control, red box) and after (A2 - TEA exposed, blue box) exposure to 25 mM TEA. Representative traces show the response to the entire stimulus protocol, and overlaid traces show the 4<sup>th</sup> burst in the sequence. Scatterplots show pair-wise correlation of time matched voltages (sampled at 500Hz) of the waveforms shown in the representative traces. R-values are results of Pearson's correlation test for these two cells. Loss of conserved output is demonstrated by the lack of correlation in the scatterplot as well as the decrease in R-value. **B.** Stimulus protocol 2 reproduces synaptic currents LCs receive from pacemaker neurons. Experiments and analyses were performed as in Stimulus Protocol 1.



**Figure 3.3 Changes in output after TEA exposure.** **A-B.** Box plots show distributions of R-values from cross-correlation analysis of LC voltage waveforms generated by Stimulus Protocol 1 (**A**) and Stimulus Protocol 2 (**B**) before (red boxes) and after (blue boxes) 25 mM TEA exposure. Lines within boxes mark the median, box boundaries represent 25<sup>th</sup> and 75<sup>th</sup> percentiles, whiskers represent maximum and minimum values. All comparisons were made between LCs of the same individual (N=12 comparisons across 6 individuals). Each stimulus was injected into an isolated LC at its natural V<sub>rest</sub> and four starting voltages. Significant differences in median R-value were tested with Mann-Whitney *U*-tests, and are denoted by asterisks (\*\* - p<0.005, \*\* - p<0.01, \* - p<0.05). **C-D.** Comparison of change in R-value with difference in R<sub>in</sub> between LCs after TEA exposure for Stimulus Protocol 1 (**C**) and Stimulus Protocol 2 (**D**). **E-F.** Comparison of change in R-value with change in R<sub>in</sub> after TEA exposure for Stimulus Protocol 1 (**E**) and Stimulus Protocol 2 (**F**).



**Figure 3.4 Effects of 4-AP on conserved output.** **A.** Overlaid representative traces of LC responses to Stimulus Protocol 1 before and after 4-AP exposure. R-values from cross-correlation analyses as in Figure 3. **B.** Box plots show distributions of the R-values from cross-correlation analysis of isolated LCs voltage waveforms generated by Stimulus Protocols 1 and 2 before (red boxes) and after (blue boxes) 1 mM 4AP exposure. The line within the box marks the median, box boundaries represent the 25<sup>th</sup> and 75<sup>th</sup> percentiles, whiskers above and below represent the maximum and minimum values. All comparisons made between LCs of the same individual (N=7 and N=6 for Stimulus Protocols 1 and 2 respectively), as described in Figure 3. Differences in median R-value were tested with Mann-Whitney U-tests, and are denoted by asterisks (\*\*\* - p<0.005, \*\* - p<0.01, \* - p<0.05).

## CHAPTER FOUR

### **LC motor neurons co-regulate electrical coupling and intrinsic conductance properties to maintain synchronized burst output**

Electrical synapses are often implicated in the synchronization of neurons within a circuit. The importance of gap junction communication is becoming increasingly appreciated in large scale neurological events such as brain rhythms (Marder et al., 2005) and epileptic seizures (Perez Velazquez and Carlen, 2000). Small, well defined and rhythmic networks, which utilize electrical coupling, are an ideal means to investigate how electrical coupling interact with other functional components of a rhythmic neural networks and can further our understanding of how groups of neurons achieve synchronous or asynchronous firing states. These model systems have recently shed light on the complexity of intrinsic excitability regulation and maintenance. Work in crustacean central pattern generators show that neurons with identical output, can have several fold variability in their intrinsic conductances (Golowasch and Marder, 1992, Schulz et al., 2006, Temporal et al., 2012); computational and biological evidence further suggest that conserved relationships between intrinsic conductances and network level properties act in maintaining similar output properties across cells with disparate intrinsic

organization (Prinz et al., 2004a, Ball et al., 2010a, Franklin et al., 2010, Ransdell et al., 2012). Here we ask if there are conserved relationships between electrical coupling strength and the disparate intrinsic organization of synchronized motor neurons, and if so are these relationships functional in maintaining synchrony. To do this we utilize the three anterior large cell (LC) motor neurons of the *Cancer borealis* cardiac ganglion. These cells have disparate intrinsic conductance organization, are electrically coupled and burst synchronously during network behavior.

We begin by exploring both the coupling strength and two intrinsic potassium currents across several animals; the purpose of this is to expose possible conserved relationships between these properties. We find that of the three anterior LCs, those which have more variability in the potassium current  $I_{HTK}$ , namely LC4 and LC5, also have greater amount of electrical coupling. Furthermore, the magnitude of  $I_{HTK}$  is positively correlated with the strength of electrical coupling between two LCs.

Next, we manipulate both electrical coupling and  $I_{HTK}$  to test if the correlations found between these properties are functional in maintaining LC synchrony. Using dynamic clamp to manipulate electrical coupling, and the pharmacological blocker TEA to inhibit  $I_{HTK}$ , we find when  $I_{HTK}$  is greater, LCs require a greater amount of electrical coupling to synchronize activity. This suggests that the correlation between  $I_{HTK}$  and coupling strength is functional in maintaining LC synchronization.

These results demonstrate that identified neurons maintain appropriate output, not only by maintaining relationships between intrinsic parameters, but also by co-regulation of intrinsic properties with network level properties such as electrical coupling.

## Introduction

Computational and biological studies in the last decade have uncovered key principles in how neurons generate and maintain appropriate output. Using model systems in which neurons are identifiable from animal to animal we now understand that both network properties, such as electrical and chemical synaptic strength, and intrinsic properties, such as voltage gated currents and input resistance, can be variable across cells and networks, while maintaining identical outputs (Swensen and Bean, 2005a, Schulz et al., 2006, Schulz et al., 2007a, Goaillard et al., 2009b, Ball et al., 2010a, Ransdell et al., 2013). In short, there are multiple solutions to a given network / neuronal output. Studies also reveal that compensatory interactions among network and intrinsic properties result in conserved relationships which can be measured across animals (Ball et al., 2010a, Franklin et al., 2010, Ransdell et al., 2012); these relationships are thought to act in maintaining the signature output of the network or neuron. While these advances are significant, it is still unclear what part regulation of intrinsic properties, and what part regulation of network properties, play in maintaining functional output (for

review see Turrigiano, 2011B); furthermore, there are few biological studies which examine if there are co-regulatory mechanisms which bridge intrinsic properties with network level properties; that is, a conserved relationship between something intrinsic to a cell and a property of the network the cell functions in. These are questions this study aims to address by carrying out dual intrinsic (ionic currents) and network level (electrical coupling strength) measurements, and examining how relationships between these properties function in maintaining an important characteristic of network function like motor neuron synchronization.

The *C. borealis* cardiac ganglion is a central pattern generator (CPG) network of only nine neurons and two distinct cell types. Four SC interneurons drive five LC motor neurons to burst synchronously causing whole heart contraction. We know of three levels of regulation which contribute to the synchronous LC output. First, LCs receive the same excitatory input from the SC pacemaker neurons. Second, LC motor neurons within a network have disparate intrinsic conductances that are actively tuned to achieve similar levels of intrinsic excitability. Third, LCs are electrically coupled to one another, albeit with coupling conductances which are variable both within a network, and across networks. The following study is based on the hypothesis that because there is variability in these last two levels of regulation (intrinsic conductances, electrical coupling strength) there are likely conserved relationships between these two parameters, which are functional in maintaining synchronization.

We approach this experimentally in two steps. We first probe anterior LCs for relationships between electrical coupling and two voltage gated potassium currents ( $I_A$ ,  $I_{HTK}$ ) known to affect LC bursts. We then test if these relationships are functional in LC synchronization by manipulating coupling strength via dynamic clamp, and intrinsic conductance via pharmacology, and examine how these manipulations affect burst synchronization across in anterior LC pairs.

## Methods

### Animals

Crabs (*Cancer borealis*) of either sex were purchased and shipped overnight from The Fresh Lobster Company (Gloucester, MA, USA). Crabs were kept at 12°C in artificial seawater. Dissections took place in chilled physiological saline: 440 mM NaCl, 26 mM MgCl<sub>2</sub> 13 mM CaCl<sub>2</sub>, 11 mM KCl, and 10 mM HEPES (pH = 7.4). Chemicals were obtained from Fisher Scientific (Pittsburgh, PA).

### Electrophysiology

Dissection preparation and electrophysiology equipment were performed as in chapter three experimental methods.

Electrical coupling and  $R_{in}$  was measured in TECC with 15 negative current injection steps ( $t = 2$  s, -1 to -15 nA). Coupling strength was always measured in both directions of an electrically coupled LC pair. Strength of electrical coupling was

$$\text{calculated as coupling coefficient (CC): } \text{CC} = \frac{\Delta V_1}{\Delta V_2}$$

Coupling strength was also measured as coupling conductance. Coupling conductance was calculated by taking the inverse of coupling resistance. To calculate coupling resistance (CR), independent of the two LCs input resistance, we used the following

$$\text{equation: CR} = \frac{(R_{input1} * R_{input2} - (R_{1 \rightarrow 2})^2)}{R_{1 \rightarrow 2}}$$

Where  $R_{input1}$  is the input resistance of the cell 1, and  $R_{1 \rightarrow 2}$  is the resistance from cell 1 to cell 2 due to electrical coupling. Coupling conductance is measured as the inverse of coupling resistance as in Haas et al. (2011).

Two-electrode voltage clamp (TEVC) and two-electrode current clamp (TECC) protocols were created, driven and recorded with Clampex 9.2 software (Axon Instruments). Recordings were analyzed with Clampfit 9.2 (Axon Instruments). TEVC measurements for  $I_A$ ,  $I_{HTK}$  were made using protocols described in chapter 2 methods

section. Current clamp Stimulus Protocol 1, described in chapter 3 Methods section, was used to test LC excitability and synchronization.

Dynamic clamp experiments used Netclamp 1.0 software (Friedman Brain Institute, New York, NY) to insert artificial electrical coupling between two isolated LCs. To combine Netclamp driven artificial electrical coupling protocol with Clampex 9.2 driven Stimulus Protocol 1, both output signals were sent through a Brownlee model 410 instrumentation amplifier, where they were summed before being sent to the current injection electrodes. Using this setup, artificial electrical synapse was added between isolated LCs while Stimulus Protoocol 1 was simultaneously injected into the two cells. These protocols were administered after both cells were exposed to 25mM TEA for 10 minutes and never extended past 45 minutes TEA exposure. Cell pairings were always between LC3 and LC4 or LC3 and LC5. The following electrical coupling strengths were used for each cell pairing: 0  $\mu$ S, .025  $\mu$ S, .05  $\mu$ S, .1  $\mu$ S, .2  $\mu$ S and .4  $\mu$ S.

## Statistics

Analyses utilized SigmaPlot 11.0 and Clampfit 9.2 software. R-values are results of Pearson correlation (Fig. 2) or cross-correlation function estimate (Fig. 3, 4) with a 10 ms lag; in cross-correlation analysis, the peak R-value across the lag period was used. Changes caused by TEA exposure were analyzed with a paired 2-tail T-test.

## Results

### Anterior LC to LC electrical coupling

The five LC motor neurons of the *C. borealis* cardiac ganglion are electrically coupled and fire synchronous bursts during normal network output. In this study we concentrate on the three anterior LCs as they can be easily isolated from network components via thread ligature placed just posterior to the anterior branch point (figure 1A). This reduced preparation offers three coupled motor neurons with disparate intrinsic properties that are able to fire synchronous burst potentials during normal network behavior (see Figure 3.1). All three anterior LCs (LC3 , LC4, LC5) are electrically coupled at the anterior branch point (Fig. 4.1A); there is additional local coupling between LC4 and LC5 somata (Fig. 4.1A). This additional local coupling likely causes LC4 and LC5 to have a greater total amount of electrical coupling to anterior LCs than LC3. Figure 4.1B shows mean coupling conductance on each of the anterior LCs (x-axis), from the additional two anterior LCs; 2 bars per cell, bar colors denote which LC the coupling conductance is impacting.

The clearest difference on the Figure 4.1B is total coupling conductance affecting LC3 is smaller than total coupling conductance affecting LC4 and LC5. We also find

that electrical coupling between LC4 and LC3 is significantly higher than coupling between LC5 and LC3 (two-tailed t-test,  $p < .001$ ), this difference is likely because electrical coupling between LC3 and LC4 or LC5 takes place at the anterior branch point of the CG, and the somata (where measurements take place) of LC4 are closer to the anterior branch point than the somata of LC5.

### **Anterior LC $I_{HTK}$ and $I_A$ properties**

Because LC3 (Fig. 4.1B orange bars) has a smaller amount of total electrical coupling to anterior LCs than LC4 (Fig. 4.1B green bars) and LC5 (Fig. 4.1B blue bars), we thought to examine if there is differential magnitude of the outward potassium currents  $I_A$  and  $I_{HTK}$  across the three anterior LCs. These currents were chosen because they can be measured without the use of pharmacological blockers, are known to be important to bursting output in these cells (See chapter 3) and can be quickly removed using the blockers TEA ( $I_{HTK}$ ) or 4AP ( $I_A$ ). In Figure 4.1C we show  $I_A$  (*upper*) and  $I_{HTK}$  (*lower*) magnitude at 0mV voltage step across multiple LC3, LC4 and LC5 neurons. We find that LC3, while having the least amount of total LC to LC coupling among the anterior cells, also has the smallest variability in  $I_{HTK}$  magnitude (quantified as coefficient of variation) across animals (Fig. 4.1D).  $I_A$  coefficient of variation did not correlate with total coupling strength on LCs. Note: total electrical coupling present on each anterior LC was calculated by adding the mean coupling conductance a LC has with the two anterior LCs (mean values shown in Fig. 4.1B). We do not see a significant

difference in LC3, LC4 and LC5 magnitude of the two currents (Fig. 4.1C,  $p > .05$  for all comparisons of current magnitude).

Because LC3 has the least amount of total electrical coupling, and also has the smallest coefficient of variation in  $I_{HTK}$  magnitude we hypothesize that LC3 may have a more constrained  $I_{HTK}$  parameter space because of a lack of LC to LC electrical coupling; or to be put another way, LC4 and LC5  $I_{HTK}$  parameter space can be more variable because the two cells have stronger total electrical coupling to other anterior LCs, which may act in constraining output properties.

### **Does Variability in $I_{HTK}$ affect LC burst output?**

Before testing if the relationship between  $I_{HTK}$  variability and coupling strength are functionally important, we sought to test first, if the difference  $I_{HTK}$  parameter space can be measured as a function of, and is relevant to, the LCs intrinsic voltage response to depolarizing stimuli. To do this we apply Stimulus Protocol 1 (see Fig. 3.2) to anterior LCs before and after TEA exposure, just as in chapter 3. Only, instead of comparing LC voltage response across a single network of anterior LCs, we instead run cross correlations on LC3 with LC3 neurons in other animals (4 animals LC3 cells yield  $n=16$  comparisons), and the same with LC4 and LC5. We hypothesize that if LC3 actually has a more constrained parameter space of  $I_{HTK}$ , then after TEA exposure ( $I_{HTK}$  removal), LC3 voltage response to Stimulus Protocol 1 will be less differential than LC4 and LC5

comparisons. Data support this hypothesis (see examples, Fig. 4.2B), with LC4-LC4 and LC5-LC5 correlations showing a significantly larger decrease in R-value (comparing voltage response to Stimulus Protocol 1) after exposure to TEA (Fig. 4.2C *Left*). This result is further demonstrated if we plot the change in R-value of LC3, LC4 and LC5 against the  $I_{HTK}$  coefficient of variability for LC3, LC4 and LC5 (Fig. 4.2C *Right*).

### **Relationships between current magnitude and coupling strength**

Because LC4 and LC5 have a larger amount of variability, both in  $I_{HTK}$  magnitude and coupling strength, we thought this cell pairing is the most appropriate to probe for relationships between intrinsic current magnitude and coupling strength. We find that the combined magnitude of an LC4 / LC5 pairs  $I_{HTK}$  has a significant positive correlation with the cell pairs coupling conductance (data not shown,  $n=7$ ,  $R$ -value = .87,  $p = 0.011$ ). This relationship is significant if either LC4 or LC5's individual  $I_{HTK}$  magnitude is compared to the coupling conductance as well (Fig. 4.3A, LC4:  $p < .05$ ; LC5:  $p < 0.1$ ). This relationship is also present and significant ( $p < .05$ ) if coupling coefficient is used rather than coupling conductance (Fig. 4.3B). There was no significant relationship found between LC4 / LC5 coupling conductance and LC4  $I_A$  ( $n=5$ ,  $p = .23$ ) or LC5  $I_A$  ( $n = 6$ ,  $p = .284$ ); though a larger sample size may be beneficial to ensure that no relationship exists.

### **Potential False relationship due to measurement error**

We do not believe the  $I_{HTK}$  / coupling conductance relationship is an experimental artifact of voltage clamping in one cell, and recruiting additional membrane and  $I_{HTK}$  current in the cell which it is coupled to. During TEVC protocols to measure  $I_{HTK}$ , the voltage in the coupled neuron is not typically depolarized enough to activate  $I_{HTK}$ . Activation of  $I_{HTK}$  begins around -20mV (Fig. 2.3D); at 0mV voltage step- post-synaptic LCs peak voltage =  $-28.5 \pm 8.3$ mV (n=7). Furthermore, in one experiment we carried out TEVC protocol to measure  $I_{HTK}$  magnitude of LC4 under regular conditions, and again with LC5 hyperpolarized via DC current injection. Under these two conditions we see less than 3% difference in current magnitude at 0mV (data not shown). This is in line with previous work which investigated the effect of electrical coupling on measured conductance magnitude in two PD neurons of the stomatogastric ganglion, results show that experimental errors are decreased (<10%) when measuring large outward potassium currents, and further reduced when measuring currents at more depolarized membrane potentials (Rabbah et al., 2005).

### **Does electrical coupling strength affect synchronization of LC output?**

In chapter three we demonstrate that the anterior LCs have disparate intrinsic tuning, yet common levels of excitability, by applying realistic current injection protocols to isolated anterior LCs. These protocol are administered with all conductances intact, resulting in similar voltage responses across LCs, and again after uniformly removing a single potassium current, causing a disparate voltage response across anterior LCs.

While these results demonstrate LCs tune similar excitability through differential intrinsic

properties, it does not take into account the electrical coupling across LCs, which likely also plays a part in maintaining a uniform and synchronous output. Now that we have found conserved relationships between coupling strength and  $I_{HTK}$ , an intrinsic property known to impact burst output in LCs, we begin to ask if these relationships are functional in producing synchronized bursts across network LCs.

To begin exploring how electrical coupling may maintain synchronous LC bursts, we carry out Stimulus Protocol 1 before and after  $I_{HTK}$  inhibition (TEA exposure); similar to what was done in chapter three. In this experiment however, there is one important difference; we leave electrical coupling between the LCs intact (no ligatures anterior of branch point), and administer the current injection protocols simultaneously to the two coupled LCs (see schematic, Fig. 4.4A). This simultaneous excitatory input is more realistic to what the coupled LCs undergo during normal network behavior, in which SCs provide very similar excitatory drive to coupled LCs (see Fig. 3.1). The goal of these experiments are to test if, like intrinsic properties, the network level property of LC-LC electrical coupling, also help in maintaining similar output across a network.

We find that when simultaneous current injections are administered to two electrically coupled LCs, those cells maintain very similar output, both before and after exposure to TEA. Correlation coefficient comparing the two coupled cells voltage response to stimulus protocol 1 was not significantly different after TEA exposure at cells

normal resting membrane potential ( $V_{rest}$ ) (Fig. 4.4B,  $p = 0.327$ ). When the two cells have a -40mV starting potential (achieved with DC current injection) the R-values are actually significantly increased after TEA exposure (Fig. 4.4C,  $p = .01$ ). This contrasts with R-values obtained when stimulus protocols are injected into only one LC at a time, see Chapter 3 Results, in which R-values are significantly reduced after TEA exposure. These data suggest that electrical coupling, like tuning of intrinsic excitability, acts in constraining uniform voltage output between LCs.

A caveat to this experimental approach is that TEA exposure also causes a significant increase in coupling conductance between the two cells in which the stimulus protocol was administered (Fig. 4.4D); the mechanism(s) behind this increase are unclear, though this increase may be responsible for the significant increase in R-value at the -40mV starting potential (Fig. 4.4C). This does not negate the result that electrical coupling helps maintain synchrony between LCs which are intrinsically “de-tuned” post-TEA exposure; however we cannot ensure that the strength of electrical coupling which is constraining output, is also physiologically relevant.

To effectively control coupling strength, and keep it within physiological range, while also using TEA to cause distinct intrinsic excitability between two LCs (as we do in chapter 3), we artificially insert electrical coupling between two isolated LCs using dynamic clamp. In these experiments we run Stimulus Protocol 1 on two isolated

anterior LCs (LC3 + LC4 or LC3 + LC5 pairings) within the same network, beginning after 10 minutes exposure to 25mM TEA. Stimulus protocol 1 is then run on the two cells with multiple, physiologically relevant coupling conductances, inserted via dynamic clamp (See Fig. 4.5A for experiment schematic) . We find, as is expected, that as coupling conductance increases the cross-correlation coefficient comparing the two LCs voltage response, also increases. In doing this across six animals we find that LC to LC synchronization is achieved within physiologically relevant levels of electrical coupling (Fig. 4.5B) after TEA exposure. Bar graph inset on Figure 4.5B shows that after TEA exposure, with only  $0.1\mu\text{S}$  of electrical coupling added, R-values range from  $0.93 - 0.99$  across six animals. This suggests LC to LC electrical coupling allows synchronization of burst output after a “de-tuning” of intrinsic conductances via TEA exposure.

**Are relationships between coupling strength and current magnitude involved in LC synchronization?**

In Figure 4.5B we find that some LC pairs require more electrical coupling to achieve a high cross correlation coefficient, or synchronized response (see Fig.4.5B black line vs. blue line). To investigate if this is based on the LCs intrinsic conductance organization, we compare  $I_{HTK}$  of the two LCs in each pair with how synchronized the cells response to Stimulus protocol 1 is (R-value); we do this comparison at two artificially inserted coupling strengths:  $0.05\mu\text{S}$  and  $0.1\mu\text{S}$ .

Based on relationships between strength of coupling and  $I_{HTK}$  present in the native network (see fig. 4.1 and fig. 4.3) we have two hypotheses: First, we predict with increased variability in  $I_{HTK}$  magnitude, a LC pairing will require greater strength in electrical coupling to maintain output. This is based on the relationship between LC  $I_{HTK}$  coefficient of variation and total coupling strength on each anterior LC. As a reduced measure of  $I_{HTK}$  variability in a single cell pair, we use the difference in  $I_{HTK}$  magnitude between the two cells. This difference is correlated to the cross correlation coefficient achieved at  $0.05\mu S$  and  $0.1\mu S$  coupling strength (Fig. 4.5C, D). If the hypothesis is correct we predict that cells with a larger difference in  $I_{HTK}$  will have a lower R-value at designated coupling strengths, this would result in a negative correlation across experiments. We do not find this to be true, instead we see no statistically significant relationship between the difference in  $I_{HTK}$  magnitude and R-value at either  $.05\mu S$  or  $.1\mu S$  coupling strength.

The second hypothesis is based on the positive relationship between magnitude of  $I_{HTK}$  and strength of electrical coupling present across LC4 / LC5 pairs(Fig. 4.3). We hypothesize that if two neurons require more coupling to synchronize activity, because of higher levels of  $I_{HTK}$ , than after removing  $I_{HTK}$  those cells will have a lower R-value at a given coupling strength; thus we will see a negative correlation between  $I_{HTK}$  magnitude and R-value at the  $0.05\mu S$  and  $0.1\mu S$  coupling strengths. Experiments support this hypothesis, we find a negative correlation between combined  $I_{HTK}$  magnitude and the R-value generated with a  $.05\mu S$  and  $.1\mu S$  coupling conductance. These data indicate the

positive relationship we see between  $I_{HTK}$  magnitude and coupling conductance (Fig. 4.3) is functional in maintaining a synchronized output between LCs.

## Discussion

In this chapter we find maintenance of a synchronized burst waveform across anterior LCs involves both tuning of intrinsic properties and electrical synaptic strength between anterior LCs. This is demonstrated in two relationships between the properties of the intrinsic conductance  $I_{HTK}$  and coupling conductance between anterior LCs. First we see that the three anterior LCs have different amounts of variability in the magnitude of  $I_{HTK}$ , with LC4 and LC5  $I_{HTK}$  having a larger coefficient of variation than LC3 (Fig. 1B *lower*, 1D). LC4 and LC5 also have significantly more LC to LC electrical coupling than LC3 (Fig. 1C, 1D). Because LC to LC electrical coupling helps constrain and synchronize burst output (Fig. 4B, C; Fig. 5B), we hypothesize that LC4 and LC5 are able to have a larger  $I_{HTK}$  parameter space than LC3, while maintaining synchronized output. To test if this hypothesis is functional, we examined how the difference in two LCs  $I_{HTK}$  magnitude correlates to the coupling conductance necessary to synchronize the two cells after TEA exposure. The reasoning in this experimental approach is if two cells have very different  $I_{HTK}$  magnitude, than this would represent a larger parameter space of  $I_{HTK}$ , and those cells would require a larger amount of coupling conductance to synchronize output, than a coupled pair with very similar  $I_{HTK}$  values. This was not the case. There

was no correlation with the difference in two cells original  $I_{HTK}$  magnitude with how much coupling was necessary to synchronize the two cells output (Fig. 5C,D).

This result, however does not displace the idea that variability in intrinsic properties may have a relationship with how much electrical coupling is necessary to synchronize output. It only demonstrates that a measure of  $I_{HTK}$  difference cannot be used to represent how disparate or similar two cell intrinsic conductance organization actually is. A better way to conduct this experiment would be to insert electrical coupling between LCs of the same number, as in LC3-LC3, LC4-LC4, and LC5-LC5. If LC3 does have a more constrained parameter space than LC4 and LC5, than we can expect that an LC3 neuron pair would not need as much electrical coupling to synchronize activity than LC4 pairs or LC5 pairs after disrupting intrinsic organization.

The second relationship we find is a positive correlation between  $I_{HTK}$  magnitude and coupling strength across the LC4 and LC5 coupled neurons. This positive correlation exists if only one LCs  $I_{HTK}$  magnitude is compared to coupling strength (data not shown), or the two cells combined  $I_{HTK}$  magnitude is compared to coupling strength (Fig. 3). Using dynamic clamp we go on to show that when two LCs original  $I_{HTK}$  values are high, after TEA exposure those two cells require more electrical coupling to synchronize output (Fig. 5E, F), thus suggesting the positive relationship between  $I_{HTK}$  and coupling strength has functional significance in regards to LC synchronization.

The next question that presents itself regarding the  $I_{HTK}$  / coupling strength correlation is what causes it. A problem in searching for co-regulated intrinsic and coupling strength properties is that intrinsic conductances, and even passive properties, can have a direct effect on coupling conductance(Saraga et al., 2006, Pereda et al., 2013). This has been demonstrated with  $I_{NaP}$  and low threshold potassium currents directly influencing coupling strength between neurons (Curti and Pereda, 2004, Haas and Landisman, 2011, Curti et al., 2012). We cannot treat coupling strength as a separate parameter from intrinsic conductances until it is demonstrated, perhaps with dynamic clamp, that the  $I_{HTK}$  measured is not directly affecting coupling conductance, and thus not also causing the relationship. However, we do not believe the positive correlation we see between coupling strength and  $I_{HTK}$  is the result of  $I_{HTK}$  current having a direct effect on coupling conductance. After TEA exposure, and removal of  $I_{HTK}$ , we actually see coupling conductance between LCs significantly increased; this result would argue that if  $I_{HTK}$  does affect coupling conductance, than its influence is to weaken, not strengthen, electrical coupling.

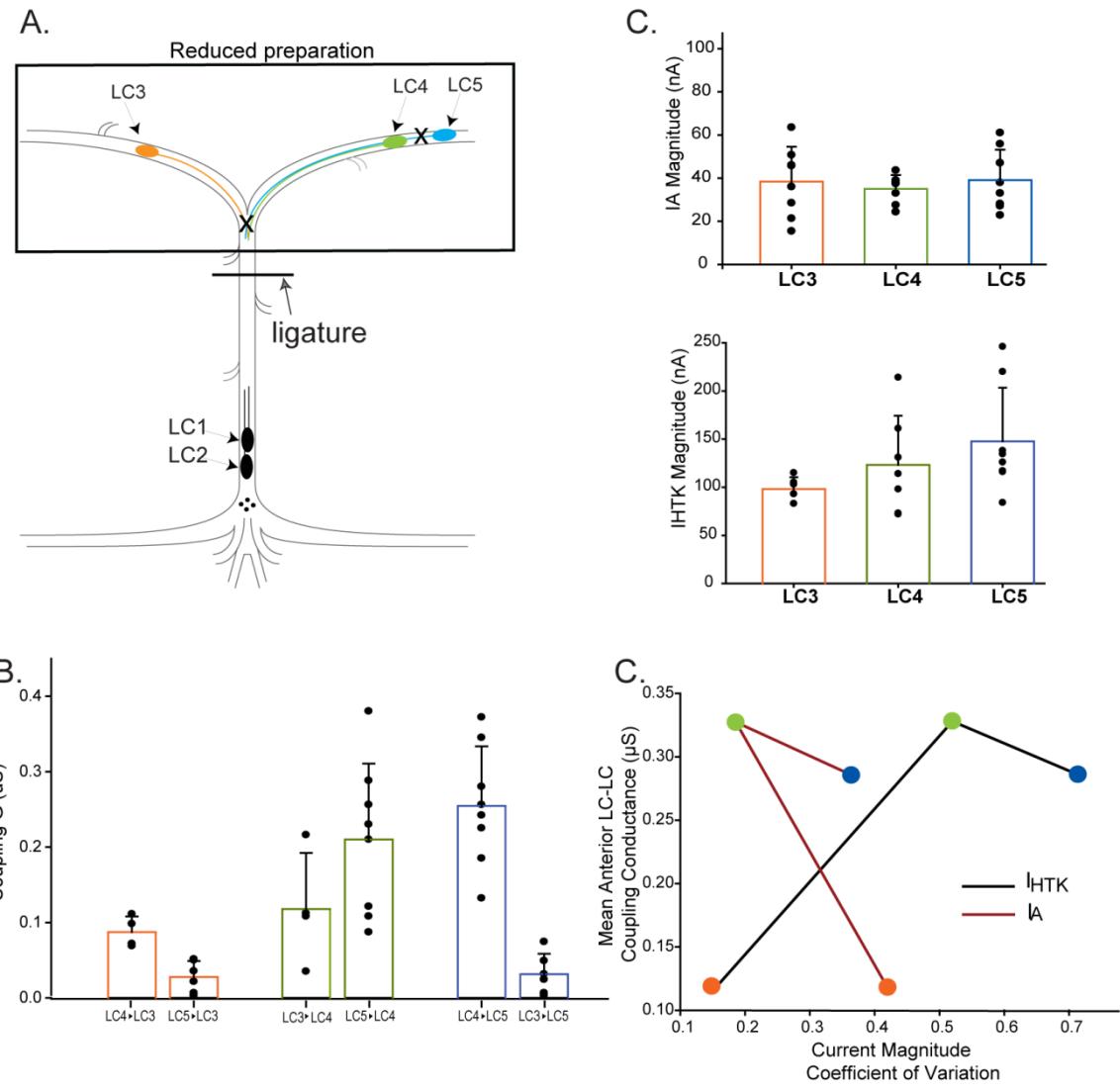
Still, we cannot conclude that  $I_{HTK}$ , or  $I_{HTK}$  alone, is co-regulated with coupling strength; a larger value of  $I_{HTK}$  may also be just a result, or symptom, of the intrinsic parameter(s) that are coregulated with coupling strength. In biological experiments we are limited by what properties we can measure at any given time, so we are unlikely to find a definite answer to this in biological experiments alone. This is an opportune time

for a LC conductance based modeling study, in which all intrinsic parameters may be examined in respect to LC to LC coupling strength and synchronization. A back and forth of modeling experiments / hypotheses, to biological testing of those hypotheses, would be an effective way to continue probing these relationships.

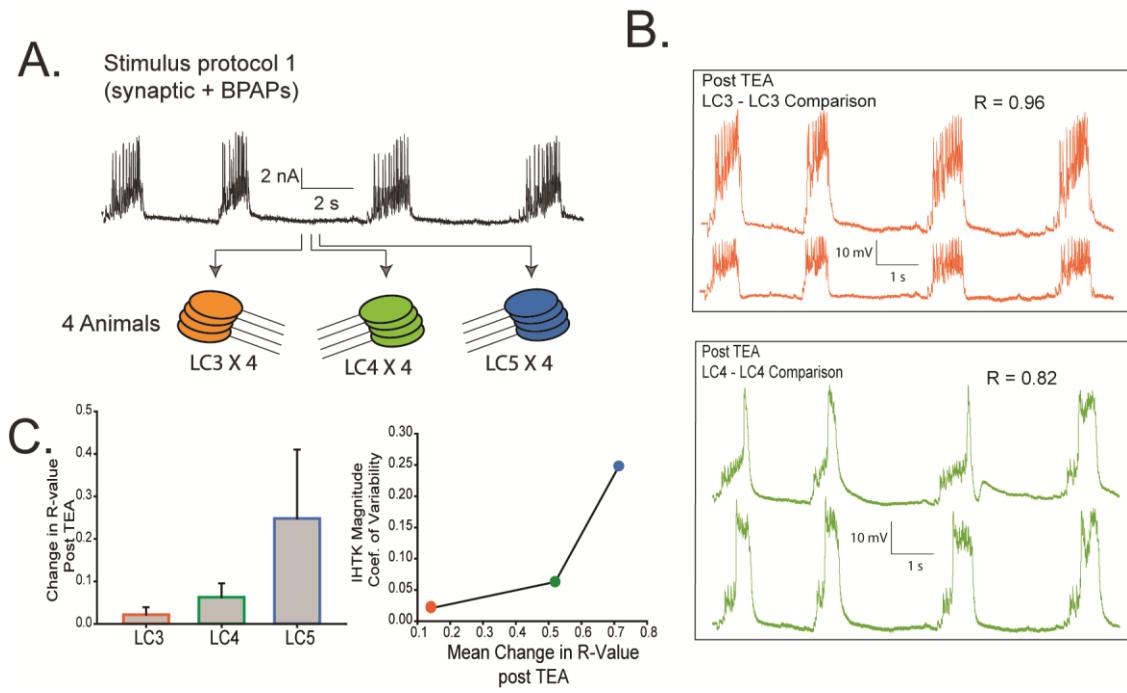
Ideas regarding the functional role of gap junctions in generating appropriate neural output has become more complex in recent years. While originally gap junctions were thought to be largely passive, bidirectional structures which allow the sharing of voltage changes between two neurons (Connors and Long, 2004); we now understand that gap junctions can be rectifying (Marder, 2009), plastic in strength (Haas et al., 2011) and can be shaped by the intrinsic conductances present in the two neurons (Curti and Pereda, 2004, Haas and Landisman, 2011, Curti et al., 2012). With a new appreciation of the dynamic properties gap junctions possess, it is important that we explore ways in which coupling strength between cells are regulated and how this impacts the functional output of the network. Using the anterior LCs of the *C. borealis* CG we have an appropriate model to explore possible mechanisms behind gap junction regulation, and if those mechanisms are functional in synchronization of motor output.

In this study we explore the possible co-regulation between intrinsic conductances of LC motor neurons with LC to LC coupling strength, we investigate these relationships in regards to functional output property of LC synchronization. The idea that this co-

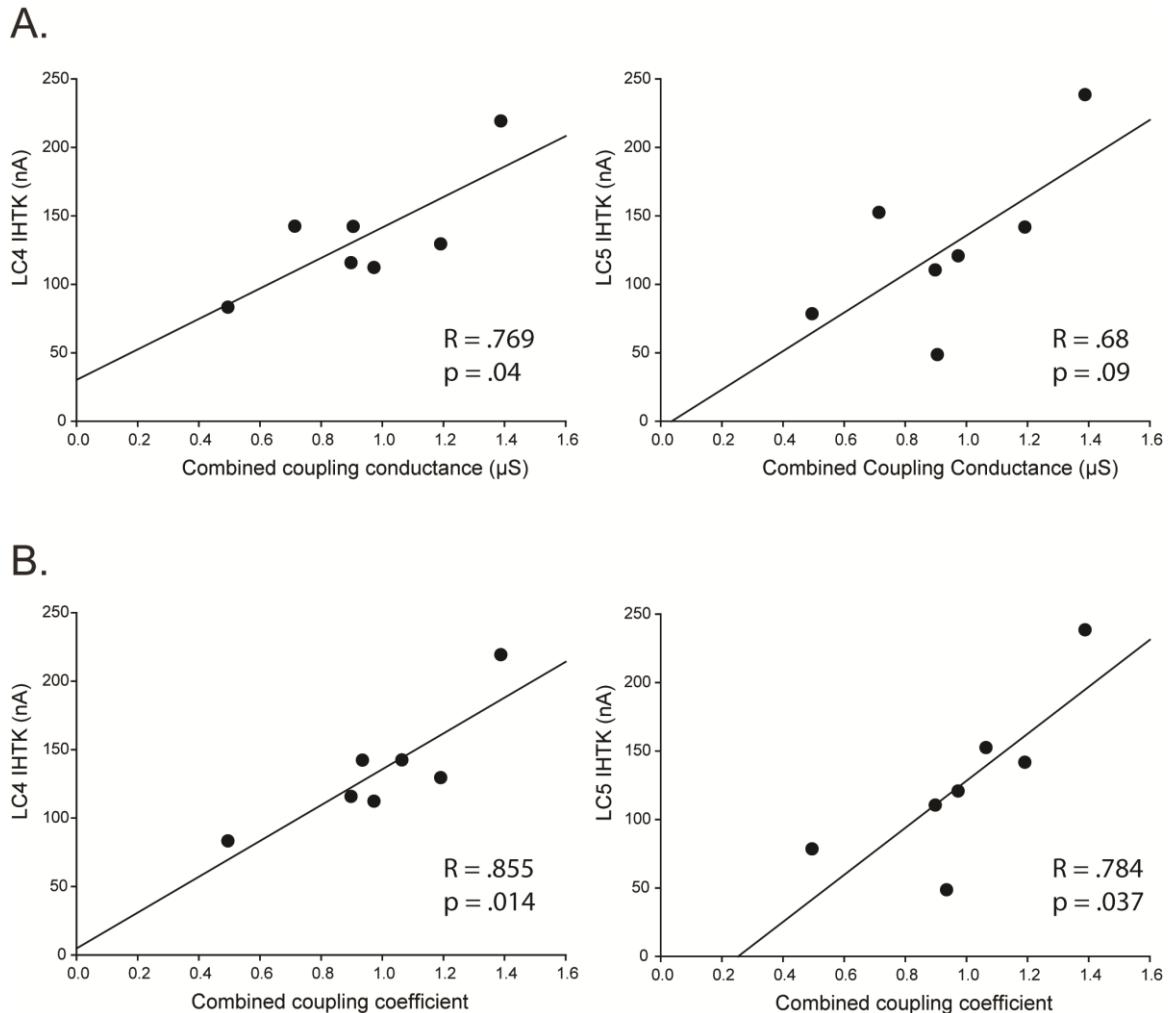
regulation may be occurring, and important has already been investigated, but at the theoretical level with computational models (Manor et al., 1997, Perez Velazquez and Carlen, 2000, Soto-Trevino et al., 2001, Pfeuty et al., 2003). In this regard theoretical studies are used to reduce complicated model systems to study how gap junction properties, intrinsic membrane properties and network architecture interact, and are summed, to produce a given network phenotype such as burst and spike synchrony or asynchrony. Attempting to understand how so many parameters, and combinations of parameters, are likely regulated to control output is a difficult feat even from a theoretical perspective. A study by Soto-Trevino et al. (2001) demonstrate this when they investigate parameters which affect output of two coupled model stomatogastric neurons. In this study the investigators limit the parameters which are varied to coupling strength, compartmental structure and weather the coupled cells are distinct or similar in properties of excitability. They find that in varying these parameters they can generate a variety of network and neuron behaviors, with some being unintuitive. While this is an appropriate strategy, especially while dealing with large neural networks and / or multiple parameter states within the network, it is important to test ideas and principles derived from these theoretical studies in biological models. The *C. borealis* CG is ideally situated to do this; furthermore this model system has its own conductance based model which will allow an eventual back in forth between biological study results, and computational model predictions.



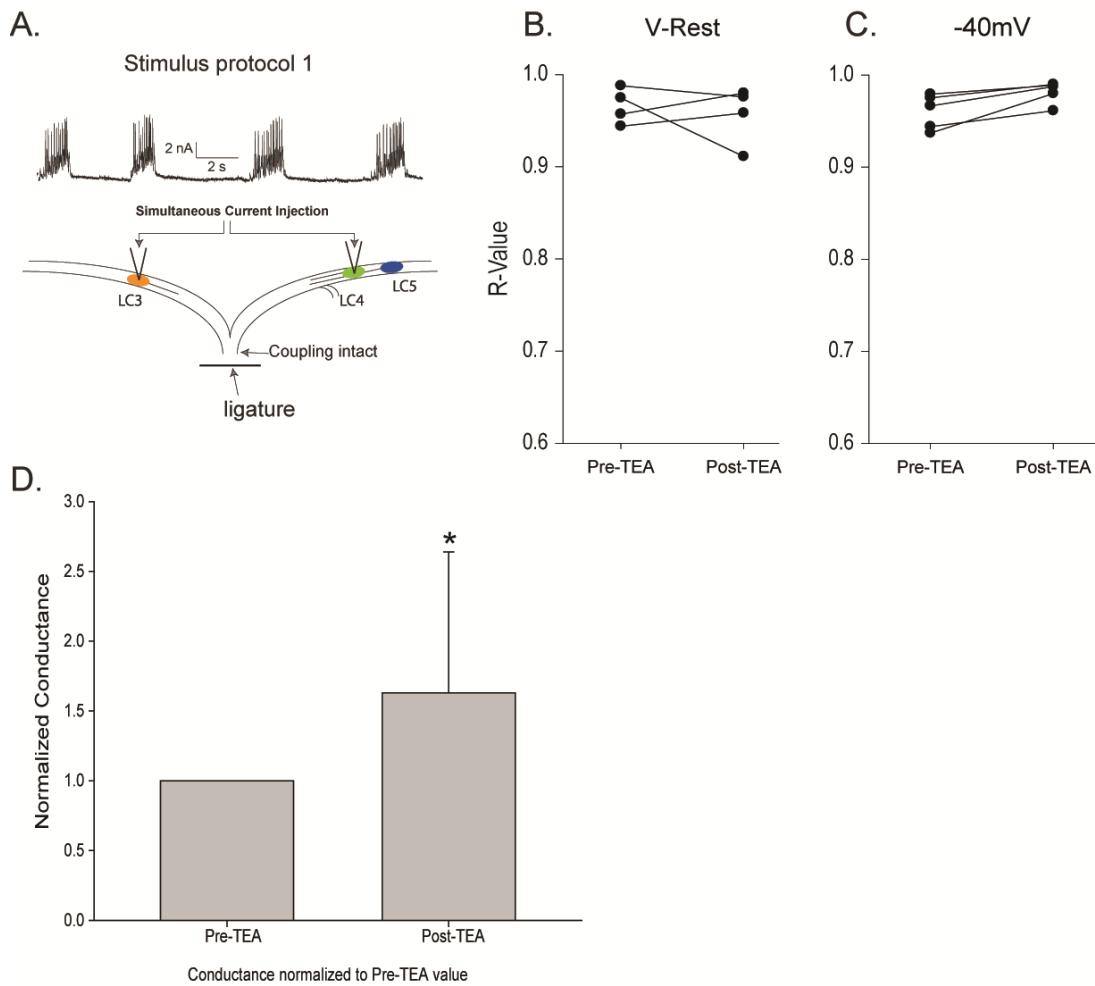
**Figure 4.1 LC 3, LC4 & LC5 strength of coupling to other anterior LCs correlates with LC3, LC4 & LC5 variability in  $I_{HTK}$  magnitude.** **A.** Schematic of reduced anterior LC preparation. “X” mark areas where electrical coupling is present between anterior LCs. Note: right branch “X” marks LC4 / LC5 local electrical coupling. Colors of LC3, LC4 and LC5 somata remain consistent throughout figures in Chapter 4. **B.** Mean  $\pm$  Std. Dev. coupling conductance between anterior LCs. Circles overlaid on bar graph are individual LC coupling conductance values. Color of each bar indicate which LC the coupling conductance affects. **C.** Mean  $\pm$  Std. Dev. of  $I_A$  (upper) and  $I_{HTK}$  (lower) in respect to LC3, LC4 and LC5. Individual LC current measurements overlaid on bars. **D.)**  $I_{HTK}$  (black line) and  $I_A$  (red line) coefficient of variation vs. mean total coupling conductance in respect to LC3, LC4 and LC5 (color coded). Note: total coupling conductance is calculated by adding together the mean coupling conductance of one LC with the two other anterior LCs. i.e. LC4 to LC3 conductance + LC5 to LC3 conductance = total LC3 coupling to anterior LCs.



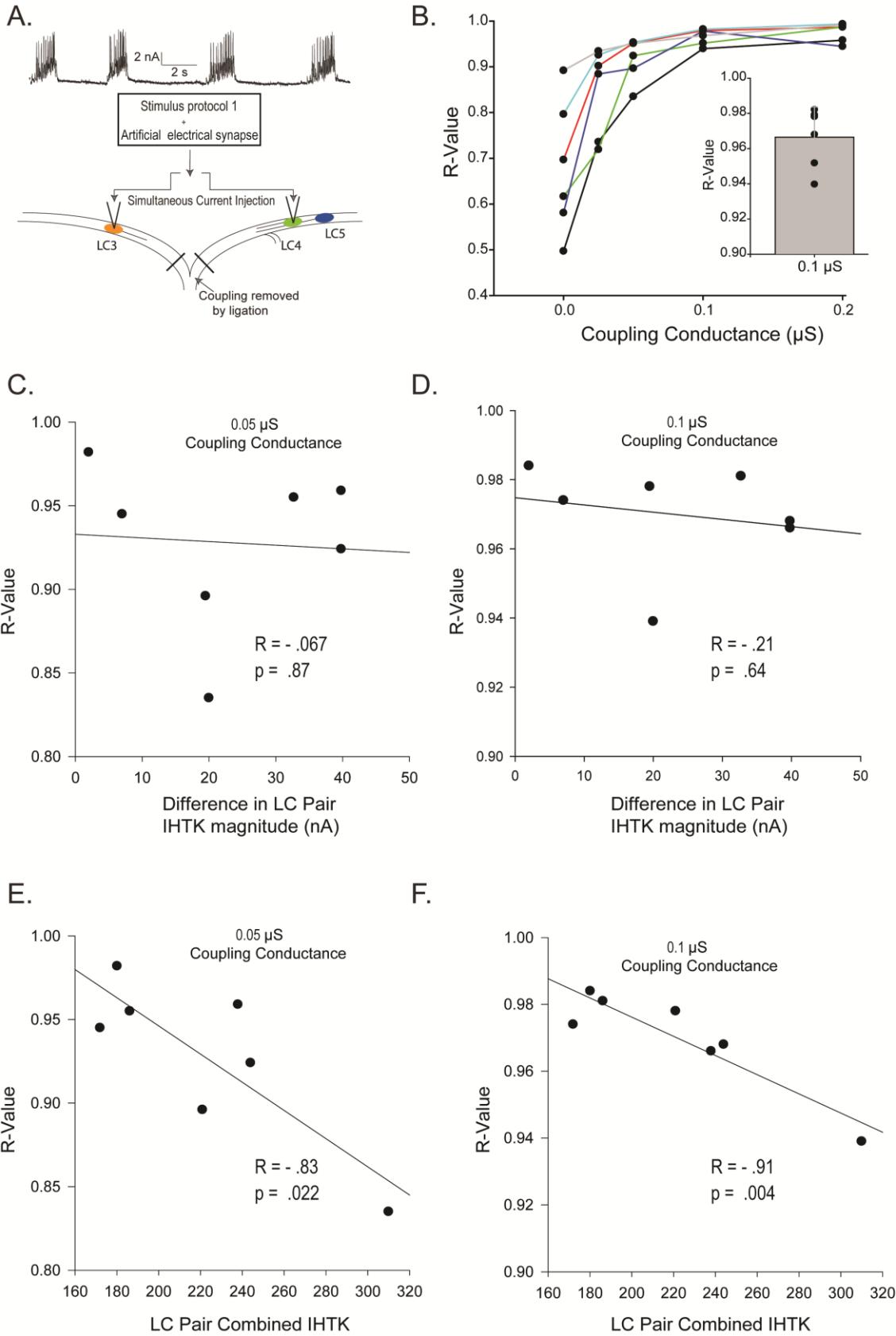
**Figure 4.2 TEA exposure affects LC3, LC4 and LC5 differentially and in coordination with  $I_{HTK}$  coefficient of variation.** **A.** Stimulus protocol one was injected in each anterior LC of four animals before and after TEA exposure. **B.** Example voltage response to Stimulus Protocol 1 comparisons. *Upper-* two LC3 neuron voltage response comparisons. *Lower-* two LC4 neuron comparisons. **C.** (*left*) Mean  $\pm$  Std. Dev. change in R-value after TEA exposure. Voltage waveform in response to current injection was cross-correlated between LCs of a given type (LC3 was only compared to other LC3 cells). (*right*) Mean change in R-value after TEA exposure vs.  $I_{HTK}$  coefficient of variation in regards to each anterior LCs (color coded).



**Figure 4.3 Coupling strength and  $I_{HTK}$  magnitude are positively correlated across LC4 / LC5 pairs. A. Coupling conductance vs. LC4 (left) and LC5 (right)  $I_{HTK}$  magnitude. B. Coupling coefficient vs. LC4 (left) and LC5 (right)  $I_{HTK}$  magnitude.  $I_{HTK}$  measured at 0mV voltage step.**



**Figure 4.4 Synchronous voltage response to depolarizing stimuli is maintained by electrical coupling.** **A.** Experimental diagram; Stimulus Protocol 1 is injected in two anterior LCs simultaneously before and after TEA exposure with electrical coupling intact. **B.** R-values are not significantly affected by TEA exposure when electrical coupling is left intact; current injection protocols are administered at LCs resting membrane potential. **C.** R-values are significantly increased by TEA exposure when electrical coupling is left intact; current injection protocols are administered at -40mV starting potential. DC current injection used bring starting potential to -40mV. **D.** Coupling conductance is significantly increased post-TEA exposure ( $p = .04$ ). Coupling conductance normalized to pre-TEA conductance values.



**Figure 4.5 Anterior LC electrical coupling and  $I_{HTK}$  magnitude are important in maintaining synchronous output.** **A.** Experimental diagram- depolarizing stimuli and artificial electrical coupling are injected into two isolated anterior LCs simultaneously after TEA exposure. **B.** R-values comparing voltage response of two isolated LCs to depolarizing stimuli with different electrical coupling strength values (x-axis). Colored lines separate experimental preparations. *Bar graph inset-* Mean + std. dev. R-value measurements across six animals with  $0.1 \mu\text{S}$  coupling conductance inserted between isolated LCs. **C-D.** Difference between  $I_{HTK}$  magnitude (x-axis) is not correlated to LC synchronization at  $.05 \mu\text{S}$  and  $.1\mu\text{S}$  coupling conductance values. **E-F.**  $I_{HTK}$  magnitude (x-axis) is significantly correlated to LC synchronization at  $.05 \mu\text{S}$  and  $.1\mu\text{S}$  coupling conductance values.

## Conclusion

An important and fundamental problem in neuroscience is revealing how underlying parameters in neurons and neural networks, generate a particular electrical output. While the strategy to do this is a seemingly simple task of characterizing the underlying biophysical components behind neuronal excitability, recent experiments on model biological and theoretical systems, in which measurements can be taken from multiple cells with identical electrical output, have complicated the issue. Until recently it was thought that two neurons which generate the same output likely have identical underlying organization. Through computational and biological experiments this hypothesis has been fundamentally altered, arguing instead that multiple intrinsic solutions can be used to generate the same output (Golowasch et al., 2002, Prinz et al., 2004a, Taylor et al., 2009, Ball et al., 2010a). Biological studies have typically provided evidence for this hypothesis by characterizing variability, along with compensatory interactions, between two or more cellular properties underlying excitability. These interactions can take place between properties intrinsic to the cell (ionic channels / currents) (Guo et al., 2005, Haedo and Golowasch, 2006, Khorkova and Golowasch, 2007, Nerbonne et al., 2008, Ransdell et al., 2012, Temporal et al., 2012) and also among network level properties such as synaptic strength (Turrigiano, 2008, Turrigiano, 2011b, 2012).

Here we utilize the *C. borealis* CG LC motor neurons to continue investigating how small networks organize underlying properties to generate a stable and functional output. The crustacean CG is a unique model system in which different types of parameters underlying network output can be segregated and studied in isolation. I break these parameters into three general classes- intrinsic excitability properties of the cell, network level interactions and neuromodulation. In the above chapters we focus our investigations on LC intrinsic parameter regulation, along with how these intrinsic parameters appear to interact with network level properties.

Briefly summarizing, I make the following conclusions as a result of these studies:

1. LC motor neurons, within the same network, utilize differential tuning of intrinsic burst generating conductances, while maintaining similar levels of excitability.
2. Two of these intrinsic currents,  $I_A$  and  $I_{HTK}$ , maintain a negative relationship across LCs, and can rapidly compensate for one another via a post-transcriptional mechanism.
3. LC  $I_{HTK}$  also maintains a relationship with coupling strength between LCs, and this relationship is functional in synchronization of LC motor neuron output.

A general theme in these findings is that there are multiple levels of regulation which are active in maintaining appropriate output in LC motor neurons. Beyond sensory feedback from heart musculature, one level of regulation which is completely left out of these studies is neuromodulation. Previous work demonstrates that the *C. borealis* CG is responsive to neuromodulatory substances (Cruz-Bermudez & Marder, 2007). Building on what we currently know regarding maintenance of CG output, studies involving neuromodulatory effects on CG output can provide important information regarding homeostatic plasticity of networks under neuromodulation. For instance, we understand that internetwork LCs have disparate conductance organization tuned to similar levels of excitability. Because neuromodulation often causes changes in conductance organization (Marder, 2011, 2012), will a neuromodulatory substance applied to each of the CG LCs cause disparate levels of excitability across LCs within a network? A de-tuning of conserved excitability similar to what TEA accomplishes in Chapter 3? If so, does coupling across LCs protect against disparate excitability levels or LCs under neuromodulation, and maintain synchronous LC bursts? The potential of these type of experiments validate why the CG is an advantageous model, in that we are able to separate and study multiple types of parameters, along with how these types of parameters interact, to produce appropriate network output.

The studies described in the above chapters build a sound foundation for understanding how LC motor neurons utilize intrinsic currents along with network properties, to generate synchronous bursts. However, there is still much to do in this

regard. In collaboration with the lab of Satish Nair (University of Missouri- Columbia Department of Electrical Engineering) we have used biological measurements from *C. borealis* LCs to help generate a conductance based computational model of LC motor neurons, as well as the nine cell cardiac network. We believe that an evolving interaction between biological studies in the CG, and theoretical studies in this model, will be extremely beneficial to the generation and testing of hypotheses regarding how underlying properties are regulated and maintained to generate LC and CG network output.

While potential studies utilizing this model are endless, I will lay out two which I think can push the most recent CG research forward:

1. I mention in chapter 4 that it is difficult to ascertain if correlations between LC  $I_{HTK}$  and coupling strength is the direct result of active co-regulation, or if the  $I_{HTK}$  magnitude is instead a symptom of other LC conductance parameters which are co-regulated with electrical coupling strength. Using a computational model we could perform similar experiments, yet have access to the full complement of LC conductances, to investigate which may be co-regulated with electrical coupling strength. In this regard, we should also investigate and quantify single LC mRNA expression of genes involved in electrical coupling (*innexin*) and genes which contribute to  $I_{HTK}$  magnitude (*BKKCA*, *shab*, *shaw*).

2. One interesting feature of the CG is that five LCs are present in an individual network, which are synchronized in burst output, and do largely the same thing. Why do five redundant neurons exist? Especially with the reticular organization of the network (Garcia-Crescioni and Miller, 2011), why can there not be one LC motor neuron with an extensive neuritic projection? One hypothesis is that because the LC output is very important to the animal, having five electrically coupled cells will ensure that if one cell has incorrect level of excitability, the four coupled LCs would act to dampen or constrain the incorrect burst. Two example situations which may result in harmful disturbance to a LCs level of excitability: stochastic turnover of ion channel proteins, and other proteins affecting cell excitability, may momentarily disrupt the conserved excitability across network LCs throughout the lifetime of the animal. Also, neuromodulation, which is known to affect conductance organization, may cause disparate levels of excitability across the five LCs.

In both these examples electrical coupling across five redundant neurons may be necessary to constrain appropriate output. To test this idea we can isolate a single biological LC and, using dynamic clamp, connect the biological neuron to four model LCs via electrical synapse. We could then use TEA exposure to de-tune the excitability of the biological neuron, and study how coupling strength between the four model cells constrains the isolated LCs burst output. Alternatively, we could de-tune one, two, or three of the model cells and

investigate how coupling strength with the biological neuron acts in constraining burst output.

The two potential experimental discussed above are only the beginning of possible questions an interaction between the CG model and biology based experiments can be used to answer. The theme which will likely hold across future CG studies is that the investigator has control to selectively limit and study multiple levels of regulation which underlie both cellular and network output; that is, intrinsic organization of the single cell, synaptic network properties in the reticular CG network and neuromodulatory input. Here we have conducted studies characterizing the intrinsic biophysical properties of LC motor neurons, and homeostatic interactions which tune appropriate output via intrinsic conductance organization and electrical coupling. In doing this we have provided novel insights regarding underlying regulation of neuronal excitability, but perhaps more importantly, we provide a valuable electrophysiological characterization of a model system which has the potential to help answer important fundamental questions in neuroscience.

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## VITA

I was born in Columbia, Missouri to parents Beverly and John Ransdell who are originally from Hannibal, Missouri. I grew up in Columbia with two older brothers and one older sister and attended David H. Hickman High School. In high school I was able to take several advanced placement courses during my Junior and Senior Years. One of these courses was AP Psychology; the instructor, Mrs. Fick, taught in a compelling way and pointed out that the physical basis behind many psychiatric disorders are currently unknown. This compelled me to explore possible career paths in neuroscience research.

I attended the University of Minnesota- Twin Cities and majored in Neuroscience. During my time as an undergraduate I worked in several laboratories which involved multiple areas of neuroscience research. These included molecular neuroscience (Dr. Robert Elde), behavioral neuroscience (Dr. Marilyn Carroll) and systems / cellular neuroscience (Dr. Karen Mesce). In Dr. Mesce's lab I was astonished at how researchers were able to take simple, yet important behaviors, in this case leech locomotion, and dissect the neural circuit mechanisms responsible. This physical characterization of circuit function, and connection to important behavioral output, triggered in me an immediate fascination.

After graduating with a B.S. in Neuroscience I was accepted into the University of Missouri- Columbia Biological Sciences Ph.D. program. During the application process I met with Dr. David Schulz and discussed his unique approach to understanding circuit mechanisms using a combination of electrophysiology and molecular biology techniques. His ideas and biological questions convinced me to join his lab which I worked in for the next five years. Since finishing my undergraduate I married my wife Chi, had a son Joseph and gained a new and better perspective on scientific reasoning. I accepted a postdoctoral position in Dr. Jeanne Nerbonne's laboratory at Washington University in St. Louis. In Dr. Nerbonne's laboratory I will continue to study mechanisms behind regulation of excitability, only in mammalian cortical neurons and human myocytes. I plan to remain active in neuroscience research throughout my career.